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***Case Control Study***

**Textural differences based on apparent diffusion coefficient maps for discriminating pT3 subclasses of rectal adenocarcinoma**

Lu ZH *et al.* DWI for pT3 rectal adenocarcinoma

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**Abstract**

BACKGROUND

The accuracy of discriminating pT3a from pT3b-c rectal cancer using high-resolution magnetic resonance imaging (MRI) remains unsatisfactory, although texture analysis (TA) could improve such discrimination.

AIM

To investigate the value of TA on apparent diffusion coefficient (ADC) maps in differentiating pT3a rectal adenocarcinomas from pT3b-c tumors.

METHODS

This was a case-control study of 59 patients with pT3 rectal adenocarcinoma, who underwent diffusion-weighted imaging (DWI) between October 2016 and December 2018. The inclusion criteria were: (1) Proven pT3 rectal adenocarcinoma; (2) Primary MRI including high-resolution T2-weighted image (T2WI) and DWI; and (3) Availability of pathological reports for surgical specimens. The exclusion criteria were: (1) Poor image quality; (2) Preoperative chemoradiation therapy; and (3) A different pathological type. First-order (ADC values, skewness, kurtosis, and uniformity) and second-order (energy, entropy, inertia, and correlation) texture features were derived from whole-lesion ADC maps. Receiver operating characteristic curves were used to determine the diagnostic value for pT3b-c tumors.

RESULTS

The final study population consisted of 59 patients (34 men and 25 women), with a median age of 66 years (range, 41-85 years). Thirty patients had pT3a, 24 had pT3b, and five had pT3c. Among the ADC first-order textural differences between pT3a and pT3b-c rectal adenocarcinomas, only skewness was significantly lower in the pT3a tumors than in pT3b-c tumors. Among the ADC second-order textural differences, energy and entropy were significantly different between pT3a and pT3b-c rectal adenocarcinomas. For differentiating pT3a rectal adenocarcinomas from pT3b-c tumors, the areas under the curves (AUCs) of skewness, energy, and entropy were 0.686, 0.657, and 0.747, respectively. Logistic regression analysis of all three features yielded a greater AUC (0.775) in differentiating pT3a rectal adenocarcinomas from pT3b-c tumors (69.0% sensitivity and 83.3% specificity).

CONCLUSION

TA features derived from ADC maps might potentially differentiate pT3a rectal adenocarcinomas from pT3b-c tumors.

**Key words:** Diffusion-weighted imaging; Apparent diffusion coefficient; Rectal cancer; Cancer stage; Texture analysis; case-control study

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**Core tip:** texture features derived from apparent diffusion coefficient maps might potentially differentiate pT3a rectal adenocarcinomas from pT3b-c tumors.

**INTRODUCTION**

Colorectal cancer, the third commonest malignancy around the world, most commonly affects elderly individuals ≥ 60 years old, with a male predominance[1-3]. The incidence of rectal cancer was 5.2 per 100000 in 2014[4]. The 5-year relative survival is 37%-100% for local disease (varying widely according to perineural invasion and satellite nodules), 44% for locoregional disease, and 8%-15% for metastatic disease[5].

The majority (60%-80%) of rectal tumors are in the pT3 stage at diagnosis, constituting a heterogeneous group[6,7]. The extramural depth (EMD) of tumor invasion is one of the most important prognostic factors in rectal cancer, and strongly influences survival and local recurrence[6]. The 5-mm cut-off of EMD has been determined to be the most discriminating and simple to use in clinical practice regardless of differences in overall survival (OS) and local recurrence[6-9]. Locoregional recurrence and cancer-related 5-year survival rates are 10.4% and 85.4% for pT3a (EMD < 5 mm), respectively, and 26.3% and 54.1% for pT3b (EMD ≥ 5 mm), respectively[9]. Therefore, there is a need for a preoperative imaging method to noninvasively identify patients with high-risk pT3 in order to provide individualized treatment strategies.

Magnetic resonance imaging (MRI) with a phased-array surface coil has an undeniable role in the preoperative staging of rectal cancer. In preoperative local T staging, the reported overall accuracy of MRI is 71%-90%[10-13]. In two studies on pT3 subclassification, the accuracies of MRI were 71.2% and 86%[10,12]. However, the accuracy of staging using high-resolution MRI remains unsatisfactory. In recent years, the potential of MRI has extended from morphological assessments to texture analysis (TA). TA refers to various mathematical-statistical methods used to extract texture features by evaluating the spatial variation of gray levels within given images[14]. These features can be used to characterize and measure tissue heterogeneity in medical images. Some texture features are useful tools for accurate diagnosis, preoperative risk stratification, and assessment of treatment response in several cancers[15-18]. Previous studies have demonstrated that MRI-based texture features are efficient in identifying preoperative KRAS mutation status in rectal cancer cases[19,20]. In addition, several MRI features and TA were shown to be valuable for predicting the therapeutic response to neoadjuvant chemoradiotherapy (nCRT) for rectal cancer and tumor recurrence[21]. However, another study reported that MRI T2-weighted sequence-based TA is not effective in predicting pathological complete response to nCRT in patients with locally advanced rectal cancer, suggesting that additional trials are required for comprehensively analyzing the potential of MRI-derived TA in this setting[22].

Diffusion-weighted imaging (DWI) is important in rectal cancer imaging because it provides superior contrast between cancerous and non-cancerous tissues. In a previous study[11], DWI was shown to be useful for evaluating the pT stage of rectal cancer and guiding EMD measurement. In addition, the apparent diffusion coefficient (ADC), a quantitative value of DWI, has been reported to correlate with the pT stage[11,23]. Nevertheless, the mean and median ADC values are not always significantly sensitive to small changes or precise status of the tumor owing to the intrinsic chaotic environment of tumors[24]. In addition, pT3 subclasses of rectal cancer have not been previously determined by ADC maps.

Given the increasing use of DWI in rectal cancer imaging and the quantitative value of ADC for accurate diagnosis, we hypothesized that texture features derived from ADC maps could discriminate pT3 subclasses. Therefore, the aim of this study was to investigate the value of TA on ADC maps in differentiating pT3a rectal adenocarcinomas from pT3b-c tumors. The results could provide interesting features for the tailoring of treatment strategies.

**MATERIALS AND METHODS**

***Study design and patients***

This case-control study was approved by the Institutional Review Board of the Changshu Hospital Affiliated to Soochow University (2018 Ethics Audit (Declaration) Batch No. 3). The requirement for individual informed consent was waived because of the retrospective design of the study. The patients who underwent imaging at the Changshu Hospital Affiliated to Soochow University between October 2016 and December 2018 were included (*n* = 120).

The inclusion criteria were: (1) Proven pT3 rectal adenocarcinoma; (2) Primary MRI including high-resolution T2-weighted image (T2WI) and DWI; and (3) Availability of pathological reports of surgical specimens. A total of 67 patients met these criteria. Eight patients were excluded for the following reasons: (1) Poor image quality apparent on DWI (*n* = 2); (2) Treatment with preoperative chemoradiation therapy (*n* = 4); and (3) A different pathological type, such as mucinous adenocarcinoma (*n* = 2).

***Data collection***

Patient features (age and sex), pathological characteristics (grade and stage), and DWI TA features (ADC, skewness, kurtosis, uniformity, energy, entropy, inertia, and correlation) were collected from the medical charts.

***MRI***

All patients were imaged using a 3.0-T MRI system (Intera Achieva 3.0T TX, Philips Medical System, Best, The Netherlands) and a 16-channel phased-array surface coil. Thirty minutes before the MRI examination, all patients were asked to take clyster in order to reduce artifacts caused by gas within the rectum. The patients also received 10 mg of anisodamine (Hangzhou Mingsheng Pharmaceuticals Co., Ltd., Zhejiang, China) by intramuscular injection 10 min before the examination to reduce bowel peristalsis.

The standard rectal imaging protocol consisted of sagittal T2WI turbo spin-echo (TSE) [repetition time/echo time (TR/TE), 3577/70 ms; TSE factor, 20; slice thickness, 3 mm; interspace, 0 mm; field of view (FOV), 24 cm] and high-resolution axial and coronal T2W (TR/TE, 3000/75 ms; TSE factor, 18; slice thickness, 2 mm for coronal and 3 mm for axial; interspace, 0 mm; FOV: 18 cm). Axial T2WI was perpendicular to the tumor axis, as identified on sagittal T2WI. Coronal T2WI was angled parallel to the tumor axis. In addition, axial DWI was used (TR/TE, 2750/76 ms; slice thickness, 3 mm; interspace, 0 mm; FOV, 22-24 cm; b-values, 0, 1000 s/mm2). Dynamic contrast-enhanced imaging was not assessed in this study. ADC maps were automatically generated from DWI data using a mono-exponential decay model.

***Image analysis and textural features calculation***

The primary tumor was distinguished on high-resolution T2WI and DWI based on final pathological outcomes. The primary tumor site was determined as a focal mass or abnormal wall thickening with intermediate signal intensity on T2WI, hyperintensity on DWI (*b* value = 1000 s/mm2), and the corresponding hypointensity on grey-scale ADC map. The entire tumor volumes were segmented independently by two experienced radiologists (Z.L. and H.J., with 9 and 4 years of experience in gastrointestinal MRI, respectively), using the Omni-Kinetics software (GE Healthcare, Waukesha, WI, United States). The resulting ADC maps were imported into Omni-Kinetics. The regions of interest (ROIs) were manually drawn slice by slice just inside the outer margin of the lesion to minimize partial volume error. The entire tumor area was covered as much as possible on ADC maps with reference to T2WI and DWI. Areas of necrosis, cysts, and gas were avoided to minimize bias. All ROIs were selected to derive the volume of interest (VOI). Then, first- and second-order texture features based on ADC maps were calculated automatically. ADC first-order texture features, as histogram features, included mean value, ADC percentiles (5th, 10th, 25th, and 90th percentiles), skewness, kurtosis, and uniformity. The ADC second-order texture features were derived from the gray-level co-occurrence matrix (GLCM), and included energy, entropy, inertia, and correlation.

***Histopathologic extramural depth of tumor invasion***

The mean time between MRI and surgery was 3.6 ± 1.4 d (range, 2-7 d). One pathologist (M.W., 15 years of experience) measured the EMD of tumor invasion on histopathologic specimens (stained routinely with hematoxylin and eosin) according to the criteria of The Radiologic Society of North America (RSNA)[7]. EMD was defined as the maximum depth of the extramural tumor spreading outside the muscularis propria (pT3a, < 5 mm; pT3b, 5-10 mm; pT3c, > 10 mm)[7]. The pathologist measured the distance between the outer border of the identifiable muscularis propria layer and the outermost border of the tumor. If the outer border was not clear, then the pathologist checked the outer border at both ends of the tumor to determine clear areas, and drew a tentative line designating the outer border of the muscle layer.

***Statistical analysis***

Statistical analyses were performed using SPSS 16.0 (IBM, Armonk, NY, United States) and MedCalc 9.0 (MedCalc Software, Mariakierke, Belgium). *P*-values < 0.05 were considered statistically significant. The Kolmogorov‑Smirnov test was used to determine the distribution of all continuous data. Normally distributed data are presented as the mean ± SD, while those with a skewed distribution are presented as the median and interquartile range. ADC texture features were compared between the pT3a and pT3b-c stages by independent samples Student's *t*-test or the Mann-Whitney *U*-test. Receiver operating characteristic (ROC) analysis was used to assess the diagnostic value of each statistically significant feature for the detection of pT3a tumors as previously proposed[25]. The areas under the curves (AUCs) were compared using the method of Delong *et al*[26]. Interobserver variability of ADC texture features extraction was evaluated using intra-class correlation coefficients (ICCs) as follows: 0.00-0.20, poor agreement; 0.21-0.40, fair agreement; 0.41-0.60, moderate agreement; 0.61-0.80, good agreement; and 0.81-1.00, excellent agreement.

**RESULTS**

***Characteristics of the patients***

A summary of the baseline characteristics of the patients is shown in Table 1. The final study population consisted of 59 patients (34 men and 25 women), with a median age of 66 years (range, 41-85 years). According to the histological measurement of the maximal tumor invasion beyond the outer border of the muscularis propria, there were 30 patients with pT3a (Figure 1), 24 with pT3b (Figure 2), and five with pT3c. Twenty-seven patients were staged as N0, 22 as N1, and 10 as N2. Fifty-five patients were staged as M0, and four as M1. Forty-four patients had moderately differentiated tumors, and 15 had poorly differentiated ones.

***ADC textural differences between pT3a and pT3b-c stages***

The ADC first-order textural differences between pT3a and pT3b-c rectal adenocarcinomas are shown in Table 2. Skewness was significantly lower in pT3a tumors than in pT3b-c counterparts (0.24 ± 0.31 *vs* 0.41 ± 0.32, *P* = 0.033). ADC value (including mean and percentiles) and ADC histogram related features (including kurtosis and uniformity) were not significantly different between the pT3a and pT3b-c stages. All ADC first-order texture features derived from ADC maps were delineated independently by two radiologists, and showed excellent agreement (ICCs ranging from 0.850 to 0.925).

The obtained ADC second-order textural differences between pT3a and pT3b-c rectal adenocarcinomas are shown in Table 3. Energy (median, 0.782 *vs* 0.640, *P* = 0.038) and entropy (median, 9.831 *vs* 10.805, *P* = 0.001) were significantly different between pT3a and pT3b-c rectal adenocarcinomas. Specifically, energy was higher for pT3a tumors than for pT3b-c ones, while entropy was lower for the pT3a stage than for pT3b-c tumors. All ADC second-order texture features derived from ADC maps were delineated independently by two radiologists, and showed excellent agreement (ICCs ranging from 0.895 to 0.921).

***Diagnostic performance of ADC first- and second-order texture features***

The diagnostic performances of statistically significant ADC first- and second-order texture features and logistic features using ROC analysis to determine the pT3a stage are shown in Table 4. For differentiating pT3a rectal adenocarcinomas from pT3b-c tumors, the AUCs of skewness, energy, and entropy were 0.686, 0.657, and 0.747, respectively. Using a logistic regression model that incorporated all three texture parameters, a moderate accuracy (AUC, 0.775) was achieved, with a sensitivity of 69.0% and specificity of 83.3% (Figure 3). We noted no significant AUC differences while comparing all pairs of texture parameters.

**DISCUSSION**

In this study, we investigated the feasibility of differentiating pT3a rectal adenocarcinomas from pT3b-c tumors using first- and second-order texture features derived from ADC maps. Skewness, energy, and entropy could significantly differentiate pT3a from pT3b-c rectal adenocarcinomas. Logistic regression analysis using all three features demonstrated a higher AUC in differentiating pT3a from pT3b-c tumors. The results indicate that texture features derived from ADC maps might potentially differentiate pT3a from pT3b-c rectal adenocarcinomas.

Statistics-based techniques are the most commonly used methods for TA[27] and contain three orders of features. First-order statistics can be obtained from the histogram of pixel intensity values, including mean intensity, maximum intensity, minimum intensity, standard deviation, uniformity, skewness, and kurtosis. Among second-order statistics, GLCM measurements calculated using spatial gray-level dependence matrices are well known, and these parameters also describe the relationship between neighboring pixels[28,29], including energy, entropy, total frequency, matrix mean, inertia, and correlation. Third-order statistics show the spatial relationships among three or more pixels[28,29]. In this study, ADC histogram features were based on first-order statistics, and GLCM measurements were based on second-order statistics.

In previous studies, the mean ADC values were significantly different among rectal cancers with different pT3 subclasses[23]. In the current study, mean ADC values were not statistically different between pT3a and pT3b-c tumors. Such a discrepancy could result from the methods used for calculating ADC. In the studies by Lu *et al*[11] and Tong *et al*[23], mean ADC values were calculated from three round ROIs that were manually delineated within solid tumor parts. On the contrary, we used whole-tumor VOI, which might better reflect the heterogeneity of the whole tumor[24]. In previous studies by our group[30,31], the 10th percentile ADC from the histogram performed better in differentiating the transition zone cancer from benign prostatic hyperplasia nodule, and was best correlated with the Gleason score of prostate cancer, because the low proportion (*e.g.*, minimum, 10th percentile) ADC from the histogram represents the focal areas of high cellularity under the heterogeneous background[32]. Therefore, we hypothesized that the low proportion of ADC from the histogram could differentiate pT3a rectal adenocarcinomas from pT3b-c tumors. Nevertheless, the results showed that different percentile ADCs from the histogram were not statistically different between pT3a and pT3b-c tumors, suggesting that in rectal cancer, the pT3 stage is possibly more spatially homogeneous. In addition, the relatively small number of patients in the present study might have been a contributing factor.

As shown above, the pT3b-c stage was associated with higher skewness than the pT3a stage. Skewness reflects the asymmetry of pixel distribution. Positive skewness means that the distribution of the histogram has an elongated tail on the right side of the mean[24]. Higher skewness indicates elevated complexity and heterogeneity in tumors. This may be important when interpreting the finding that pT3b-c stage tumors have greater skewness than pT3a ones. The results of the present study were similar to those of Liu *et al*[33]. Moreover, uniformity had a near-significant difference between pT3a and pT3b-c tumors. Uniformity reflects how close the image is to a uniform distribution of gray levels, and high uniformity indicates uniformity in the image and lower heterogeneity[29]. Meng *et al*[34] reported a significant difference in pre-uniformity between advanced patients with rectal cancer that were responders *vs* non-responders in pathologic complete response. The above results revealed that uniformity was potentially advantageous in differentiating pT3a rectal adenocarcinomas from pT3b-c tumors. Hence, future studies will need larger patient cohorts to investigate the differences in uniformity between patients with pT3a and pT3b-c rectal adenocarcinomas.

As for second-order texture features, energy was significantly higher in pT3a rectal adenocarcinomas than in pT3b-c tumors, while entropy was significantly lower. Theoretically, the meaning of energy is similar to that of uniformity. Entropy represents the spatial disorder of the ADC gray-level distribution. Higher entropy and lower energy reflect greater lesional heterogeneity[35,36]. This may be important when interpreting the findings of second-order textural differences between pT3a and pT3b-c tumors. Similar findings have been reported in previous studies. For example, Caruso *et al*[35] observed significantly higher energy in complete responders compared with non-responders to neoadjuvant chemoradiotherapy for colorectal cancer. In studies exploring the value of ADC texture features in characterizing pathologic features of rectal cancer, pT3-4 rectal cancer was significantly higher in entropy in comparison with pT1-2[33,37].

There were several limitations in the present study. First, because of its retrospective design, selection bias was inevitable. Second, the study population was relatively small, and all patients were enrolled in the same hospital, which indicates the low generalizability of the present findings. The low proportion of ADC from the histogram could not significantly differentiate pT3a from pT3b-c tumors, which contradicted previous studies from our group. A future study would benefit from a larger study population. Third, we did not correlate TA with other MRI sequences such as T2WI. High-resolution T2WI plays a pivotal role in the preoperative staging of rectal cancer. Hence, future studies should include T2WI-based TA. Fourth, although gadolinium was used as the contrast agent for MRI, its effect was not examined in this study. Fifth, the study's outcomes only had short-term clinical applicability. Finally, first- and second-order texture features were derived from the DWI datasets, which are sensitive to the applied *b*-values[38]. In designing future studies, the choice of the *b*-value needs to be taken into account.

**CONCLUSION**

Texture features derived from ADC maps, especially skewness, energy, and entropy, might potentially differentiate pT3a rectal adenocarcinomas from pT3b-c tumors. This could have a practical value for the individualized management of rectal cancer patients.

**ARTICLE HIGHLIGHTS**

***Research background***

The accuracy of discriminating pT3a from pT3b-c rectal cancer using high-resolution magnetic resonance imaging remains unsatisfactory. Indeed, the mean and median apparent diffusion coefficient (ADC) values are not always significantly sensitive to small changes or precise status of the tumor owing to the intrinsic chaotic environment of tumors.

***Research motivation***

Texture analysis (TA) could improve the discrimination of pT3a rectal adenocarcinomas from pT3b-c tumors, but pT3 subclasses of rectal cancer have not been previously determined by ADC maps.

***Research objectives***

To investigate the value of TA on ADC maps in differentiating pT3a rectal adenocarcinomas from pT3b-c tumors.

***Research methods***

This case-control study assessed patients with pT3 rectal adenocarcinoma, who underwent DWI between October 2016 and December 2018. First-order (ADC values, skewness, kurtosis, and uniformity) and second-order (energy, entropy, inertia, and correlation) texture features were derived from whole-lesion ADC maps. Receiver operating characteristic (ROC) curves were used to determine the diagnostic value for pT3b-c tumors.

***Research results***

Totally 59 patients (34 men and 25 women) were included, with a median age of 66 years (range, 41-85 years). Thirty patients had pT3a, 24 had pT3b, and five had pT3c. Skewness was significantly lower in the pT3a stage than in pT3b-c tumors. In addition, energy and entropy were significantly different between pT3a rectal adenocarcinomas and pT3b-c tumors. For differentiating pT3a rectal adenocarcinomas from pT3b-c tumors, the areas under the curves (AUCs) of skewness, energy, and entropy were 0.686, 0.657, and 0.747, respectively. Logistic regression analysis of all three features yielded a greater AUC (0.775) in differentiating pT3a rectal adenocarcinomas from pT3b-c tumors (69.0% sensitivity and 83.3% specificity).

***Research conclusions***

TA features derived from ADC maps might potentially differentiate pT3a rectal adenocarcinomas from pT3b-c tumors, especially skewness, energy, and entropy and their combination.

***Research perspectives***

Future studies should include T2WI-based TA, since high-resolution T2WI plays a pivotal role in the preoperative staging of rectal cancer, and *b*-values should also be taken into account. In addition, features with long-term clinical applicability should be assessed. Finally, large multicenter studies are needed to confirm and increase the generalizability of the above findings.

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**Footnotes**

**Institutional review board statement:** This case-control study was approved by the Institutional Review Board of the Changshu Hospital Affiliated to Soochow University (2018 Ethics Audit (Declaration) Batch No. 3).

**Informed consent statement:** The requirement for individual informed consent was waived because of the retrospective design of the study.

**Conflict-of-interest statement:** No benefits in any form have been received or will be received from a commercial party related directly or indirectly to the subject of this article.

**Data sharing statement:** The datasets used and/or analyzed during the current study are available from the corresponding author on reasonable request.

**STROBE statement:** The authors have read the STROBE Statement—checklist of items, and the manuscript was prepared and revised according to the STROBE Statement—checklist of items.

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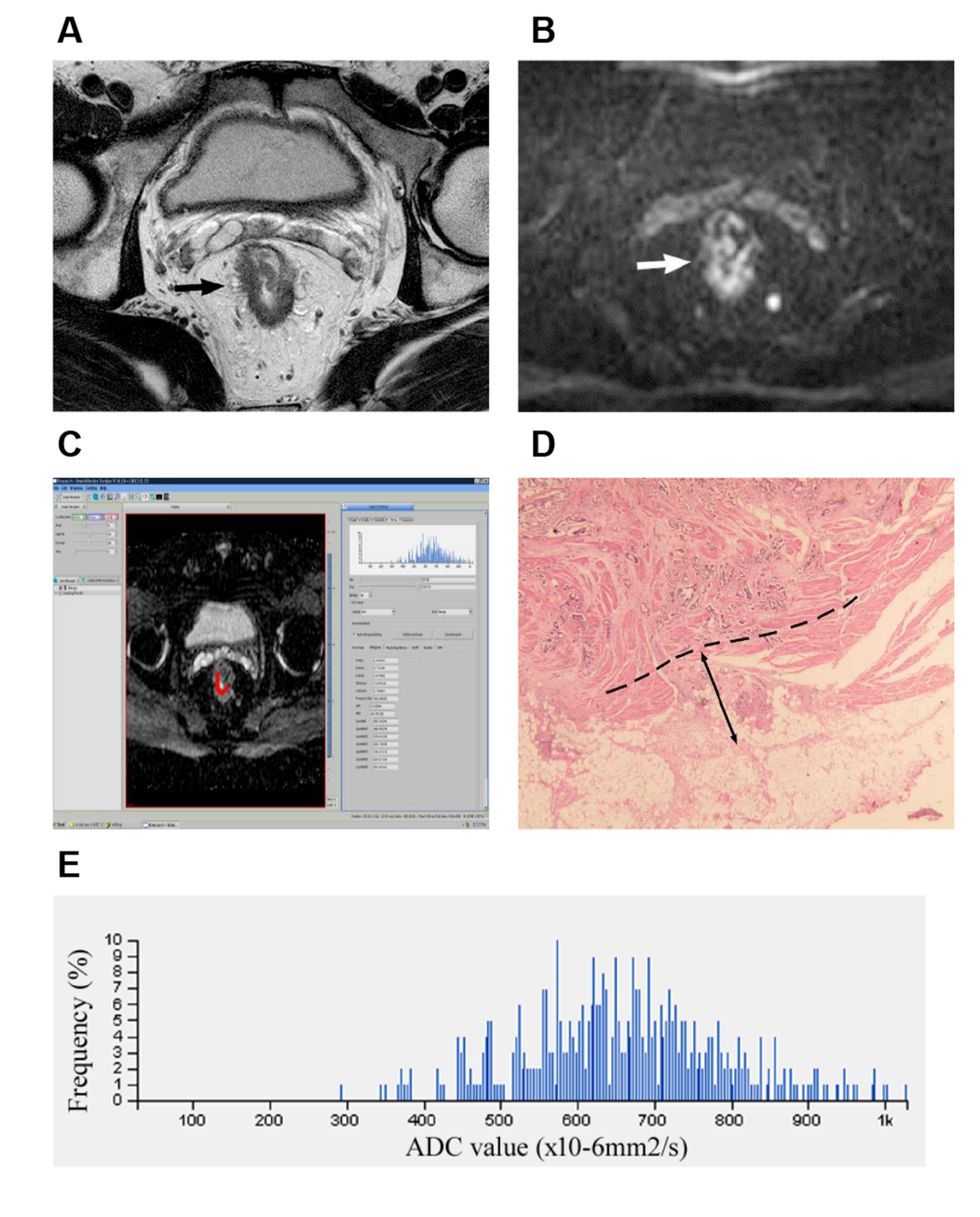
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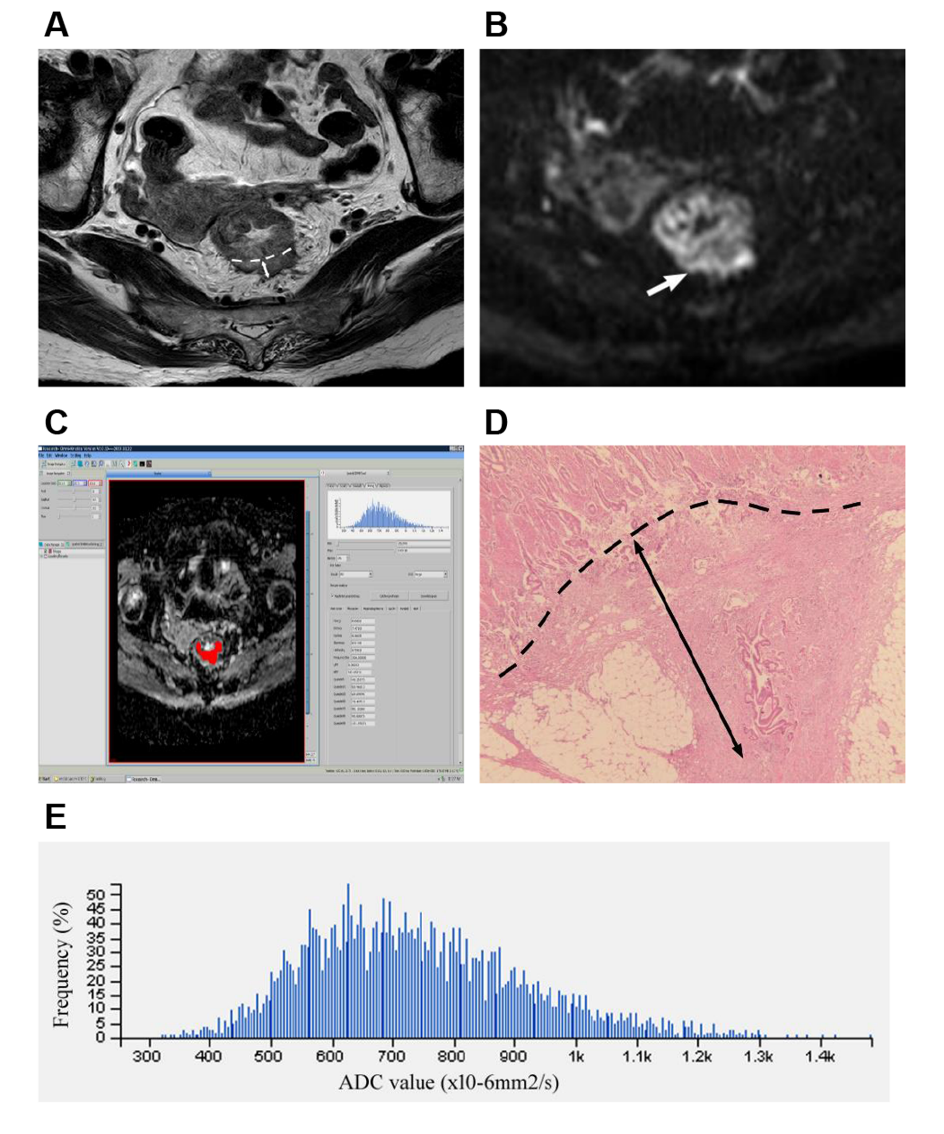
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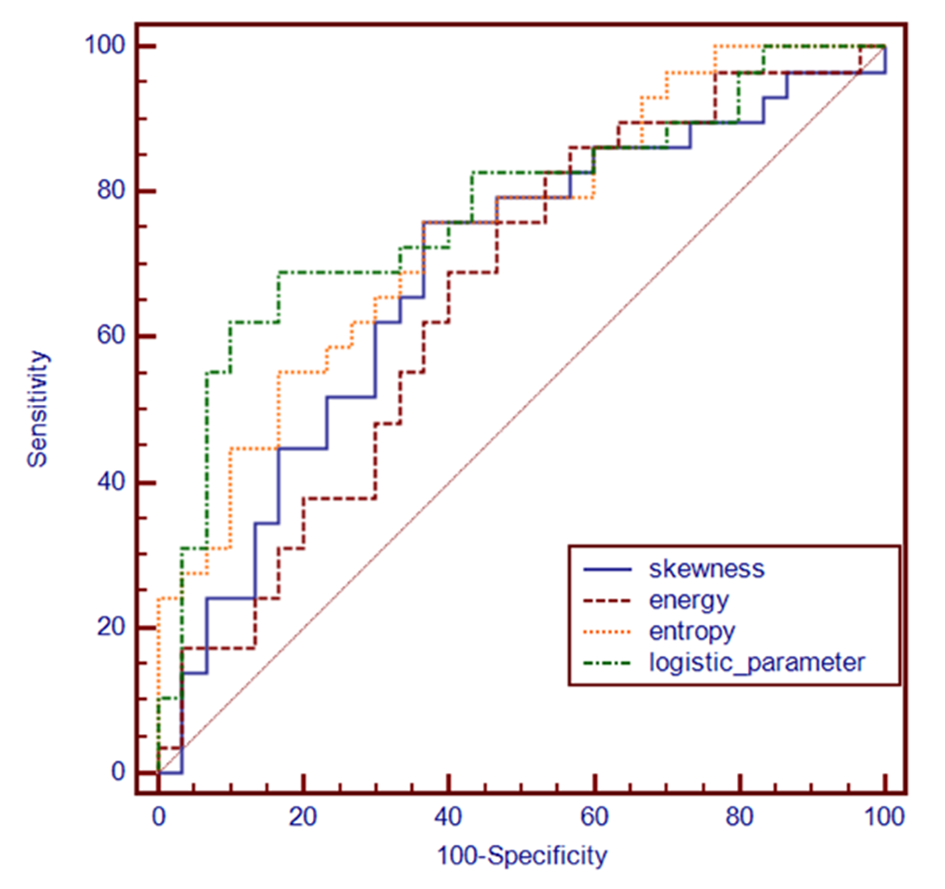
**Figure Legends**



**Figure 1 T3a stage rectal adenocarcinoma.** A: Axial high-resolution T2WI showing that the rectal mass had destroyed the muscularis propria and spread into the mesorectum (black arrow); B: Diffusion-weighted imaging showing an area of high signal intensity with irregular rectal wall margin (white arrow); C: Regions of interest were manually drawn, slice by slice, covering the whole lesion (red area) on the apparent diffusion coefficient (ADC) map; D: Photomicrograph (hematoxylin & eosin staining, magnification × 200) showing that the extramural depth of tumor invasion was 2.5 mm; E: The histogram obtained from the whole lesion on ADC maps provided first-order texture features. ADC: apparent diffusion coefficient.

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**Figure 2 T3b stage rectal adenocarcinoma.** A: Axial high-resolution T2WI showing that the muscularis propria at the 4-6 o’clock direction was destroyed. An imaginary line (dash line) connecting two breakpoints of the muscularis propria layer is shown. The tumor had spread into the mesorectum (white double arrow); B: Diffusion-weighted imaging showing an area of high signal intensity where the tumor invaded the muscularis propria, and the 4-6 o'clock direction of the tumor was the main invasion direction (white arrow); C: Regions of interest were manually drawn, slice by slice, covering the whole lesion (red area) on the apparent diffusion coefficient (ADC) map; D: Photomicrograph (hematoxylin & eosin staining, magnification ×200) showing that the extramural depth of tumor invasion was 7 mm; E: The histogram obtained from the whole lesion on ADC maps provided first-order texture features. ADC: apparent diffusion coefficient.

****

**Figure 3 Receiver operating characteristic curves of four important texture features for calculating the areas under the curves in differentiating pT3a rectal adenocarcinomas from pT3b-c tumors.**

**Table 1 Demographic and pathologic characteristics of patients**

|  |  |
| --- | --- |
| **characteristic** | ***n* = 59** |
| Age (yr), median (IQR) | 66 (58-74) |
| Sex |  |
| Men | 34 (57.6) |
| Women | 25 (42.4) |
| Differentiation grade |  |
| Moderately differentiated | 44 (74.6) |
| Poorly differentiated | 15 (25.4) |
| T3 stage |  |
| T3a | 30 (50.9) |
| T3b | 24 (40.7) |
| T3c | 5 (8.5) |
| N stage |  |
| N0 | 27 (45.8) |
| N1 | 22 (37.3) |
| N2 | 10 (17.0) |
| M stage |  |
| M0 | 55 (93.2) |
| M1 | 4 (6.8) |

Except for age, data are expressed as *n* (%). IQR: interquartile range.

**Table 2 Comparison of apparent diffusion coefficient first-order textural differences between pT3a and pT3b-c stage**

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
| **ADC histogram feature** | **pT3a (*n* = 30)** | **pT3b-c (*n* = 29)** | ***p* value** | **ICC** |
| Mean ADC (× 10-6 mm2/s)1 | 879.5 ± 202.3 | 832.8 ± 166.7 | 0.339 | 0.906 |
| 5th ADC (× 10-6 mm2/s)1 | 584.4 ± 163.3 | 533.1 ± 111.9 | 0.164 | 0.898 |
| 10th ADC (× 10-6 mm2/s)1 | 638.6 ± 164.2 | 589.5 ± 111.0 | 0.183 | 0.901 |
| 25th ADC (× 10-6 mm2/s)1 | 720.2 ± 175.8 | 664.5 ± 125.7 | 0.168 | 0.921 |
| 90th ADC (× 10-6 mm2/s)1 | 1113.8 ± 275.8 | 1055.7 ± 229.3 | 0.383 | 0.850 |
| Skewness1 | 0.24 ± 0.31 | 0.41 ± 0.32 | 0.033 | 0.925 |
| Kurtosis1 | 0.66 ± 0.52 | 0.80 ± 0.70 | 0.376 | 0.909 |
| Uniformity1 | 0.78 ± 0.06 | 0.76 ± 0.05 | 0.058 | 0.921 |

1Independent samples *t*-test, and data are the mean ± SD.

ADC: apparent diffusion coefficient; ICC: intraclass correlation coefficient.

**Table 3 Comparison of apparent diffusion coefficient textural differences between pT3a and pT3b-c stages**

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
| **ADC texture feature** | **pT3a (*n* = 30)** | **pT3b-c (*n* = 29)** | ***P* value** | **ICC** |
| Energy (× 10-3)2 | 0.782 (0.527, 1.399) | 0.640 (0.437, 0.779) | 0.038 | 0.895 |
| Entropy2 | 9.831 (8.969, 10.652) | 10.805 (10.189, 11.592) | 0.001 | 0.920 |
| Inertia1 | 753.0 ± 417.0 | 878.9 ± 279.0 | 0.180 | 0.918 |
| Correlation (× 10-3)2 | 0.538 (0.399, 1.255) | 0.476 (0.414, 0.642) | 0.332 | 0.921 |

1Independent samples *t*-test, and data are the mean ± SD.

2Mann-Whitney *U*-test, and data are the median ± interquartile range.

ADC: apparent diffusion coefficient; ICC: intra-class correlation coefficient.

**Table 4 Diagnostic performances of texture features and logistic feature to discriminate pT3a rectal adenocarcinomas from pT3b-c tumors**

|  |  |  |  |  |  |  |  |  |  |  |  |
| --- | --- | --- | --- | --- | --- | --- | --- | --- | --- | --- | --- |
| **Texture features** | **AUC (95%CI)** | **Sensitivity** | **Specificity** | **+LR** | **-LR** | **+PV** | **-PV** | **Comparison of AUC (*p* value)** | | | |
| **Skewness** | **Energy** | **Entropy** | **Logistic feature** |
| Skewness | 0.686 (0.552-0.801) | 75.9% | 63.3% | 2.07 | 0.38 | 66.7 | 73.1 | — | 0.7469 | 0.4667 | 0.1471 |
| Energy | 0.657 (0.522-0.776) | 86.2% | 43.3% | 1.52 | 0.32 | 59.5 | 76.2 |  | — | 0.0956 | 0.0617 |
| Entropy | 0.747 (0.617-0.851) | 75.9% | 63.3% | 2.07 | 0.38 | 66.7 | 73.1 |  |  | — | 0.3998 |
| Logistic feature | 0.775 (0.647-0.873) | 69.0% | 83.3% | 4.14 | 0.37 | 80.0 | 73.5 |  |  |  | — |

AUC: area under the curve; CI: confidence interval; LR: likelihood ratio; PV: predictive value.



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