**Name of Journal:** *World Journal of Gastroenterology*

**Manuscript NO:** 82557

**Manuscript Type:** REVIEW

**Non-invasive evaluation of liver steatosis with imaging modalities: New techniques and applications**

Zeng KY *et al*. Imaging techniques for liver steatosis

Ke-Yu Zeng, Wu-Yong-Ga Bao, Yun-Han Wang, Min Liao, Jie Yang, Jia-Yan Huang, Qiang Lu

**Ke-Yu Zeng, Wu-Yong-Ga Bao, Yun-Han Wang, Min Liao, Jie Yang, Jia-Yan Huang, Qiang Lu,** Department of Medical Ultrasound, West China Hospital of Sichuan University, Chengdu 610041, Sichuan Province, China

**Author contributions:** Lu Q conceived and designed the protocol; Zeng KY performed the literature search; Bao WYG and Wang YH selected the studies and extracted relevant information; Liao M, Yang J and Huang JY prepared the figures and tables; Zeng KY wrote the first version of draft; Lu Q critically revised successive drafts of the paper and approved the final version.

**Corresponding author: Qiang Lu, MD, Professor,** Department of Medical Ultrasound, West China Hospital of Sichuan University, No. 37 Guoxue Xiang, Chengdu 610041, Sichuan Province, China. luqiang@scu.edu.cn

**Received:** December 23, 2022

**Revised:** February 26, 2023

**Accepted:** April 11, 2023

**Published online:** May 7, 2023

**Abstract**

In the world, nonalcoholic fatty liver disease (NAFLD) accounts for majority of diffuse hepatic diseases. Notably, substantial liver fat accumulation can trigger and accelerate hepatic fibrosis, thus contributing to disease progression. Moreover, the presence of NAFLD not only puts adverse influences for liver but is also associated with an increased risk of type 2 diabetes and cardiovascular diseases. Therefore, early detection and quantified measurement of hepatic fat content are of great importance. Liver biopsy is currently the most accurate method for the evaluation of hepatic steatosis. However, liver biopsy has several limitations, namely, its invasiveness, sampling error, high cost and moderate intraobserver and interobserver reproducibility. Recently, various quantitative imaging techniques have been developed for the diagnosis and quantified measurement of hepatic fat content, including ultrasound- or magnetic resonance-based methods. These quantitative imaging techniques can provide objective continuous metrics associated with liver fat content and be recorded for comparison when patients receive check-ups to evaluate changes in liver fat content, which is useful for longitudinal follow-up. In this review, we introduce several imaging techniques and describe their diagnostic performance for the diagnosis and quantified measurement of hepatic fat content.

**Key Words:** Non-alcoholic fatty liver disease; Hepatic steatosis; Imaging techniques; Quantitative evaluation; Ultrasound; Quantitative ultrasound

**©The** **Author(s) 2023.** Published by Baishideng Publishing Group Inc. All rights reserved.

**Citation:** Zeng KY, Bao WYG, Wang YH, Liao M, Yang J, Huang JY, Lu Q. Non-invasive evaluation of liver steatosis with imaging modalities: New techniques and applications. *World J Gastroenterol* 2023; 29(17): 2534-2550

**URL:** https://www.wjgnet.com/1007-9327/full/v29/i17/2534.htm

**DOI:** https://dx.doi.org/10.3748/wjg.v29.i17.2534

**Core Tip:** Accurate evaluation of the hepatic steatosis is important. The conventional gray scale ultrasound has the limitation of low diagnostic accuracy for mild hepatic steatosis and inability to make quantification evaluations. Quantification imaging techniques including ultrasound-based techniques and magnetic resonance imaging-based techniques can provide objective continuous numbers associated with liver fat content and past records can be found when patients receiving check-ups to evaluate change of liver fat content, which is useful for the longitudinal follow-up to monitor the impact of clinical interventions.

**INTRODUCTION**

There are several types of chronic liver diseases, but nonalcoholic fatty liver disease (NAFLD) is the broadest state[1,2]. NAFLD represents a wide range of liver abnormalities[3]. Over 25% of general population is influenced by NAFLD, while affected proportion of type 2 diabetes population is 55%-80%[1]. Simple fatty liver may progress to non-alcoholic steatohepatitis (NASH), which is a severe form of fatty liver characterized by inflammation of hepatocyte. This form may result in cirrhosis with portal hypertension or liver dysfunction or even to hepatocellular carcinoma (HCC)[4]. Notably, there is an annual incidence of 0.4 cases of HCC per 1000 population-years among patients with NAFLD, making it the third most common cause of HCC in the United States[5]. A diagnosis of NAFLD is associated with not only adverse effects on the liver, but also an increased risk of type 2 diabetes and cardiovascular disease[6,7]. A study suggested that there was a significant increase in mortality associated with liver-specific diseases or cardiovascular diseases in patients with NAFLD compared to controls[8]. For patients who received hepatectomy, hepatic steatosis can increase incidence of postoperative complications and death[9]. The risk of graft failure for patients undergoing liver transplantation increases when hepatic steatosis exceeds 30%[10].

As NAFLD poses substantial risks of HCC, liver-associated complications and other adverse events to patients, it is of great importance to diagnose and quantify hepatic fat content early[4]. NAFLD is likely to be reversible in its early stage even with simple treatments, for example, lifestyle changes[11]. In addition, the main factor contributing to disease progression in patients with NAFLD is liver fibrosis[1,3]. Abundant liver fat accumulation can trigger and accelerate hepatic fibrosis, thus contributing to disease progression[12,13]. Therefore, in patients with NAFLD, quantitative measurements of liver steatosis could be useful for prognostic assessment and treatment[4]. Although high level of liver fat can lead to fibrosis progression, it is of note that the level of liver fat is not always parallel to the grade of fibrosis. It has been suggested that patients without fibrosis or in the early stages of fibrosis may demonstrate obvious disease progression with high level of liver fat content; however, the fat content decreases when disease progresses to advanced fibrosis or cirrhosis[14-16]. Therefore, when evaluating the value of measuring hepatic steatosis for assessing disease progression and prognosis, the fibrosis status should first be taken into account[17].

When it comes to diagnosing diffuse hepatic disease, liver histopathologic examination is the most precise method. With liver biopsy, quantification of the liver fat level is classified into four grades (grade 0, < 5%; grade 1, 5%-33%; grade 2, 33%-66%; grade 3, > 66%)[18]. Although the use of liver biopsy correctly evaluates liver steatosis, its limitations include its invasiveness, sampling error, which make biopsy impractical for patients who have only simple steatosis[19,20]. Therefore, noninvasive methods to diagnose the presence of steatosis and to monitor changes in hepatic steatosis are needed (Table 1). Conventional gray-scale ultrasound can be applied to diagnose liver steatosis. However, its inability to provide accurate quantification of liver fat has limited its use in the diagnostic pathway of liver steatosis[21]. At present, a number of imaging techniques for the evaluation of hepatic fat content, including MR- and ultrasound-based methods, have been developed. In this review, we summarize the available imaging methods for the quantified measurement of hepatic fat content. In addition, we briefly discuss the clinical performance of these methods.

**Ultrasound-based methods to diagnose and quantify hepatic steatosis**

Table 2 summarizes published diagnostic utility metrics and optimal cutoff values of quantitative ultrasound methods for quantified measurement of hepatic fat content.

***Conventional gray scale ultrasound***

Due to its low price and availability, gray scale ultrasound is a traditional diagnostic method for diagnosing and monitoring liver steatosis[22]. When using this method, fatty infiltration is indicated by the following signs: Hyperechogenicity of the liver parenchyma, liver-to-kidney comparison, ultrasound beam attenuation, and impaired visualization of the intrahepatic structures[23]. However, it is difficult for operators to grade liver steatosis solely based on the gray scale ultrasound[24]. Degree of liver fat content can be classified into 4 grades (normal, mild, moderate, and severe)[22]. For moderate to severe hepatic steatosis, gray scale ultrasound has a high diagnostic accuracy. A meta-analysis enrolling a total of 2815 patients and using hepatic histopathologic results as the golden standard demonstrated that the overall sensitivity and specificity of gray scale ultrasound to distinguish normal liver and moderate steatosis were 85% and 93%[25]. However, gray scale ultrasound has restricted diagnostic performance for mild steatosis[24]. Another limitation is that gray scale ultrasound is based on qualitative visual features, and the intraobserver and interobserver reproducibility vary with different operators[26,27].

***Hepatorenal index***

To improve the diagnostic performance of using gray scale ultrasound for the measurement of liver content, hepatorenal index (HRI) was developed[28] (Figure 1). This metric calculates the rate of parenchymal echo of the liver and the renal cortex[28]. Previous studies found that HRI had a significant correlation with histologic steatosis[29-31]. Marshall *et al*[32] reported a sensitivity, confirmed by liver biopsy, of 100% with an HRI cutoff of 1.27 for detecting more than 5% steatosis. Borges *et al*[33] reported for diagnosing fatty liver, the cutoff value of 1.24 revealed 93% sensitivity and specificity, but this study only used healthy volunteers as the control group. Stahlschmidt *et al*[34] suggested in livers with advanced fibrosis, HRI should not be used to measure steatosis because fibrosis replaces fat as NAFLD progresses. Similarly, patients suffering from chronic kidney disease may present increased echo of the renal cortex, which makes the HRI unreliable for grading steatosis[35]. Furthermore, Kjaergaard *et al*[36] found that HRI presented a higher incidence of failure (12%) compared to controlled attenuation parameter (CAP, 2%). In addition, it can be challenging to diagnose mild steatosis by HRI[33].

***Quantitative ultrasound techniques***

**Mechanism of quantitative ultrasound techniques:** Conventional gray scale ultrasound and HRI cannotprovide quantitative information about liver fat content. Essentially, quantitative methods are used to model the relationship between physical properties of hepatic tissue and the echo signals that are scattered by it. The impedance difference of fat vesicles in hepatocytes causes increased scattering magnitudes and signal attenuation. A frequency-dependent analysis of signal attenuation and backscatter is performed on signals returned by tissue[37].

The quantitative ultrasound techniquesused for the measurement of hepatic fat quantification included the spectral-based techniques and the techniques based on envelope statistics. Estimation of either attenuation coefficient (AC) or the backscatter coefficient (BSC) is used for spectral based techniques. The AC measures energy loss as ultrasound wave passes through tissue and the BSC measures the returned ultrasound energy when ultrasound wave strikes the microstructure of tissue. Techniques based on the envelope statistics of the backscattered ultrasound include the acoustic structure quantification (ASQ), normalized local variance (NLV), and estimation of sound speed[38]. Techniques according to envelope statistics are relatively novel. Microstructural characteristics of tissues can be determined by the shape and attributes of backscattered ultrasound[38].

Current commercial techniques and their mechanism of hepatic steatosis quantification are presented in Table 3.

**CAP:** CAP was the initial available technique for quantified measurement of hepatic fat content. Attenuation of the ultrasound beam is applied to generate the CAP amount[39,40]. Typically, two types of probes, the medium probe and the extra-large probe, can be utilized. The choice of optimal probe is automatically controlled according to skin-to-liver capsule distance (SCD). When the SCD exceeds 2.5 cm, the extra-large probe is more effective than the M probe. The CAP is presented in units of decibels per meter (dB/m)[41].

More than 160 studies have discussed the efficacy of CAP as a metric for quantified measurement of liver fat content, and acceptable accuracy was found. The general diagnostic accuracy evaluated by the area under the receiver operating curve (AUROC) of CAP for detecting presence of steatosis has been displayed to range from 0.64 to 0.97[42-44]. A meta-analysis including 19 studies found that CAP had good diagnostic performance with AUROCs of 0.823 for distinguishing steatosis grade > S0, 0.865 for distinguishing steatosis grade > S1, 0.882 for distinguishing steatosis grade > S2. The corresponding optimal cutoff values for > S0, > S1, > S2 were 248, 268 and 280 dB/m. Moreover, they found that there was a potential link between NAFLD, diabetes mellitus, and body mass index with the CAP value[45]. Although the diagnostic utility of CAP for differentiating patients with and without hepatic steatosis has been fully validated, the optimal cutoff value to determine the presence of steatosis varies significantly between studies[17]. A meta-analysis of 2346 participants with different diffused hepatic diseases demonstrated that CAP cutoffs varied according to the etiology of the hepatic diseases, including NAFLD, chronic viral hepatitis, alcoholic liver disease[46].

The CAP value demonstrated a moderate to strong correlation with magnetic resonance (MR)-based techniques for liver steatosis quantification[47,48]. However, compared with MR-based methods, the CAP has inferior diagnostic ability in grading liver steatosis. Diagnostic effectiveness of MR spectroscopy (MRS) over CAP for diagnosing S1 was significantly higher (AUROC, 0.77 *vs* 0.99)[49]. Imajo *et al*[50] demonstrated suboptimal diagnostic performance of CAP compared to MRI-proton density fat fraction (MRI-PDFF) in grading liver steatosis.

However, CAP has the limitation of failure rate up to 7.7%. According to previous reports, an association was found between measurement failure and sex, body mass index, and metabolic syndrome[51]. Use of the extra-large probe can reduce the failure rate because it is designed for patients with obesity[4].

**Quantification of attenuation using ultrasound imaging:** Several techniques aiming to evaluate the attenuation coefficient applying ultrasound guidance have been exploited, including attenuation imaging (ATI), attenuation measurement function (ATT), and ultrasound guided attenuation parameter (UGAP). CAP has a disadvantage that it lacks the guidance of gray scale ultrasound images in choosing the area for measurement. In contrast, the ATI, ATT, and UGAP techniques are characterized by evaluating liver steatosis on gray scale ultrasonography images with accurate placement of region of interest[17]. When using these techniques, conventional gray scale ultrasound images can be evaluated simultaneously, and the exact region of interest can be placed to avoid the vessels, bile duct, masses or cysts. Therefore, the technical success rate using these methods is high[52-55]. Another advantage of ATI, ATT, and UGAP is that these techniques have high intraobserver and interobserver agreement. A range of 0.81 to 0.98 is found for the intraobserver agreement of ATI, and a range of 0.79 to 0.92 is found for the interobserver agreement. Although there are few studies investigating the topic, the intraobserver and interobserver agreement of UGAP is reported to be 0.86 and 0.84, respectively. In addition, ATI measurements among different operators demonstrated high agreement (intraclass correlation coefficients: 0.91)[17,44,56].

ATI is a kind of two-dimensional attenuation imaging technique (Figure 2)[57,58]. ATI assesses the attenuation of ultrasound beams in a region of interest using color-coded maps in real time. dB/cm/MHz is the unit of measurement for the attenuation coefficient[35]. In addition, to ensure a high technique success rate, the ATI is equipped with a reliability index (R2), and an R2 value ≥ 0.80 is considered a reliable measurement[59-61]. In the reported measurements, the cutoff values ranged from 0.63 to 0.69 dB/cm/MHz for detecting ≥ S1, 0.66-0.72 dB/cm/MHz for detecting ≥ S2, and 0.68-0.86 dB/cm/MHz for detecting = S3. The reported AUROCs were 0.80-0.97 for detecting ≥ S1, 0.86-0.99 for detecting ≥ S2, and 0.79-0.99 for detecting = S3[59-70]. It has been found that ATI measurements have a significant correlation with histological steatosis grade determined by liver biopsy[59,60,67]. Additionally, in case where MRI-PDFF was applied as the gold standard, the ATI demonstrated positive correlation with it (*r* = 0.70-0.83)[57,65,66]. The ATI also outperformed the CAP in evaluating the grades of hepatic steatosis. A study including 72 consecutive adult patients found that the AUROC for detecting S0 *vs* S1-S3 of CAP was lower than that of ATI (0.85 *vs* 0.92, respectively)[66].

ATT is a technique developed by Fujifilm Health Care company (previously Hitachi Medical Systems, Japan) (Figure 3). In ATT, a beamline is connected to an ultrasonic transmitter with two ultrasonic waves of different frequencies (F0, F1) at once. The received signal is obtained, and attenuation coefficients are determined by the slope of the received signal ratio (F0/F1). The results are presented in units of dB/cm/MHz[54,55,71-73]. A study enrolled 351 patients and biopsy specimens were examined quantitatively for fat content. In terms of fat area, ATT had a significant correlation (*r* = 0.50, *P* < 0.001). The cutoff values were 0.62 dB/cm/MHz for S ≥ 1, 0.67 dB/cm/MHz for S ≥ 2 and 0.73 dB/cm/MHz for S ≥ 3 and corresponding AUROCs were 0.79, 0.87 and 0.96[54]. An analysis of 94 patients who received both ATT and CAP examinations when undergoing liver histopathologic examination revealed that ATT exhibited diagnostic accuracy equivalent to that of CAP for grading histological steatosis[73].

With known attenuation and BSC, an ultrasound system uses a phantom method to calculate attenuation coefficients measurement implemented in UGAP (Figure 4). Using this method, the US system's transmitting and receiving beamforming characteristics can be compensated. The result is presented in units of dB/cm/MHz[4,74-76]. Several studies reported good diagnostic efficacy of UGAP for liver fat content quantification applying hepatic histological results as the gold standard, and a positive association was found between UGAP and steatosis percentage (correlation coefficient: 0.78-0.81). The reported AUROCs were 0.89-0.92 for detecting steatosis grade ≥ S1, 0.90–0.95 for detecting steatosis grade ≥ S2, and 0.88-0.96 for detecting steatosis grade = S3[75,77-79]. Several other studies compared UGAP with MR-based methods, and a significant correlation between MR-based methods and attenuation coefficient values by UGAP was found (correlation coefficient: 0.72-0.77)[76,80]. Imajo *et al*[76] conducted a multicentric study with 1010 patients and reported that UGAP had good diagnostic efficacy for making quantified measurement of liver fat content. In their study, the AUROCs were 0.910 for detecting MRI-PDFF ≥ 5.2%, 0.912 for MRI-PDFF ≥ 11.3%, and 0.894 for MRI-PDFF ≥17.1%[76]. Fujiwara *et al*[75] reported that as compared to CAP, UGAP achieved significantly higher AUROCs for identifying ≥ S2 (0.950 *vs* 0.841) and ≥ S3 (0.959 *vs* 0.817). In addition, they also reported 5.2% of CAP patients had measurement failures, while no UGAP patients did. Tada *et al*[81] reported that there was no effect of liver stiffness on UGAP attenuation coefficient values.

**Attenuation plane-wave ultrasound:** Attenuation Plane-Wave Ultrasound (Att. PLUS) presents information on ultraphonic beam attenuation through a region of interest. The ultrasound beam attenuation is calculated in a region of interest at a constant depth. The attenuation coefficient results are displayed in units of dB/cm/MHz[56]. The Att. PLUS measurement is combined with the sound speed measurement for each acquisition. It is the median of five measurements taken consecutively that determines the final result[35]. Only one published study regarding this method was found. Popa *et al*[82] carried out a study aiming to assess the clinical value of Att. PLUS of noninvasive measurement of fatty liver with the CAP value considered as control. They reported that the cutoff value to detect S2-S3 was 0.5 dB/cm/MHz (sensitivity 53.1%, specificity 82.0%), and the AUROC was 0.72.

**Tissue attenuation imaging and** **tissue scatter distribution imaging:** Tissue attenuation imaging (TAI) parameter indicates slope of the ultrasound central frequency downshift along depth, which is able to be utilized to calculate acoustic attenuation. The tissue scatter distribution imaging (TSI) parameter is a measurement of the Nakagami parameters in the region of interest, which reflects the concentration of ultrasound scatterers and their arrangement locally[35,83].

We found three studies comparing TAI and TSI with MRI-PDFF, and these studies revealed that both TAI and TSI revealed correlation with MRI-PDFF[84-86]. Jeon *et al*[86] enrolled 120 patients to assess feasibility of TAI and TSI for hepatic steatosis quantification utilizing MRI-PDFF as the reference. According to MRI-PDFF, the participants were classified into three groups (≤ 5%, 5%-10%, and ≥ 10%). They found that both methods had excellent utility for diagnosing and evaluating the degree of hepatic steatosis. For diagnosing fatty quantification of ≥ 5% and ≥ 10%, the AUROCs of TAI were 0.861 and 0.835, and those of TSI were 0.964 and 0.935, respectively[86]. Rónaszéki *et al*[84] compared TAI with TSI utilizing MRI-PDFF as gold standard enrolling 101 participants and found that TAI provided better diagnostic performance than TSI for diagnosing ≥ 5% MRI-PDFF (AUROC: 0.89 *vs* 0.87) and ≥ 10% (AUROC: 0.93 *vs* 0.86). TAI and TSI revealed good intra- and interobserver agreement. In TAI, the intra- and interobserver ICCs were reported at 0.994 and 0.975, respectively, while in TSI, they were reported at 0.991 and 0.947[87].

**Techniques based on ultrasound BSC:** Using the BSC, we can determine amount of ultrasound energy reflected by the tissue. Applying computer algorithm and a reference phantom, the BSC can be estimated with less changeability resulted from ultrasound systems and operators. The right liver lobe was used to obtain gray scale images, and in the same liver region, a continuous series of 10 frames of transducer signals was captured. Then, in the tissue-imitating reference phantom, which mimics the acoustic properties of human hepatic tissue, consecutive frames were noted without changing scanner settings[35,88-90].

The diagnostic accuracy of the BSC has been evaluated by Lin *et al*[91] by analyzing 204 participants. They found that BSC was positively correlated with MRI-PDFF (Spearman’s *ρ* = 0.80; *P* < 0.0001). BSC had an AUROC of 0.98 with a cutoff value of 0.00381/cm-steradian for detecting patients with hepatic steatosis. In addition, when using the optimal BSC cutoff value, in the training group, hepatic steatosis was detected with 93% sensitivity and 97% specificity, while in the validation group, it was detected with 87% sensitivity and 91% specificity[91].

Han *et al*[89,90,92,93] published several studies focusing on the use of the BSC. In a study including 102 participants, they revealed moderate correlation of the BSC with MRI-PDFF (Pearson’s *r* = 0.58, *P* < 0.001)[93]. In addition, they enrolled 41 participants to study the repeatability and reproducibility of BSC and found that ICC were 0.87-0.95 for BSC acquired without participant repositioning and 0.69-0.82 with participant repositioning, suggesting that BSC measurement is repeatable and reproducible in patients with NAFLD[89].

***Ultrasound-derived fat fraction***

The ultrasound-derived fat fraction (UDFF) technique is a coalition of attenuation coefficient and BSC, and a percentage of liver fat content is reported as the result. Data from reference phantoms is integrated into the ultrasound system, and a fixed-acquisition region of interest is utilized[4] (Figure 5). Labyed and Milkowski[37] designed the UDFF method and conducted a study including 101 participants. They found that the UDFF was positively correlated with the MRI-PDFF (Pearson’s *r* = 0.87). Using the histology results as the gold standard, the AUROCs of UDFF were 0.94 for detecting S ≥ 1, 0.88 for S ≥ 2 and 0.83 for S = 3. When using MRI-PDFF to be the gold standard, AUROCs of UDFF were 0.97 for diagnosing MRI-PDFF higher than 5%, 0.95 for diagnosing MRI-PDFF higher than 10%[37]. Similarly, Dillman *et al*[94] reported that liver fat content quantification applying UDFF showed a significant correlation with MRI-PDFF (Spearman’s *ρ* = 0.82; *P* < 0.001).

**ASQ:** Quantifying the acoustic structure of an environment by comparing theoretical and real echo amplitude distributions is referred to as ASQ. In order to compute the theoretical echo amplitude distribution of the hepatic section imaged, the Rayleigh distribution function, assuming that solely ultrasound beam interference from small scattering objects generates the speckle pattern, is applied. However, actual echo amplitude distribution of the liver parenchyma does not follow the Rayleigh distribution. Because ultrasound beams are scattered by small structures, for example the walls of hepatic vessels, resulting in heterogeneity in echo amplitudes[95,96]. However, when diffuse liver diseases cause changes in parenchymal echotexture, ASQ can provide quantitative information by comparing theoretical echo amplitude distribution to a real distribution[97]. Kuroda *et al*[98] tested the ASQ-derived focal disturbance ratio (FD ratio) with 9 Leptin-deficient mice in comparison with histopathological results and found that the FD ratio had significant negative correlations with the fat droplet area (Spearman *r* = -0.72, *P* = 0.0017) and fat droplet size (Spearman *r* = -0.98, *P* = 0.0052), suggesting that the FD ratio can be used to quantify steatosis grade in an animal model and may be a quantitative metric of hepatic steatosis[98]. Karlas *et al*[95] conducted a cohort study to compare ASQ with MRS, and negative correlation was found between FD ratio and MRS (Spearman *r* = -0.43, *P* = 0.004). Similarly, in a prospective study including 36 patients with suspected fatty liver disease, the FD ratio showed a strong, negative correlation with the MRS in 36 patients[99]. Son *et al*[100] also reported FD ratio is comparable to hepatic fat fraction by MRS to make quantified measurement of liver fat content and diagnose liver fat content more than 10% in donor liver patients. Keller *et al*[96] found significant negative correlation between ASQ and steatosis level obtained by histological examination (*r* = -0.55, *P* < 0.0001). Nevertheless, they found no correlation between histologically determined fibrosis stage and any measurements of ASQ.

**NLV:** The NLV is derived from ASQ and analyzes ultrasound amplitudes sampled from grayscale ultrasound images[4,101]. Bae *et al*[102] assessed the clinical value of the NLV in the measurement of liver fat content in comparison with MRS in 40 male mice using histopathology as the golden standard and found that the AUROCs for diagnosing mild, moderate, and severe hepatic steatosis were 0.953, 0.896, and 0.735, and the NLV value performed similarly to MRS in detecting mild or moderate hepatic steatosis. The same authors also conducted a study with 194 patients to assess the diagnostic efficacy of the NLV for diagnosing and grading liver fat content using liver histopathology as the reference standard. They demonstrated the NLV had excellent diagnostic efficacy in detecting and grading fatty liver with AUROCs of 0.911 for ≥ steatosis grade 1, 0.974 for ≥ steatosis grade 2, and 0.954 ≥ steatosis grade 3[103].

**Speed of sound:** A speed of sound (SS) estimation is based on the fact that sound speed varies with fat content in soft tissues, and that the relationship between sound speed and liver fat percentage can be identified[104]. Dioguardi Burgio *et al*[104] carried out a study aiming to explore the value of SS for detecting and quantifying liver steatosis and included 100 patients who underwent both SS and abdominal MR. They found that, in the training cohort, a cut-off value of less than 1.537mm/s led to 87% sensitivity and 95.7% specificity for diagnosing any steatosis with an AUROC of 0.882%. Based on an SS cut-off value of 1.511mm/s, the sensitivity was 100% and specificity was 95.6% for detecting moderate to severe steatosis and the AUROC was 0.989[104].

Sound speed plane-wave ultrasound (SSp.PLUS) is a novel technique for measuring intrahepatic sound speed which is correlated with the liver fat content. The measurement of SSp.PLUS is expressed in m/s[82]. Popa *et al*[82] performed a study with 215 patients to test the value of SSp.PLUS in detecting and grading hepatic fat level applying the CAP value as the gold standard. As a first finding, SSp.PLUS is more closely correlated with CAP values than Att.PLUS: (*r* = -0.74) *vs* (*r* = 0.45). Furthermore, the SSp.PLUS cut-off of less than 1516 m/s indicated 98.36% specificity and 58.74% sensitivity for predicting the presence of significant steatosis (S2-S3)[82].

**CONCLUSION**

Quantification ultrasound techniques can provide objective continuous number associated with liver fat content and past records can be found when patients receiving check-ups to evaluate change of degree of fatty liver, which is useful for follow-up to monitor the impact of any clinical interventions. Besides, as hepatic steatosis may pose adverse effects to prognosis of patients, quantification of liver fat holds clinical significance. For example, substantial hepatic fat accumulation may contribute to rapid disease progression toward NASH or liver fibrosis[105]. Patients with liver resections are more likely to suffer postoperative complications and die due to liver fat accumulation. Compared with patients without steatosis, those with ≤ 30% steatosis have a significantly increased risk of postoperative complications and patients with > 30% steatosis have an increased risk of postoperative death[9,106,107]. It is worth to be mentioned that simple steatosis may lead to poor prognosis. A study carried out in a nationwide Swedish cohort from 1966 to 2017 including 10568 patients found that simple steatosis, non-fibrotic NASH, non-cirrhotic fibrosis, and cirrhosis were associated with significant higher hazard ratio for mortality risk compared with controls. The all-cause mortalities of cohorts with simple steatosis, non-fibrotic NASH, non-cirrhotic fibrosis, and cirrhosis were 2.52% person-years, 3.03% person-years, 3.53% person-years, and 7.05% person-years respectively whereas the mortality of population comparators was 1.69% person-years[108]. Association between imaging quantification method and clinical prognosis is another issue. In patients with chronic hepatitis C, CAP value ≤ 221 dB/m is associated with higher risk of HCC and in patients with NAFLD, CAP value ≤ 265 dB/m is associated with higher risk of HCC[109]. Similarly, in another cross-sectional study including 130 patients (HCC) and 54 patients (chronic hepatitis C), the authors reported that CAP value of chronic hepatitis C group was significantly higher than that of HCC group (259.96 dB/m *vs* 209.57 dB/m, *P* < 0.001)[110].

While serving as the conventional reference standard, liver histopathologic test has the limitations of invasiveness, sampling error, and high cost. Issues including availability, cost, accuracy and reliability should be taken into consideration when choosing the optimal noninvasive methods. The further application of noninvasive methods is desirable for detecting and grading hepatic steatosis at the initial diagnosis and monitoring changes in liver fat content during follow-up after receiving clinical therapies.

MRS and MRI-PDFF are reported to be the most accurate imaging modalities for quantified measurement of liver fat content. However, their low accessibility and high cost make it impossible to use MR-based techniques as repeatable methods to monitor the process of liver steatosis. Therefore, ultrasound-based techniques are more desirable with the advantages of portability and cost-effectiveness. CAP is the first method based on attenuation of the ultrasound beam, and its performance has been validated in several studies. However, the limitations of CAP are nonnegligible in that due to its blindness, it has a high rate of measurement failures because it cannot determine the exact location of the region of interest. UGAP, ATT and ATI have been developed to improve this situation, and these metrics can be used to evaluate degree of fatty liver on gray scale ultrasonography in real-time with a correct region of interest. The CAP measurement also showed suboptimal performance in quantifying liver fat content especially in mild steatosis, which limited its use as a golden standard to evaluate the efficacy of novel imaging methods for liver fat content quantification. In addition, techniques derived from other principles, such as ASQ, TSI and UDFF, have been developed. These techniques are reported to have nice clinical efficacy for liver fat quantification. Nevertheless, studies exploring value of such techniques enrolled a small number of participants. Therefore, future studies enrolling more participants are needed to test the utility of such techniques. Besides, imaging-based techniques may have some limitations. For example, CAP, ATI and MRI-PDFF may be unable to differentiate grade 2 with grade 3 liver steatosis.

Several hepatic steatosis quantification tools are launched by commercial platforms. Larger clinical studies are needed to compare the efficacy among different products. For patients with NAFLD, except for steatosis, inflammation and fibrosis are also significant features which are associated with prognosis. The steatosis measurement is able to be obtained together with the stiffness value by some tools. In this way, comprehensive evaluation of patients with NAFLD can be made. Except for elastography tools, ASQ has also been studied to evaluate liver stiffness. Hepatic steatosis measurement and stiffness measurement, in conjunction with other ultrasound methods, are promising tools for patients with diffuse liver disease to supervise curative effect and disease progression. Developing such a multi-parametric ultrasound modality will require future studies.

**ACKNOWLEDGEMENTS**

We thank all medical staff and technicians who agreed to participate in this review.

**REFERENCES**

1 **Younossi Z**, Anstee QM, Marietti M, Hardy T, Henry L, Eslam M, George J, Bugianesi E. Global burden of NAFLD and NASH: trends, predictions, risk factors and prevention. *Nat Rev Gastroenterol Hepatol* 2018; **15**: 11-20 [PMID: 28930295 DOI: 10.1038/nrgastro.2017.109]

2 **Powell EE**, Wong VW, Rinella M. Non-alcoholic fatty liver disease. *Lancet* 2021; **397**: 2212-2224 [PMID: 33894145 DOI: 10.1016/S0140-6736(20)32511-3]

3 **Chalasani N**, Younossi Z, Lavine JE, Charlton M, Cusi K, Rinella M, Harrison SA, Brunt EM, Sanyal AJ. The diagnosis and management of nonalcoholic fatty liver disease: Practice guidance from the American Association for the Study of Liver Diseases. *Hepatology* 2018; **67**: 328-357 [PMID: 28714183 DOI: 10.1002/hep.29367]

4 **Ferraioli G**, Berzigotti A, Barr RG, Choi BI, Cui XW, Dong Y, Gilja OH, Lee JY, Lee DH, Moriyasu F, Piscaglia F, Sugimoto K, Wong GL, Wong VW, Dietrich CF. Quantification of Liver Fat Content with Ultrasound: A WFUMB Position Paper. *Ultrasound Med Biol* 2021; **47**: 2803-2820 [PMID: 34284932 DOI: 10.1016/j.ultrasmedbio.2021.06.002]

5 **Younossi ZM**, Koenig AB, Abdelatif D, Fazel Y, Henry L, Wymer M. Global epidemiology of nonalcoholic fatty liver disease-Meta-analytic assessment of prevalence, incidence, and outcomes. *Hepatology* 2016; **64**: 73-84 [PMID: 26707365 DOI: 10.1002/hep.28431]

6 **El-Serag HB**, Tran T, Everhart JE. Diabetes increases the risk of chronic liver disease and hepatocellular carcinoma. *Gastroenterology* 2004; **126**: 460-468 [PMID: 14762783 DOI: 10.1053/j.gastro.2003.10.065]

7 **Adams LA**, Lymp JF, St Sauver J, Sanderson SO, Lindor KD, Feldstein A, Angulo P. The natural history of nonalcoholic fatty liver disease: a population-based cohort study. *Gastroenterology* 2005; **129**: 113-121 [PMID: 16012941 DOI: 10.1053/j.gastro.2005.04.014]

8 **Musso G**, Gambino R, Cassader M, Pagano G. Meta-analysis: natural history of non-alcoholic fatty liver disease (NAFLD) and diagnostic accuracy of non-invasive tests for liver disease severity. *Ann Med* 2011; **43**: 617-649 [PMID: 21039302 DOI: 10.3109/07853890.2010.518623]

9 **Leandro G**, Mangia A, Hui J, Fabris P, Rubbia-Brandt L, Colloredo G, Adinolfi LE, Asselah T, Jonsson JR, Smedile A, Terrault N, Pazienza V, Giordani MT, Giostra E, Sonzogni A, Ruggiero G, Marcellin P, Powell EE, George J, Negro F; HCV Meta-Analysis (on) Individual Patients' Data Study Group. Relationship between steatosis, inflammation, and fibrosis in chronic hepatitis C: a meta-analysis of individual patient data. *Gastroenterology* 2006; **130**: 1636-1642 [PMID: 16697727 DOI: 10.1053/j.gastro.2006.03.014]

10 **Linares I**, Hamar M, Selzner N, Selzner M. Steatosis in Liver Transplantation: Current Limitations and Future Strategies. *Transplantation* 2019; **103**: 78-90 [PMID: 30418431 DOI: 10.1097/TP.0000000000002466]

11 **Hossain N**, Kanwar P, Mohanty SR. A Comprehensive Updated Review of Pharmaceutical and Nonpharmaceutical Treatment for NAFLD. *Gastroenterol Res Pract* 2016; **2016**: 7109270 [PMID: 27006654 DOI: 10.1155/2016/7109270]

12 **Ajmera V**, Park CC, Caussy C, Singh S, Hernandez C, Bettencourt R, Hooker J, Sy E, Behling C, Xu R, Middleton MS, Valasek MA, Faulkner C, Rizo E, Richards L, Sirlin CB, Loomba R. Magnetic Resonance Imaging Proton Density Fat Fraction Associates With Progression of Fibrosis in Patients With Nonalcoholic Fatty Liver Disease. *Gastroenterology* 2018; **155**: 307-310.e2 [PMID: 29660324 DOI: 10.1053/j.gastro.2018.04.014]

13 **Stine JG**, Munaganuru N, Barnard A, Wang JL, Kaulback K, Argo CK, Singh S, Fowler KJ, Sirlin CB, Loomba R. Change in MRI-PDFF and Histologic Response in Patients With Nonalcoholic Steatohepatitis: A Systematic Review and Meta-Analysis. *Clin Gastroenterol Hepatol* 2021; **19**: 2274-2283.e5 [PMID: 32882428 DOI: 10.1016/j.cgh.2020.08.061]

14 **Vilar-Gomez E**, Calzadilla-Bertot L, Wai-Sun Wong V, Castellanos M, Aller-de la Fuente R, Metwally M, Eslam M, Gonzalez-Fabian L, Alvarez-Quiñones Sanz M, Conde-Martin AF, De Boer B, McLeod D, Hung Chan AW, Chalasani N, George J, Adams LA, Romero-Gomez M. Fibrosis Severity as a Determinant of Cause-Specific Mortality in Patients With Advanced Nonalcoholic Fatty Liver Disease: A Multi-National Cohort Study. *Gastroenterology* 2018; **155**: 443-457.e17 [PMID: 29733831 DOI: 10.1053/j.gastro.2018.04.034]

15 **Permutt Z**, Le TA, Peterson MR, Seki E, Brenner DA, Sirlin C, Loomba R. Correlation between liver histology and novel magnetic resonance imaging in adult patients with non-alcoholic fatty liver disease - MRI accurately quantifies hepatic steatosis in NAFLD. *Aliment Pharmacol Ther* 2012; **36**: 22-29 [PMID: 22554256 DOI: 10.1111/j.1365-2036.2012.05121.x]

16 **Wildman-Tobriner B**, Middleton MM, Moylan CA, Rossi S, Flores O, Chang ZA, Abdelmalek MF, Sirlin CB, Bashir MR. Association Between Magnetic Resonance Imaging-Proton Density Fat Fraction and Liver Histology Features in Patients With Nonalcoholic Fatty Liver Disease or Nonalcoholic Steatohepatitis. *Gastroenterology* 2018; **155**: 1428-1435.e2 [PMID: 30031769 DOI: 10.1053/j.gastro.2018.07.018]

17 **Tamaki N**, Ajmera V, Loomba R. Non-invasive methods for imaging hepatic steatosis and their clinical importance in NAFLD. *Nat Rev Endocrinol* 2022; **18**: 55-66 [PMID: 34815553 DOI: 10.1038/s41574-021-00584-0]

18 **Kleiner DE**, Brunt EM, Van Natta M, Behling C, Contos MJ, Cummings OW, Ferrell LD, Liu YC, Torbenson MS, Unalp-Arida A, Yeh M, McCullough AJ, Sanyal AJ; Nonalcoholic Steatohepatitis Clinical Research Network. Design and validation of a histological scoring system for nonalcoholic fatty liver disease. *Hepatology* 2005; **41**: 1313-1321 [PMID: 15915461 DOI: 10.1002/hep.20701]

19 **Davison BA**, Harrison SA, Cotter G, Alkhouri N, Sanyal A, Edwards C, Colca JR, Iwashita J, Koch GG, Dittrich HC. Suboptimal reliability of liver biopsy evaluation has implications for randomized clinical trials. *J Hepatol* 2020; **73**: 1322-1332 [PMID: 32610115 DOI: 10.1016/j.jhep.2020.06.025]

20 **Wong VW**, Adams LA, de Lédinghen V, Wong GL, Sookoian S. Noninvasive biomarkers in NAFLD and NASH - current progress and future promise. *Nat Rev Gastroenterol Hepatol* 2018; **15**: 461-478 [PMID: 29844588 DOI: 10.1038/s41575-018-0014-9]

21 **Castera L**, Friedrich-Rust M, Loomba R. Noninvasive Assessment of Liver Disease in Patients With Nonalcoholic Fatty Liver Disease. *Gastroenterology* 2019; **156**: 1264-1281.e4 [PMID: 30660725 DOI: 10.1053/j.gastro.2018.12.036]

22 **Barr RG**. Ultrasound of Diffuse Liver Disease Including Elastography. *Radiol Clin North Am* 2019; **57**: 549-562 [PMID: 30928077 DOI: 10.1016/j.rcl.2019.01.003]

23 **Saadeh S**, Younossi ZM, Remer EM, Gramlich T, Ong JP, Hurley M, Mullen KD, Cooper JN, Sheridan MJ. The utility of radiological imaging in nonalcoholic fatty liver disease. *Gastroenterology* 2002; **123**: 745-750 [PMID: 12198701 DOI: 10.1053/gast.2002.35354]

24 **Dasarathy S**, Dasarathy J, Khiyami A, Joseph R, Lopez R, McCullough AJ. Validity of real time ultrasound in the diagnosis of hepatic steatosis: a prospective study. *J Hepatol* 2009; **51**: 1061-1067 [PMID: 19846234 DOI: 10.1016/j.jhep.2009.09.001]

25 **Hernaez R**, Lazo M, Bonekamp S, Kamel I, Brancati FL, Guallar E, Clark JM. Diagnostic accuracy and reliability of ultrasonography for the detection of fatty liver: a meta-analysis. *Hepatology* 2011; **54**: 1082-1090 [PMID: 21618575 DOI: 10.1002/hep.24452]

26 **Strauss S**, Gavish E, Gottlieb P, Katsnelson L. Interobserver and intraobserver variability in the sonographic assessment of fatty liver. *AJR Am J Roentgenol* 2007; **189**: W320-W323 [PMID: 18029843 DOI: 10.2214/AJR.07.2123]

27 **Cengiz M**, Sentürk S, Cetin B, Bayrak AH, Bilek SU. Sonographic assessment of fatty liver: intraobserver and interobserver variability. *Int J Clin Exp Med* 2014; **7**: 5453-5460 [PMID: 25664055]

28 **Osawa H**, Mori Y. Sonographic diagnosis of fatty liver using a histogram technique that compares liver and renal cortical echo amplitudes. *J Clin Ultrasound* 1996; **24**: 25-29 [PMID: 8655663 DOI: 10.1002/(SICI)1097-0096(199601)24:1<25::AID-JCU4>3.0.CO;2-N]

29 **Mancini M**, Prinster A, Annuzzi G, Liuzzi R, Giacco R, Medagli C, Cremone M, Clemente G, Maurea S, Riccardi G, Rivellese AA, Salvatore M. Sonographic hepatic-renal ratio as indicator of hepatic steatosis: comparison with (1)H magnetic resonance spectroscopy. *Metabolism* 2009; **58**: 1724-1730 [PMID: 19716568 DOI: 10.1016/j.metabol.2009.05.032]

30 **Webb M**, Yeshua H, Zelber-Sagi S, Santo E, Brazowski E, Halpern Z, Oren R. Diagnostic value of a computerized hepatorenal index for sonographic quantification of liver steatosis. *AJR Am J Roentgenol* 2009; **192**: 909-914 [PMID: 19304694 DOI: 10.2214/AJR.07.4016]

31 **Shiralkar K**, Johnson S, Bluth EI, Marshall RH, Dornelles A, Gulotta PM. Improved method for calculating hepatic steatosis using the hepatorenal index. *J Ultrasound Med* 2015; **34**: 1051-1059 [PMID: 26014325 DOI: 10.7863/ultra.34.6.1051]

32 **Marshall RH**, Eissa M, Bluth EI, Gulotta PM, Davis NK. Hepatorenal index as an accurate, simple, and effective tool in screening for steatosis. *AJR Am J Roentgenol* 2012; **199**: 997-1002 [PMID: 23096171 DOI: 10.2214/AJR.11.6677]

33 **Borges VF**, Diniz AL, Cotrim HP, Rocha HL, Andrade NB. Sonographic hepatorenal ratio: a noninvasive method to diagnose nonalcoholic steatosis. *J Clin Ultrasound* 2013; **41**: 18-25 [PMID: 22997020 DOI: 10.1002/jcu.21994]

34 **Stahlschmidt FL**, Tafarel JR, Menini-Stahlschmidt CM, Baena CP. Hepatorenal index for grading liver steatosis with concomitant fibrosis. *PLoS One* 2021; **16**: e0246837 [PMID: 33577616 DOI: 10.1371/journal.pone.0246837]

35 **Bozic D**, Podrug K, Mikolasevic I, Grgurevic I. Ultrasound Methods for the Assessment of Liver Steatosis: A Critical Appraisal. *Diagnostics (Basel)* 2022; **12** [PMID: 36291976 DOI: 10.3390/diagnostics12102287]

36 **Kjaergaard M**, Lindvig KP, Hansen CD, Detlefsen S, Krag A, Thiele M. Hepatorenal Index by B-Mode Ratio Versus Imaging and Fatty Liver Index to Diagnose Steatosis in Alcohol-Related and Nonalcoholic Fatty Liver Disease. *J Ultrasound Med* 2023; **42**: 487-496 [PMID: 35475550 DOI: 10.1002/jum.15991]

37 **Labyed Y**, Milkowski A. Novel Method for Ultrasound-Derived Fat Fraction Using an Integrated Phantom. *J Ultrasound Med* 2020; **39**: 2427-2438 [PMID: 32525261 DOI: 10.1002/jum.15364]

38 **Oelze ML**, Mamou J. Review of Quantitative Ultrasound: Envelope Statistics and Backscatter Coefficient Imaging and Contributions to Diagnostic Ultrasound. *IEEE Trans Ultrason Ferroelectr Freq Control* 2016; **63**: 336-351 [PMID: 26761606 DOI: 10.1109/TUFFC.2015.2513958]

39 **Sasso M**, Beaugrand M, de Ledinghen V, Douvin C, Marcellin P, Poupon R, Sandrin L, Miette V. Controlled attenuation parameter (CAP): a novel VCTE™ guided ultrasonic attenuation measurement for the evaluation of hepatic steatosis: preliminary study and validation in a cohort of patients with chronic liver disease from various causes. *Ultrasound Med Biol* 2010; **36**: 1825-1835 [PMID: 20870345 DOI: 10.1016/j.ultrasmedbio.2010.07.005]

40 **Seneviratne N**, Fang C, Sidhu PS. Ultrasound-based hepatic fat quantification: current status and future directions. *Clin Radiol* 2023; **78**: 187-200 [PMID: 36411088 DOI: 10.1016/j.crad.2022.10.003]

41 **Ferraioli G**, Soares Monteiro LB. Ultrasound-based techniques for the diagnosis of liver steatosis. *World J Gastroenterol* 2019; **25**: 6053-6062 [PMID: 31686762 DOI: 10.3748/wjg.v25.i40.6053]

42 **de Lédinghen V**, Vergniol J, Foucher J, Merrouche W, le Bail B. Non-invasive diagnosis of liver steatosis using controlled attenuation parameter (CAP) and transient elastography. *Liver Int* 2012; **32**: 911-918 [PMID: 22672642 DOI: 10.1111/j.1478-3231.2012.02820.x]

43 **Caussy C**, Brissot J, Singh S, Bassirian S, Hernandez C, Bettencourt R, Rizo E, Richards L, Sirlin CB, Loomba R. Prospective, Same-Day, Direct Comparison of Controlled Attenuation Parameter With the M vs the XL Probe in Patients With Nonalcoholic Fatty Liver Disease, Using Magnetic Resonance Imaging-Proton Density Fat Fraction as the Standard. *Clin Gastroenterol Hepatol* 2020; **18**: 1842-1850.e6 [PMID: 31843596 DOI: 10.1016/j.cgh.2019.11.060]

44 **Park J**, Lee JM, Lee G, Jeon SK, Joo I. Quantitative Evaluation of Hepatic Steatosis Using Advanced Imaging Techniques: Focusing on New Quantitative Ultrasound Techniques. *Korean J Radiol* 2022; **23**: 13-29 [PMID: 34983091 DOI: 10.3348/kjr.2021.0112]

45 **Karlas T**, Petroff D, Sasso M, Fan JG, Mi YQ, de Lédinghen V, Kumar M, Lupsor-Platon M, Han KH, Cardoso AC, Ferraioli G, Chan WK, Wong VW, Myers RP, Chayama K, Friedrich-Rust M, Beaugrand M, Shen F, Hiriart JB, Sarin SK, Badea R, Jung KS, Marcellin P, Filice C, Mahadeva S, Wong GL, Crotty P, Masaki K, Bojunga J, Bedossa P, Keim V, Wiegand J. Individual patient data meta-analysis of controlled attenuation parameter (CAP) technology for assessing steatosis. *J Hepatol* 2017; **66**: 1022-1030 [PMID: 28039099 DOI: 10.1016/j.jhep.2016.12.022]

46 **Petroff D**, Blank V, Newsome PN, Shalimar, Voican CS, Thiele M, de Lédinghen V, Baumeler S, Chan WK, Perlemuter G, Cardoso AC, Aggarwal S, Sasso M, Eddowes PJ, Allison M, Tsochatzis E, Anstee QM, Sheridan D, Cobbold JF, Naveau S, Lupsor-Platon M, Mueller S, Krag A, Irles-Depe M, Semela D, Wong GL, Wong VW, Villela-Nogueira CA, Garg H, Chazouillères O, Wiegand J, Karlas T. Assessment of hepatic steatosis by controlled attenuation parameter using the M and XL probes: an individual patient data meta-analysis. *Lancet Gastroenterol Hepatol* 2021; **6**: 185-198 [PMID: 33460567 DOI: 10.1016/S2468-1253(20)30357-5]

47 **Caussy C**, Alquiraish MH, Nguyen P, Hernandez C, Cepin S, Fortney LE, Ajmera V, Bettencourt R, Collier S, Hooker J, Sy E, Rizo E, Richards L, Sirlin CB, Loomba R. Optimal threshold of controlled attenuation parameter with MRI-PDFF as the gold standard for the detection of hepatic steatosis. *Hepatology* 2018; **67**: 1348-1359 [PMID: 29108123 DOI: 10.1002/hep.29639]

48 **Shao CX**, Ye J, Dong Z, Li F, Lin Y, Liao B, Feng S, Zhong B. Steatosis grading consistency between controlled attenuation parameter and MRI-PDFF in monitoring metabolic associated fatty liver disease. *Ther Adv Chronic Dis* 2021; **12**: 20406223211033119 [PMID: 34408822 DOI: 10.1177/20406223211033119]

49 **Runge JH**, Smits LP, Verheij J, Depla A, Kuiken SD, Baak BC, Nederveen AJ, Beuers U, Stoker J. MR Spectroscopy-derived Proton Density Fat Fraction Is Superior to Controlled Attenuation Parameter for Detecting and Grading Hepatic Steatosis. *Radiology* 2018; **286**: 547-556 [PMID: 28915103 DOI: 10.1148/radiol.2017162931]

50 **Imajo K**, Kessoku T, Honda Y, Tomeno W, Ogawa Y, Mawatari H, Fujita K, Yoneda M, Taguri M, Hyogo H, Sumida Y, Ono M, Eguchi Y, Inoue T, Yamanaka T, Wada K, Saito S, Nakajima A. Magnetic Resonance Imaging More Accurately Classifies Steatosis and Fibrosis in Patients With Nonalcoholic Fatty Liver Disease Than Transient Elastography. *Gastroenterology* 2016; **150**: 626-637.e7 [PMID: 26677985 DOI: 10.1053/j.gastro.2015.11.048]

51 **de Lédinghen V**, Vergniol J, Capdepont M, Chermak F, Hiriart JB, Cassinotto C, Merrouche W, Foucher J, Brigitte le B. Controlled attenuation parameter (CAP) for the diagnosis of steatosis: a prospective study of 5323 examinations. *J Hepatol* 2014; **60**: 1026-1031 [PMID: 24378529 DOI: 10.1016/j.jhep.2013.12.018]

52 **Yoo J**, Lee JM, Joo I, Lee DH, Yoon JH, Kang HJ, Ahn SJ. Reproducibility of ultrasound attenuation imaging for the noninvasive evaluation of hepatic steatosis. *Ultrasonography* 2020; **39**: 121-129 [PMID: 31693842 DOI: 10.14366/usg.19034]

53 **Yuri M**, Nishimura T, Tada T, Yoshida M, Fujiwara A, Kawata S, Yoshihara K, Yoshioka R, Ota S, Nakano R, Yuri Y, Takashima T, Aizawa N, Ikeda N, Shiomi H, Ide YH, Enomoto H, Yasuhiro F, Yano H, Iijima H. Diagnosis of hepatic steatosis based on ultrasound attenuation imaging is not influenced by liver fibrosis. *Hepatol Res* 2022; **52**: 1009-1019 [PMID: 36018852 DOI: 10.1111/hepr.13831]

54 **Tamaki N**, Koizumi Y, Hirooka M, Yada N, Takada H, Nakashima O, Kudo M, Hiasa Y, Izumi N. Novel quantitative assessment system of liver steatosis using a newly developed attenuation measurement method. *Hepatol Res* 2018; **48**: 821-828 [PMID: 29679473 DOI: 10.1111/hepr.13179]

55 **Tamaki N**, Kurosaki M, Yasui Y, Tsuchiya K, Izumi N. Attenuation coefficient (ATT) measurement for liver fat quantification in chronic liver disease. *J Med Ultrason (2001)* 2021; **48**: 481-487 [PMID: 34165645 DOI: 10.1007/s10396-021-01103-4]

56 **Ferraioli G**, Kumar V, Ozturk A, Nam K, de Korte CL, Barr RG. US Attenuation for Liver Fat Quantification: An AIUM-RSNA QIBA Pulse-Echo Quantitative Ultrasound Initiative. *Radiology* 2022; **302**: 495-506 [PMID: 35076304 DOI: 10.1148/radiol.210736]

57 **Kwon EY**, Kim YR, Kang DM, Yoon KH, Lee YH. Usefulness of US attenuation imaging for the detection and severity grading of hepatic steatosis in routine abdominal ultrasonography. *Clin Imaging* 2021; **76**: 53-59 [PMID: 33549920 DOI: 10.1016/j.clinimag.2021.01.034]

58 **Jang JK**, Kim SY, Yoo IW, Cho YB, Kang HJ, Lee DH. Diagnostic performance of ultrasound attenuation imaging for assessing low-grade hepatic steatosis. *Eur Radiol* 2022; **32**: 2070-2077 [PMID: 34549325 DOI: 10.1007/s00330-021-08269-y]

59 **Bae JS**, Lee DH, Lee JY, Kim H, Yu SJ, Lee JH, Cho EJ, Lee YB, Han JK, Choi BI. Assessment of hepatic steatosis by using attenuation imaging: a quantitative, easy-to-perform ultrasound technique. *Eur Radiol* 2019; **29**: 6499-6507 [PMID: 31175413 DOI: 10.1007/s00330-019-06272-y]

60 **Bae JS**, Lee DH, Suh KS, Kim H, Lee KB, Lee JY, Han JK. Noninvasive assessment of hepatic steatosis using a pathologic reference standard: comparison of CT, MRI, and US-based techniques. *Ultrasonography* 2022; **41**: 344-354 [PMID: 34852424 DOI: 10.14366/usg.21150]

61 **Jeon SK**, Lee JM, Joo I, Yoon JH, Lee DH, Lee JY, Han JK. Prospective Evaluation of Hepatic Steatosis Using Ultrasound Attenuation Imaging in Patients with Chronic Liver Disease with Magnetic Resonance Imaging Proton Density Fat Fraction as the Reference Standard. *Ultrasound Med Biol* 2019; **45**: 1407-1416 [PMID: 30975533 DOI: 10.1016/j.ultrasmedbio.2019.02.008]

62 **Tada T**, Iijima H, Kobayashi N, Yoshida M, Nishimura T, Kumada T, Kondo R, Yano H, Kage M, Nakano C, Aoki T, Aizawa N, Ikeda N, Takashima T, Yuri Y, Ishii N, Hasegawa K, Takata R, Yoh K, Sakai Y, Nishikawa H, Iwata Y, Enomoto H, Hirota S, Fujimoto J, Nishiguchi S. Usefulness of Attenuation Imaging with an Ultrasound Scanner for the Evaluation of Hepatic Steatosis. *Ultrasound Med Biol* 2019; **45**: 2679-2687 [PMID: 31277922 DOI: 10.1016/j.ultrasmedbio.2019.05.033]

63 **Tada T**, Kumada T, Toyoda H, Nakamura S, Shibata Y, Yasuda S, Watanuki Y, Tsujii K, Fukuda N, Fujioka M, Takeshima K, Niwa F, Ogawa S, Hashinokuchi S, Kataoka S, Ichikawa H, Iijima H. Attenuation imaging based on ultrasound technology for assessment of hepatic steatosis: A comparison with magnetic resonance imaging-determined proton density fat fraction. *Hepatol Res* 2020; **50**: 1319-1327 [PMID: 32876367 DOI: 10.1111/hepr.13563]

64 **Jeon SK**, Lee JM, Joo I, Yoon JH. Assessment of the inter-platform reproducibility of ultrasound attenuation examination in nonalcoholic fatty liver disease. *Ultrasonography* 2022; **41**: 355-364 [PMID: 34933319 DOI: 10.14366/usg.21167]

65 **Ferraioli G**, Maiocchi L, Raciti MV, Tinelli C, De Silvestri A, Nichetti M, De Cata P, Rondanelli M, Chiovato L, Calliada F, Filice C. Detection of Liver Steatosis With a Novel Ultrasound-Based Technique: A Pilot Study Using MRI-Derived Proton Density Fat Fraction as the Gold Standard. *Clin Transl Gastroenterol* 2019; **10**: e00081 [PMID: 31609745 DOI: 10.14309/ctg.0000000000000081]

66 **Ferraioli G**, Maiocchi L, Savietto G, Tinelli C, Nichetti M, Rondanelli M, Calliada F, Preda L, Filice C. Performance of the Attenuation Imaging Technology in the Detection of Liver Steatosis. *J Ultrasound Med* 2021; **40**: 1325-1332 [PMID: 32960457 DOI: 10.1002/jum.15512]

67 **Sugimoto K**, Abe M, Oshiro H, Takahashi H, Kakegawa T, Tomita Y, Yoshimasu Y, Takeuchi H, Itoi T. The most appropriate region-of-interest position for attenuation coefficient measurement in the evaluation of liver steatosis. *J Med Ultrason (2001)* 2021; **48**: 615-621 [PMID: 34453648 DOI: 10.1007/s10396-021-01124-z]

68 **Lee DH**. Quantitative assessment of fatty liver using ultrasound attenuation imaging. *J Med Ultrason (2001)* 2021; **48**: 465-470 [PMID: 34453237 DOI: 10.1007/s10396-021-01132-z]

69 **Hsu PK**, Wu LS, Su WW, Su PY, Chen YY, Hsu YC, Yen HH, Wu CL. Comparing the controlled attenuation parameter using FibroScan and attenuation imaging with ultrasound as a novel measurement for liver steatosis. *PLoS One* 2021; **16**: e0254892 [PMID: 34653177 DOI: 10.1371/journal.pone.0254892]

70 **Hsu PK**, Wu LS, Yen HH, Huang HP, Chen YY, Su PY, Su WW. Attenuation Imaging with Ultrasound as a Novel Evaluation Method for Liver Steatosis. *J Clin Med* 2021; **10** [PMID: 33801163 DOI: 10.3390/jcm10050965]

71 **Cerit M**, Şendur HN, Cindil E, Erbaş G, Yalçın MM, Cerit ET, Allahverdiyeva S, Oktar SÖ, Yücel C. Quantification of liver fat content with ultrasonographic attenuation measurement function: Correlation with unenhanced multidimensional computerized tomography. *Clin Imaging* 2020; **65**: 85-93 [PMID: 32387801 DOI: 10.1016/j.clinimag.2020.04.028]

72 **Ferraioli G**, Raimondi A, Maiocchi L, De Silvestri A, Filice C. Quantification of Liver Fat Content with the iATT Algorithm: Correlation with Controlled Attenuation Parameter. *Diagnostics (Basel)* 2022; **12** [PMID: 35892497 DOI: 10.3390/diagnostics12081787]

73 **Koizumi Y**, Hirooka M, Tamaki N, Yada N, Nakashima O, Izumi N, Kudo M, Hiasa Y. New diagnostic technique to evaluate hepatic steatosis using the attenuation coefficient on ultrasound B mode. *PLoS One* 2019; **14**: e0221548 [PMID: 31454369 DOI: 10.1371/journal.pone.0221548]

74 **Bende F**, Sporea I, Șirli R, Bâldea V, Lazăr A, Lupușoru R, Fofiu R, Popescu A. Ultrasound-Guided Attenuation Parameter (UGAP) for the quantification of liver steatosis using the Controlled Attenuation Parameter (CAP) as the reference method. *Med Ultrason* 2021; **23**: 7-14 [PMID: 33220028 DOI: 10.11152/mu-2688]

75 **Fujiwara Y**, Kuroda H, Abe T, Ishida K, Oguri T, Noguchi S, Sugai T, Kamiyama N, Takikawa Y. The B-Mode Image-Guided Ultrasound Attenuation Parameter Accurately Detects Hepatic Steatosis in Chronic Liver Disease. *Ultrasound Med Biol* 2018; **44**: 2223-2232 [PMID: 30077415 DOI: 10.1016/j.ultrasmedbio.2018.06.017]

76 **Imajo K**, Toyoda H, Yasuda S, Suzuki Y, Sugimoto K, Kuroda H, Akita T, Tanaka J, Yasui Y, Tamaki N, Kurosaki M, Izumi N, Nakajima A, Kumada T. Utility of Ultrasound-Guided Attenuation Parameter for Grading Steatosis With Reference to MRI-PDFF in a Large Cohort. *Clin Gastroenterol Hepatol* 2022; **20**: 2533-2541.e7 [PMID: 34768008 DOI: 10.1016/j.cgh.2021.11.003]

77 **Ogino Y**, Wakui N, Nagai H, Igarashi Y. The ultrasound-guided attenuation parameter is useful in quantification of hepatic steatosis in non-alcoholic fatty liver disease. *JGH Open* 2021; **5**: 947-952 [PMID: 34386604 DOI: 10.1002/jgh3.12615]

78 **Kuroda H**, Abe T, Fujiwara Y, Nagasawa T, Takikawa Y. Diagnostic accuracy of ultrasound-guided attenuation parameter as a noninvasive test for steatosis in non-alcoholic fatty liver disease. *J Med Ultrason (2001)* 2021; **48**: 471-480 [PMID: 34415481 DOI: 10.1007/s10396-021-01123-0]

79 **Kuroda H**, Fujiwara Y, Abe T, Nagasawa T, Oguri T, Noguchi S, Kamiyama N, Takikawa Y. Two-dimensional shear wave elastography and ultrasound-guided attenuation parameter for progressive non-alcoholic steatohepatitis. *PLoS One* 2021; **16**: e0249493 [PMID: 33826669 DOI: 10.1371/journal.pone.0249493]

80 **Tada T**, Kumada T, Toyoda H, Kobayashi N, Sone Y, Oguri T, Kamiyama N. Utility of Attenuation Coefficient Measurement Using an Ultrasound-Guided Attenuation Parameter for Evaluation of Hepatic Steatosis: Comparison With MRI-Determined Proton Density Fat Fraction. *AJR Am J Roentgenol* 2019; **212**: 332-341 [PMID: 30476453 DOI: 10.2214/AJR.18.20123]

81 **Tada T**, Kumada T, Toyoda H, Yasuda S, Sone Y, Hashinokuchi S, Ogawa S, Oguri T, Kamiyama N, Chuma M, Akita T, Tanaka J. Liver stiffness does not affect ultrasound-guided attenuation coefficient measurement in the evaluation of hepatic steatosis. *Hepatol Res* 2020; **50**: 190-198 [PMID: 31661724 DOI: 10.1111/hepr.13442]

82 **Popa A**, Bende F, Șirli R, Popescu A, Bâldea V, Lupușoru R, Cotrău R, Fofiu R, Foncea C, Sporea I. Quantification of Liver Fibrosis, Steatosis, and Viscosity Using Multiparametric Ultrasound in Patients with Non-Alcoholic Liver Disease: A "Real-Life" Cohort Study. *Diagnostics (Basel)* 2021; **11** [PMID: 33926073 DOI: 10.3390/diagnostics11050783]

83 **Jeon SK**, Lee JM, Joo I. Clinical Feasibility of Quantitative Ultrasound Imaging for Suspected Hepatic Steatosis: Intra- and Inter-examiner Reliability and Correlation with Controlled Attenuation Parameter. *Ultrasound Med Biol* 2021; **47**: 438-445 [PMID: 33277108 DOI: 10.1016/j.ultrasmedbio.2020.11.009]

84 **Rónaszéki AD**, Budai BK, Csongrády B, Stollmayer R, Hagymási K, Werling K, Fodor T, Folhoffer A, Kalina I, Győri G, Maurovich-Horvat P, Kaposi PN. Tissue attenuation imaging and tissue scatter imaging for quantitative ultrasound evaluation of hepatic steatosis. *Medicine (Baltimore)* 2022; **101**: e29708 [PMID: 35984128 DOI: 10.1097/MD.0000000000029708]

85 **Şendur HN**, Özdemir Kalkan D, Cerit MN, Kalkan G, Şendur AB, Özhan Oktar S. Hepatic Fat Quantification With Novel Ultrasound Based Techniques: A Diagnostic Performance Study Using Magnetic Resonance Imaging Proton Density Fat Fraction as Reference Standard. *Can Assoc Radiol J* 2023; **74**: 362-369 [PMID: 36113064 DOI: 10.1177/08465371221123696]

86 **Jeon SK**, Lee JM, Joo I, Park SJ. Quantitative Ultrasound Radiofrequency Data Analysis for the Assessment of Hepatic Steatosis in Nonalcoholic Fatty Liver Disease Using Magnetic Resonance Imaging Proton Density Fat Fraction as the Reference Standard. *Korean J Radiol* 2021; **22**: 1077-1086 [PMID: 33739636 DOI: 10.3348/kjr.2020.1262]

87 **Şendur HN**, Cerit MN, Ibrahimkhanli N, Şendur AB, Özhan Oktar S. Interobserver Variability in Ultrasound-Based Liver Fat Quantification. *J Ultrasound Med* 2023; **42**: 833-841 [PMID: 35778902 DOI: 10.1002/jum.16048]

88 **Coila A**, Oelze ML. Effects of acoustic nonlinearities on the ultrasonic backscatter coefficient estimation. *J Acoust Soc Am* 2019; **146**: 85 [PMID: 31370607 DOI: 10.1121/1.5115355]

89 **Han A**, Andre MP, Deiranieh L, Housman E, Erdman JW Jr, Loomba R, Sirlin CB, O'Brien WD Jr. Repeatability and Reproducibility of the Ultrasonic Attenuation Coefficient and Backscatter Coefficient Measured in the Right Lobe of the Liver in Adults With Known or Suspected Nonalcoholic Fatty Liver Disease. *J Ultrasound Med* 2018; **37**: 1913-1927 [PMID: 29359454 DOI: 10.1002/jum.14537]

90 **Han A**, Zhang YN, Boehringer AS, Andre MP, Erdman JW Jr, Loomba R, Sirlin CB, O'Brien WD Jr. Inter-platform reproducibility of ultrasonic attenuation and backscatter coefficients in assessing NAFLD. *Eur Radiol* 2019; **29**: 4699-4708 [PMID: 30783789 DOI: 10.1007/s00330-019-06035-9]

91 **Lin SC**, Heba E, Wolfson T, Ang B, Gamst A, Han A, Erdman JW Jr, O'Brien WD Jr, Andre MP, Sirlin CB, Loomba R. Noninvasive Diagnosis of Nonalcoholic Fatty Liver Disease and Quantification of Liver Fat Using a New Quantitative Ultrasound Technique. *Clin Gastroenterol Hepatol* 2015; **13**: 1337-1345.e6 [PMID: 25478922 DOI: 10.1016/j.cgh.2014.11.027]

92 **Han A**, Labyed Y, Sy EZ, Boehringer AS, Andre MP, Erdman JW Jr, Loomba R, Sirlin CB, O'Brien WD Jr. Inter-sonographer reproducibility of quantitative ultrasound outcomes and shear wave speed measured in the right lobe of the liver in adults with known or suspected non-alcoholic fatty liver disease. *Eur Radiol* 2018; **28**: 4992-5000 [PMID: 29869170 DOI: 10.1007/s00330-018-5541-9]

93 **Han A**, Zhang YN, Boehringer AS, Montes V, Andre MP, Erdman JW Jr, Loomba R, Valasek MA, Sirlin CB, O'Brien WD Jr. Assessment of Hepatic Steatosis in Nonalcoholic Fatty Liver Disease by Using Quantitative US. *Radiology* 2020; **295**: 106-113 [PMID: 32013792 DOI: 10.1148/radiol.2020191152]

94 **Dillman JR**, Thapaliya S, Tkach JA, Trout AT. Quantification of Hepatic Steatosis by Ultrasound: Prospective Comparison With MRI Proton Density Fat Fraction as Reference Standard. *AJR Am J Roentgenol* 2022; **219**: 784-791 [PMID: 35674351 DOI: 10.2214/AJR.22.27878]

95 **Karlas T**, Berger J, Garnov N, Lindner F, Busse H, Linder N, Schaudinn A, Relke B, Chakaroun R, Tröltzsch M, Wiegand J, Keim V. Estimating steatosis and fibrosis: Comparison of acoustic structure quantification with established techniques. *World J Gastroenterol* 2015; **21**: 4894-4902 [PMID: 25945002 DOI: 10.3748/wjg.v21.i16.4894]

96 **Keller J**, Kaltenbach TE, Haenle MM, Oeztuerk S, Graeter T, Mason RA, Seufferlein T, Kratzer W. Comparison of Acoustic Structure Quantification (ASQ), shearwave elastography and histology in patients with diffuse hepatopathies. *BMC Med Imaging* 2015; **15**: 58 [PMID: 26637242 DOI: 10.1186/s12880-015-0100-1]

97 **Lin YH**, Wan YL, Tai DI, Tseng JH, Wang CY, Tsai YW, Lin YR, Chang TY, Tsui PH. Considerations of Ultrasound Scanning Approaches in Non-alcoholic Fatty Liver Disease Assessment through Acoustic Structure Quantification. *Ultrasound Med Biol* 2019; **45**: 1955-1969 [PMID: 31130411 DOI: 10.1016/j.ultrasmedbio.2019.04.018]

98 **Kuroda H**, Kakisaka K, Kamiyama N, Oikawa T, Onodera M, Sawara K, Oikawa K, Endo R, Takikawa Y, Suzuki K. Non-invasive determination of hepatic steatosis by acoustic structure quantification from ultrasound echo amplitude. *World J Gastroenterol* 2012; **18**: 3889-3895 [PMID: 22876042 DOI: 10.3748/wjg.v18.i29.3889]

99 **Lee DH**, Lee JY, Park MS, Han JK. Non-invasive monitoring of hepatic steatosis via acoustic structure quantification of ultrasonography with MR spectroscopy as the reference standard. *Ultrasonography* 2020; **39**: 70-78 [PMID: 31639886 DOI: 10.14366/usg.19002]

100 **Son JY**, Lee JY, Yi NJ, Lee KW, Suh KS, Kim KG, Lee JM, Han JK, Choi BI. Hepatic Steatosis: Assessment with Acoustic Structure Quantification of US Imaging. *Radiology* 2016; **278**: 257-264 [PMID: 26121121 DOI: 10.1148/radiol.2015141779]

101 **Zhao Y**, Zhang C, Xu S, Zhang H, Wei S, Huang P, Zhang L, Wong YN, Xu W, Huang P. Quantitative evaluation of hepatic steatosis using novel ultrasound technology normalized local variance (NLV) and its standard deviation with different ROIs in patients with metabolic-associated fatty liver disease: a pilot study. *Abdom Radiol (NY)* 2022; **47**: 693-703 [PMID: 34958409 DOI: 10.1007/s00261-021-03394-0]

102 **Bae JS**, Lee JY, Lee DH, Kim H, Lee Y, Han JK. Quantitative Evaluation of Hepatic Steatosis Using Normalized Local Variance in a Rat Model: Comparison with Histopathology as the Reference Standard. *Korean J Radiol* 2019; **20**: 1399-1407 [PMID: 31464118 DOI: 10.3348/kjr.2019.0068]

103 **Bae JS**, Lee DH, Lee JY, Kim H, Yu SJ, Lee JH, Cho EJ, Lee YB, Han JK, Choi BI. Quantitative Assessment of Fatty Liver using Ultrasound with Normalized Local Variance Technique. *Ultraschall Med* 2021; **42**: 599-606 [PMID: 32323278 DOI: 10.1055/a-1143-3091]

104 **Dioguardi Burgio M**, Imbault M, Ronot M, Faccinetto A, Van Beers BE, Rautou PE, Castera L, Gennisson JL, Tanter M, Vilgrain V. Ultrasonic Adaptive Sound Speed Estimation for the Diagnosis and Quantification of Hepatic Steatosis: A Pilot Study. *Ultraschall Med* 2019; **40**: 722-733 [PMID: 30396216 DOI: 10.1055/a-0660-9465]

105 **Suliman I**, Abdelgelil N, Kassamali F, Hassanein TI. The Effects of Hepatic Steatosis on the Natural History of HBV Infection. *Clin Liver Dis* 2019; **23**: 433-450 [PMID: 31266618 DOI: 10.1016/j.cld.2019.05.001]

106 **Abdalla EK**, Vauthey JN. Steatosis as a risk factor in liver surgery. *Ann Surg* 2007; **246**: 340-1; author reply 341 [PMID: 17667519 DOI: 10.1097/SLA.0b013e31811ea9d2]

107 **Spitzer AL**, Lao OB, Dick AA, Bakthavatsalam R, Halldorson JB, Yeh MM, Upton MP, Reyes JD, Perkins JD. The biopsied donor liver: incorporating macrosteatosis into high-risk donor assessment. *Liver Transpl* 2010; **16**: 874-884 [PMID: 20583086 DOI: 10.1002/lt.22085]

108 **Simon TG**, Roelstraete B, Khalili H, Hagström H, Ludvigsson JF. Mortality in biopsy-confirmed nonalcoholic fatty liver disease: results from a nationwide cohort. *Gut* 2021; **70**: 1375-1382 [PMID: 33037056 DOI: 10.1136/gutjnl-2020-322786]

109 **Izumi T**, Sho T, Morikawa K, Shigesawa T, Suzuki K, Nakamura A, Ohara M, Kawagishi N, Umemura M, Shimazaki T, Kimura M, Nakai M, Suda G, Natsuizaka M, Ogawa K, Kudo Y, Nishida M, Ono K, Baba M, Furuya K, Sakamoto N. Assessing the risk of hepatocellular carcinoma by combining liver stiffness and the controlled attenuation parameter. *Hepatol Res* 2019; **49**: 1207-1217 [PMID: 31219667 DOI: 10.1111/hepr.13391]

110 **Abdelaziz AO**, Shousha HI, Said EM, Soliman ZA, Shehata AA, Nabil MM, Abdelmaksoud AH, Elbaz TM, Abdelsalam FM. Evaluation of liver steatosis, measured by controlled attenuation parameter, in patients with hepatitis C-induced advanced liver fibrosis and hepatocellular carcinoma. *Eur J Gastroenterol Hepatol* 2018; **30**: 1384-1388 [PMID: 30179227 DOI: 10.1097/MEG.0000000000001196]

**Footnotes**

**Conflict-of-interest statement:** The authors have no financial relationships to disclose.

**Open-Access:** This article is an open-access article that was selected by an in-house editor and fully peer-reviewed by external reviewers. It is distributed in accordance with the Creative Commons Attribution NonCommercial (CC BY-NC 4.0) license, which permits others to distribute, remix, adapt, build upon this work non-commercially, and license their derivative works on different terms, provided the original work is properly cited and the use is non-commercial. See: https://creativecommons.org/Licenses/by-nc/4.0/

**Provenance and peer review:** Invited article; Externally peer reviewed.

**Peer-review model:** Single blind

**Peer-review started:** December 23, 2022

**First decision:** February 16, 2023

**Article in press:** April 11, 2023

**Specialty type:** Gastroenterology and hepatology

**Country/Territory of origin:** China

**Peer-review report’s scientific quality classification**

Grade A (Excellent): A, A

Grade B (Very good): B, B

Grade C (Good): C

Grade D (Fair): 0

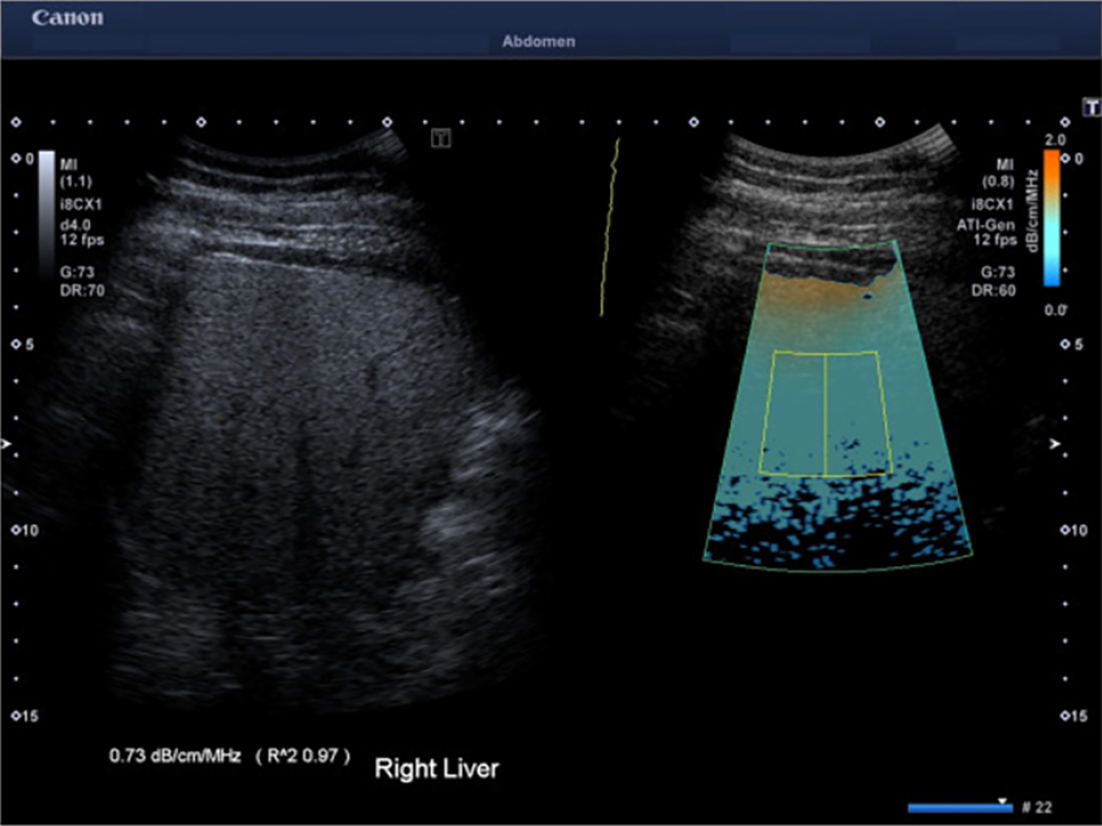
Grade E (Poor): 0

**P-Reviewer:** Losurdo G, Italy; Tai DI, Taiwan; Uhlmann D, Germany **S-Editor:** Yan JP **L-Editor:** A **P-Editor:** Zhao S

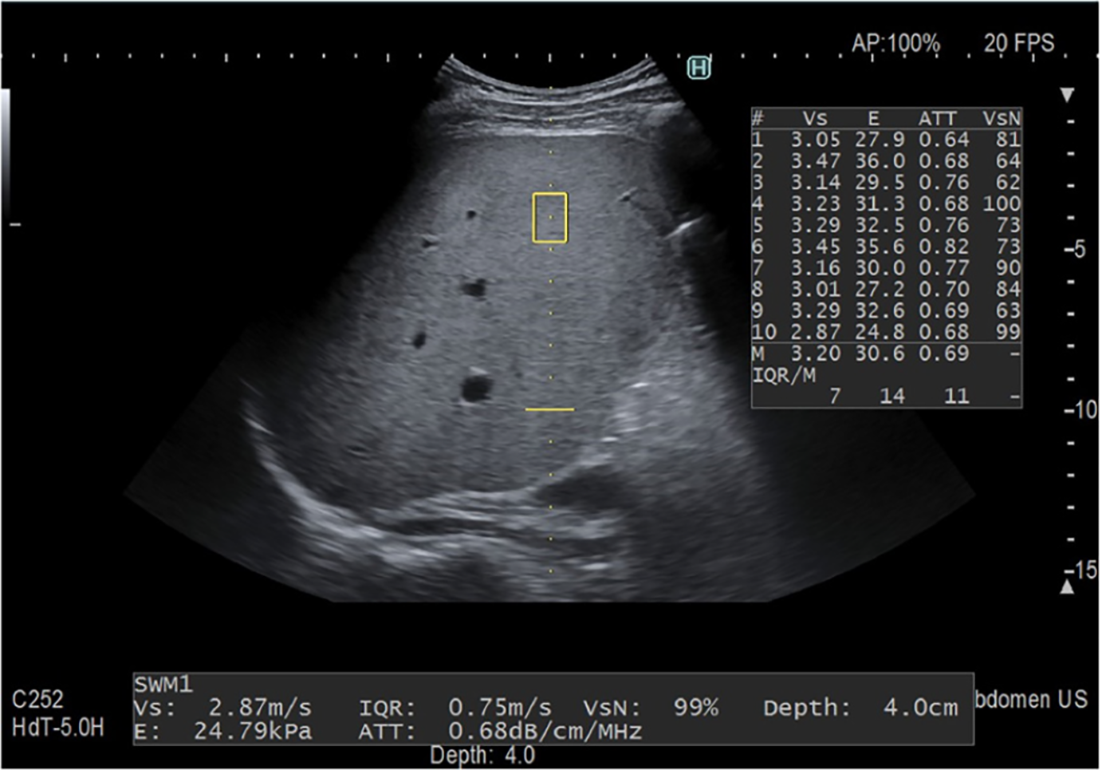
**Figure Legends**

****

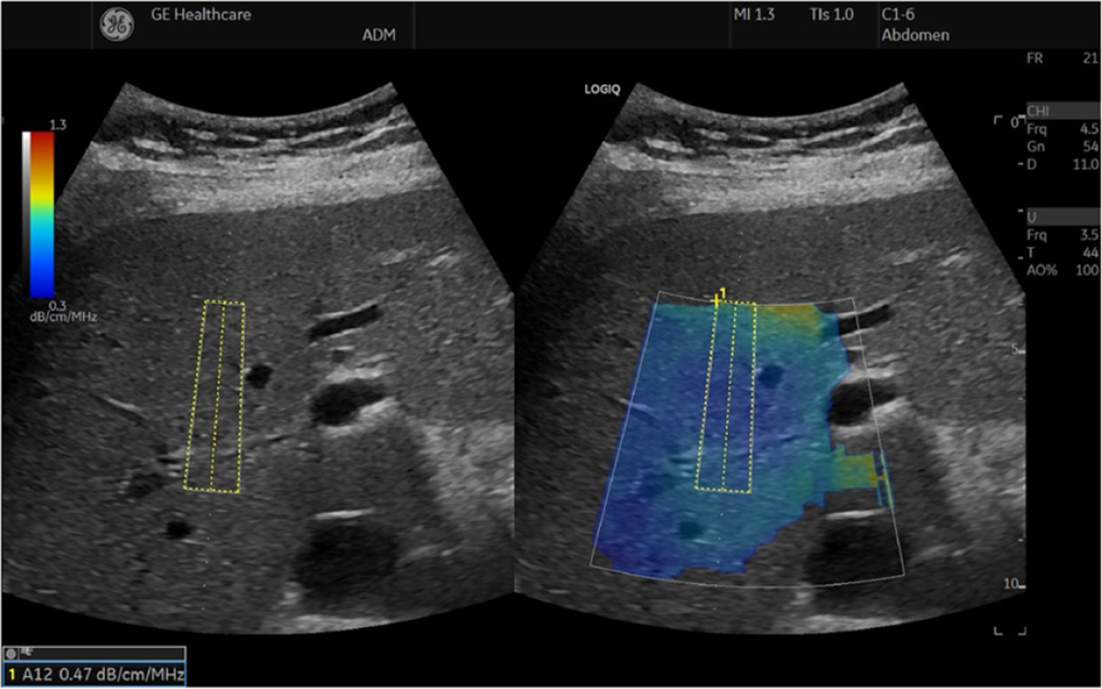
**Figure 1 Hepatorenal index.** In this case, the result was 2.66, indicating severe hepatic steatosis.

****

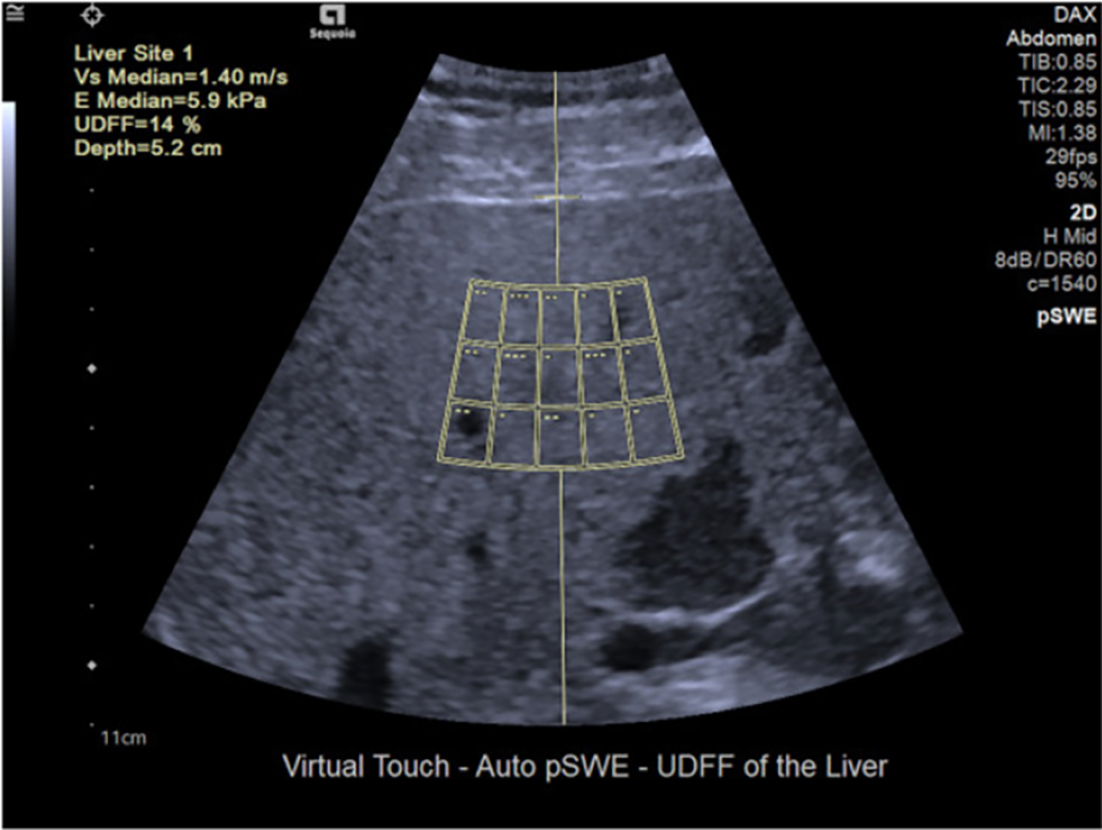
**Figure 2** **Attenuation imaging technique by Canon with reliability indicator (R2)[40].** The Gray scale image and the corresponding attenuation imaging image are shown side by side. The attenuation coefficient measurement of the images shown here is 0.73 dB/cm/MHz with an R2 of 0.97, indicating a valid measurement. Citation: Seneviratne N, Fang C, Sidhu PS. Ultrasound-based hepatic fat quantification: current status and future directions. *Clin Radiol* 2023; 78: 187-200. Copyright© The Author(s) 2023. Published by Elsevier Ltd. The authors have obtained the permission for figure using (Supplementary material).



**Figure 3 The attenuation measurement function technique was developed by Fujifilm Health Care company[4].** The attenuation coefficient (0.68 dB/cm/MHz) is measured in a fixed area (yellow box) along the same axis as the liver stiffness measurement. Ten acquisitions are performed, and the median value is utilized as the final metric. Citation: Ferraioli G, Berzigotti A, Barr RG, Choi BI, Cui XW, Dong Y, Gilja OH, Lee JY, Lee DH, Moriyasu F, Piscaglia F, Sugimoto K, Wong GL, Wong VW, Dietrich CF. Quantification of Liver Fat Content with Ultrasound: A WFUMB Position Paper. *Ultrasound Med Biol* 2021; 47: 2803-2820. Copyright© The Author(s) 2021. Published by Elsevier Ltd. The authors have obtained the permission for figure using (Supplementary material).



**Figure 4 The ultrasound-guided attenuation parameter method implemented in the LOGIQ E9 XDclear 2.0 US scanner[4].** The attenuation coefficient is 0.47 dB/cm/MHz, indicating less than 5% steatosis. Citation: Ferraioli G, Berzigotti A, Barr RG, Choi BI, Cui XW, Dong Y, Gilja OH, Lee JY, Lee DH, Moriyasu F, Piscaglia F, Sugimoto K, Wong GL, Wong VW, Dietrich CF. Quantification of Liver Fat Content with Ultrasound: A WFUMB Position Paper. *Ultrasound Med Biol* 2021; 47: 2803-2820. Copyright© The Author(s) 2021. Published by Elsevier Ltd. The authors have obtained the permission for figure using (Supplementary material).



**Figure 5** **Ultrasound-derived fat fraction method[40].** The ultrasound-derived fat fraction method approximates the magnetic resonance imaging-derived proton density fat fraction and is based on the combination of the attenuation and backscatter coefficient. The method provides both liver stiffness measurement (5.9 kPa in this case) and the percentage of fat accumulation (14% in this case). Citation: Seneviratne N, Fang C, Sidhu PS. Ultrasound-based hepatic fat quantification: current status and future directions. *Clin Radiol* 2023; 78: 187-200. Copyright© The Author(s) 2023. Published by Elsevier Ltd. The authors have obtained the permission for figure using (Supplementary material).

**Table 1 Characteristics of imaging techniques for hepatic steatosis evaluation**

|  |  |  |
| --- | --- | --- |
| **Techniques** | **Clinical characteristics** | **Limitations** |
| CAP | Low cost; High availability; Time-saving | High measurement failure rate |
|  | Allows simultaneous evaluation of steatosis and fibrosis | Measurement without B-mode ultrasound image |
|  | Moderate to high diagnostic accuracy for detecting and grading steatosis | The cutoff value for diagnosing steatosis is poorly standardized |
|  | Moderate to high repeatability and reproducibility |  |
|  | Well validated |  |
| ATI, ATT and UGAP | Outperform or have comparable diagnostic accuracy compared with CAP | The measurement may be influenced by liver fibrosis |
|  | High repeatability and reproducibility | Fairly small number of studies |
|  | Strong correlation with liver histology or MRI-PDFF |  |
|  | Low measurement failure rate |  |
|  | Measured on B-mode ultrasound images |  |
| Att. PLUS | Measurement is obtained at the same time as the sound speed measurement | Fairly small number of studies |
|  | Comparable diagnostic accuracy with CAP | No study comparing this technique with liver histology or MRI-PDFF |
| TAI and TSI | High diagnostic accuracy for detecting and grading steatosis | Fairly small number of studies |
|  | Strong correlation with MRI-PDFF |  |
|  | High repeatability and reproducibility |  |
| BSC | Uses a reference phantom to reduce sources of variability due to ultrasound systems or operators | Fairly small number of studies |
|  | High diagnostic accuracy for detecting and grading steatosis |  |
|  | Strong correlation with liver histology or MRI-PDFF |  |
|  | High repeatability and reproducibility |  |
| UDFF | Is a combination of both attenuation coefficient and backscatter coefficient | Fairly small number of studies |
|  | UDFF approximates MRI-PDFF |  |
| ASQ and NLV | Moderate to high diagnostic accuracy for detecting and grading steatosis | Weak correlation with liver histology |
|  | Strong correlation with CAP | The correlation with MR-based techniques is controversial |
|  |  | The influence of fibrosis on measurement is controversial |
|  |  | Fairly small number of studies |
| SS | Moderate to high diagnostic accuracy for detecting and grading steatosis | Fairly small number of studies |
|  | Strong correlation with CAP |  |
| MRS and MRI-PDFF | High diagnostic accuracy for detecting and grading steatosis | High cost; low availability |
|  | Considered as the reference standard | Time-consuming |

CAP:Controlled attenuation parameter; ATI: Attenuation imaging; ATT: Attenuation measurement function; UGAP: Ultrasound-guided attenuation parameter; Att. PLUS: Attenuation plane-wave ultrasound; TAI: Tissue attenuation imaging; TSI: Tissue scatter distribution imaging; BSC: Backscatter coefficient; UDFF: Ultrasound-derived fat fraction; ASQ:Acoustic structure quantification; NLV: Normalized local variance; SS: Speed of sound; MRS: Magnetic resonance spectroscopy; MRI-PDFF: Magnetic resonance imaging-proton density fat fraction.

**Table 2 Summary of studies using ultrasound methods to evaluate hepatic steatosis**

|  |  |  |  |  |  |  |
| --- | --- | --- | --- | --- | --- | --- |
| **Ref.** | **No.** | **Method** | **Reference standard** | **Grade of steatosis** | **Optimal cutoff value** | **AUROC** |
| Bae *et al*[59], 2019 | 108 | ATI | LB | ≥ S1 | 0.64 | 0.84 |
|  |  |  |  | ≥ S2 | 0.70 | 0.89 |
|  |  |  |  | ≥ S3 | 0.75 | 0.93 |
| Bae *et al*[60], 2022 | 120 | ATI | LB | ≥ S1 | 0.66 | 0.91 |
|  |  |  |  | ≥ S2 | 0.66 | 0.91 |
| Tada *et al*[62], 2019 | 148 | ATI | LB | ≥ S1 | 0.66 | 0.85 |
|  |  |  |  | ≥ S2 | 0.67 | 0.91 |
|  |  |  |  | ≥ S3 | 0.68 | 0.91 |
| Tada *et al*[63], 2020 | 119 | ATI | MRI-PDFF | ≥ S1 | 0.63 | 0.81 |
|  |  |  |  | ≥ S2 | 0.73 | 0.87 |
|  |  |  |  | ≥ S3 | 0.75 | 0.94 |
| Jeon *et al*[61], 2019 | 87 | ATI | MRI-PDFF | ≥ S1 | 0.59 | 0.76 |
| Ferraioli *et al*[65], 2019 | 129 | ATI | MRI-PDFF | ≥ S1 | 0.63 | 0.91 |
|  |  |  |  | ≥ S2 | 0.72 | 0.95 |
| Ferraioli *et al*[66], 2021 | 72 | ATI-GEN | MRI-PDFF | ≥ S1 | 0.62 | 0.92 |
|  |  | ATI-PEN | MRI-PDFF | ≥ S1 | 0.69 | 0.90 |
| Sugimoto *et al*[67], 2021 | 111 | ATI | LB | ≥ S1 | 0.67 | 0.88 |
|  |  |  |  | ≥ S2 | 0.72 | 0.86 |
|  |  |  |  | ≥ S3 | 0.86 | 0.79 |
| Hsu *et al*[70], 2021 | 28 | ATI | LB | ≥ S1 | 0.69 | 0.97 |
|  |  |  |  | ≥ S2 | 0.78 | 0.99 |
|  |  |  |  | ≥ S3 | 0.82 | 0.97 |
| Kwon *et al*[57], 2021 | 100 | ATI | MRI-PDFF | ≥ S1 | 0.62 | 0.91 |
|  |  |  |  | ≥ S2 | 0.72 | 0.94 |
| Jang *et al*[58], 2022 | 57 | ATI | LB | ≥ S1 | 0.62 | 0.81 |
| Koizumi *et al*[73], 2019 | 89 | ATT | LB | ≥ S1 | 0.68 | 0.74 |
|  |  |  |  | ≥ S2 | 0.72 | 0.80 |
|  |  |  |  | ≥ S3 | 0.78 | 0.96 |
| Tamaki *et al*[54], 2018 | 351 | ATT | LB | ≥ S1 | 0.63 | 0.79 |
|  |  |  |  | ≥ S2 | 0.69 | 0.87 |
|  |  |  |  | ≥ S3 | 0.85 | 0.96 |
| Fujiwara *et al*[75], 2018 | 163 | UGAP | LB | ≥ S1 | 0.53 | 0.90 |
|  |  |  |  | ≥ S2 | 0.60 | 0.95 |
|  |  |  |  | ≥ S3 | 0.65 | 0.96 |
| Imajo *et al*[76], 2022 | 1010 | UGAP | MRI-PDFF | ≥ S1 | 0.65 | 0.91 |
|  |  |  |  | ≥ S2 | 0.71 | 0.91 |
|  |  |  |  | ≥ S3 | 0.77 | 0.89 |
| Kuroda *et al*[79], 2021 | 202 | UGAP | LB | ≥ S1 | 0.49 | 0.89 |
|  |  |  |  | ≥ S2 | 0.65 | 0.91 |
|  |  |  |  | ≥ S3 | 0.69 | 0.92 |
| Tada *et al*[80], 2019 | 126 | UGAP | MRI-PDFF | ≥ S1 | 0.60 | 0.92 |
|  |  |  |  | ≥ S2 | 0.69 | 0.87 |
|  |  |  |  | ≥ S3 | 0.69 | 0,89 |
| Jeon *et al*[83], 2021 | 120 | TAI | MRI-PDFF | ≥ S1 | 0.88 | 0.86 |
|  |  | TSI | MRI-PDFF | ≥ S1 | 91.2 | 0.96 |
| Rónaszéki *et al*[84], 2022 | 110 | TAI | MRI-PDFF | ≥ S1 | 0.59 | 0.92 |
|  |  | TSI | MRI-PDFF | ≥ S1 | 99.7 | 0.91 |
| Şendur *et al*[85], 2023 | 80 | TAI | MRI-PDFF | ≥ S1 | 0.75 | 0.95 |
|  |  |  |  | ≥ S2 | 0.86 | 0.97 |
|  |  |  |  | ≥ S3 | 0.96 | 0.97 |
|  |  | TSI | MRI-PDFF | ≥ S1 | 92.44 | 0.96 |
|  |  |  |  | ≥ S2 | 96.64 | 0.91 |
|  |  |  |  | ≥ S3 | 99.45 | 0.94 |
| Lin *et al*[91], 2015 | 204 | BSC | MRI-PDFF | ≥ S1 | 0.0038 | 0.98 |
| Dillman *et al*[94], 2022 | 56 | UDFF | MRI-PDFF | ≥ S1 | 5% | 0.90 |
| Labyed *et al*[37], 2020 | 101 | UDFF | LB | ≥ S1 | 8.1% | 0.94 |
|  |  |  |  | ≥ S2 | 15.9% | 0.88 |
|  |  |  |  | ≥ S3 | 16.1% | 0.83 |

AUROC: Area under the receiver operating characteristic curve; LB: Liver biopsy; MRI-PDFF: Magnetic resonance imaging-proton density fat fraction; ATI: Attenuation imaging; ATT: Attenuation measurement function; UGAP: Ultrasound-guided attenuation parameter; TAI: Tissue attenuation imaging; TSI: Tissue scatter distribution imaging; BSC: Backscatter coefficient; UDFF: Ultrasound-derived fat fraction.

**Table 3** **Summary of techniques for liver fat quantification and their mechanisms**

|  |  |  |
| --- | --- | --- |
| **Technique** | **Mechanism for liver fat quantification** | **Principle of the techniques** |
| CAP | Spectral based technique (AC) | CAP measures the attenuation of or reduction in the amplitude of the ultrasound waves on their way through the liver |
| ATI | Spectral based technique (AC) | ATI quantifies the degree of the ultrasound beam attenuation. The attenuation of the ultrasound beam is calculated by analyzing echo signals received by the transducer |
| ATT | Spectral based technique (AC) | Two ultrasonic waves of different frequencies (F0, F1; F0 < F1) are transmitted to the same beamline and the received signal is obtained. ATT estimates the attenuation coefficient it by calculating the slope of the received signal ratio (F0/F1) |
| UGAP | Spectral based technique (AC) | UGAP compares the measured liver signal and the referential signal (measured on the reference phantom with known attenuation and backscatter coefficients) |
| Att. PLUS | Spectral based technique (AC) | Att. PLUS measures the decrease in amplitude of ultrasound waves as they propagate throughout the tissue |
| TAI | Spectral based technique (AC) | TAI is determined based on the attenuation properties of different frequency components in the tissue, and the spectrum of radiofrequency signals provides a downshift of the center frequency according to depth. The TAI parameter indicates the slope of the ultrasound center frequency downshift |
| BSC | Spectral based technique (BSC) | BSC measures the ultrasound energy returned from the tissue |
| UDFF | Spectral based technique (BSC) | UDFF is obtained by combining both AC and BSC and the result is presented as the percentage of hepatic steatosis. Reference phantom data is integrated into the ultrasound system and fixed-acquisition region of interest is applied |
| TSI | Envelope Statistic based technique | The TSI is based on the shape parameter of the Nakagami distribution which reflects the local concentration and arrangement of ultrasound scatterers |
| ASQ | Envelope Statistic based technique | ASQ measures the FD ratio, which is based on the difference between theoretical and real echo amplitude distributions |
| NLV | Envelope Statistic based technique | NLV parameter was derived from ASQ, which analyzed ultrasound amplitudes sampled from gray-scale ultrasound images |
| SS | Envelope Statistic based technique | SS calculates the speed of sound through the liver |
| SSp.PLUS | Envelope Statistic based technique | SSp.PLUS is a novel technique that allows quantification of the intrahepatic speed of sound which is correlated with the liver fat content |

AC: Attenuation coefficient; BSC: Backscatter coefficient; CAP: Controlled attenuation parameter; ATI: Attenuation imaging; ATT: Attenuation measurement function; UGAP: Ultrasound-guided attenuation parameter; Att.PLUS: Attenuation plane-wave ultrasound; TAI: Tissue attenuation imaging; UDFF: Ultrasound-derived fat fraction; TSI: Tissue scatter distribution imaging; ASQ: Acoustic structure quantification; NLV: Normalized local variance; SS: Speed of sound; SSp.PLUS: Sound speed plane-wave ultrasound; FD: Focal disturbance.



Published by **Baishideng Publishing Group Inc**

7041 Koll Center Parkway, Suite 160, Pleasanton, CA 94566, USA

**Telephone:** +1-925-3991568

**E-mail:** bpgoffice@wjgnet.com

**Help Desk:** https://www.f6publishing.com/helpdesk

https://www.wjgnet.com



**© 2023 Baishideng Publishing Group Inc. All rights reserved.**