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MINIREVIEWS

- 1 Clinical anatomy of hepatic vessels by computed tomography angiography: A minireview
Firat A, Abbasoglu TT, Karcaaltincaba M, Balaban YH
- 10 Advancements of molecular imaging and radiomics in pancreatic carcinoma
Pang XX, Xie L, Yao WJ, Liu XX, Pan B, Chen N

ORIGINAL ARTICLE**Retrospective Study**

- 20 Diagnostic efficacy of diffusion-weighted imaging and semiquantitative and quantitative dynamic contrast-enhanced magnetic resonance imaging in salivary gland tumors
Gökçe E, Beyhan M

ABOUT COVER

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Advancements of molecular imaging and radiomics in pancreatic carcinoma

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Abstract

Despite the recent progress of medical technology in the diagnosis and treatment of tumors, pancreatic carcinoma remains one of the most malignant tumors, with extremely poor prognosis partly due to the difficulty in early and accurate imaging evaluation. This paper focuses on the research progress of magnetic resonance imaging, nuclear medicine molecular imaging and radiomics in the diagnosis of pancreatic carcinoma. We also briefly described the achievements of our team in this field, to facilitate future research and explore new technologies to optimize diagnosis of pancreatic carcinoma.

Key Words: Pancreatic carcinoma; Magnetic resonance imaging; Molecular imaging; Positron emission tomography-computed tomography; Positron emission tomography-magnetic resonance; Artificial intelligence

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Core Tip: Pancreatic carcinoma remains high incidence and poor prognosis. Molecular imaging enables early and precise diagnosis, efficient assessment, non-invasive pathological classification. This paper aims to review the recent research progress of nuclear medicine, magnetic resonance imaging and radiomics in the diagnosis of pancreatic carcinoma, and also briefly describe our team's work in this field.

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INTRODUCTION

In the past decade, significant progress has been made in the medical technology for the treatment of cancers. However, the prognosis of pancreatic carcinoma remains extremely poor due to its insidious location, high malignancy, easy metastasis and rapid progression, which increases the difficulty of early and accurate assessment. Radical surgical resection rate of pancreatic cancer patients is less than 20%. Pancreatic carcinoma is also resistant to radiotherapy and chemotherapy. Moreover, targeted drug therapy, and cytotoxic T-lymphocyte-associated protein 4 and programmed death-1/programmed death-ligand 1 antibody immunotherapy are ineffective. The five-year survival rate of patients remains below 5%-9%, and the number of deaths is the fourth highest among malignant tumors[1]. Early and accurate diagnosis as well as efficacious assessment of pancreatic carcinoma have important clinical significance.

Conventional imaging techniques makes important significance in theranostic of pancreatic cancer; however, these technologies are still deficiencies yet. First of all, magnetic resonance (MR) and computed tomography (CT) only detects limited range with regional scan in clinical routine diagnosis of pancreatic carcinoma, therefore, many patients with distant metastasis are misdiagnosed or never diagnosed. Secondly, the rate of misdiagnosis was high in lymphatic metastasis by MR and CT scan. By reason of no static image provided, ultrasound examination is very unfavorable for reading in clinical work, even this method has the double advantage of real time imaging and radiation lessness. What's more, ultrasound is affected greatly by operators. Finally, some patients who cannot have a proper assessment in regional lymphatic metastasis, especially patients after chemotherapy, even whole body ¹⁸F-FDG positron emission tomography (PET)/CT scan.

Molecular imaging has advanced rapidly in recent years. It enables early and precise diagnosis, efficacy assessment, non-invasive pathological classification, and acts as an important "bridge" to achieve precise diagnosis and treatment[2]. It can meet clinical demands and better protect patient privacy compared to genetic testing. This paper aimed to review the recent research progress of nuclear medicine, magnetic resonance imaging, molecular imaging and radiomics in the diagnosis and treatment of pancreatic carcinoma, and also briefly describe our team's work in this field.

NUCLEAR MEDICINE MOLECULAR IMAGING

Nuclear medicine molecular imaging is based on the principle of injecting microscopic molecular probes into the body and selectively targeting them to appropriate sites based on different properties, in order to qualify or quantify organs, tissues or lesions for assessing diseases at the molecular level. Molecular imaging in nuclear medicine has made significant advances in the treatment of pancreatic carcinoma in recent years.

Glucose metabolism imaging

¹⁸F-FDG is a glucose analogue, which is rapidly taken up by the glucose-transporter on the cell surface after intravenous injection. Various tumor cells, including pancreatic carcinoma, and inflammatory cells in the tumor microenvironment absorb a large amount of ¹⁸F-FDG, but the uptake is influenced by various conditions and the underlying mechanisms are complex[3].

¹⁸F-FDG PET/CT has high specificity, accuracy and sensitivity in the diagnosis of pancreatic carcinoma, and has important clinical value in the diagnosis, staging, surgical indication and evaluation efficacy of pancreatic carcinoma[4]. ¹⁸F-FDG PET/CT is more sensitive and accurate than CT in detecting tumor metastasis, and its whole-body scan is beneficial for tumor staging[5]. This technique detected distant metastases in about one-third of pancreatic carcinoma patients and changed the staging of approximately 26.8% of patients[6]. Its standardized uptake value (SUV) quantification and the rate of change were significantly correlated with tumor size[7], malignancy[8], vascular invasion[9], and lymph node metastasis. In addition, ¹⁸F-FDG PET has significant value in efficacy assessment[10] and survival

prediction[11]. For example, the patients with baseline SUV < 3.5 (and/or) SUV decrease \geq 60% had better overall survival (OS) and progression-free survival (PFS)[12]. In locally advanced or metastatic pancreatic carcinoma, the PFS of patients with $SUV_{max} < 6.8$ was significantly longer than that of patients with $SUV_{max} \geq 6.8$ [13]. ^{18}F -FDG PET/CT-guided radiotherapy with metabolic tumor volume and total lesion glycolysis (TLG) can be used as independent factors affecting prognosis[14]. Yamamoto *et al*[15] found that the early postoperative recurrence rate of pancreatic carcinoma in patients with $SUV_{max} \geq 6.0$ was higher than that of patients with $SUV_{max} < 6.0$, and median OS of the former was lower than the latter (Table 1)[16].

With the increasing application of ^{18}F -FDG PET/CT in recent years, several shortcomings have been gradually revealed. First, as a non-tumor-specific imaging agent, ^{18}F -FDG PET reflects glucose metabolism and is not directly related to the biological properties of the tumor. So non-neoplastic lesions such as inflammation, tuberculosis, or even non-specific uptake with increased glucose metabolism can lead to false positive results. Second, if the patient has high blood glucose levels, uses short-acting insulin or exercises, ^{18}F -FDG can also lead to reduced sensitivity due to increased background uptake. In order to address these problems, nuclear medicine researchers have developed a series of more specific imaging agents for different targets.

Non-glucose metabolism imaging

The highly specific non-FDG molecular probes with different targets achieve accurate diagnosis of pancreatic carcinoma, and also enable non-invasive visualization of the expression of different receptors in tumors, facilitating individualized precision medicine. These imaging agents have been particularly successful in imaging of integrin receptor, somatostatin receptor, tumor-associated fibroblasts, *etc.* Our team has also conducted in-depth research on PD-L1-targeted imaging, non-radioactive molecular imaging and highly specific targeted radiotherapy.

Somatostatin receptor imaging

Somatostatin receptor imaging is mainly used in pancreatic neuroendocrine tumors, with sensitivity of 86%-100% and specificity of 79%-100%[17]. The precursors of somatostatin receptor (SSTR) imaging agents are mainly Tyr(3)-octreotate, 1-Nal(3)-octreotide and D-Phe1-Tyr(3)-octreotide, which have different affinities for different somatostatin receptor subtypes[17]. The neuroendocrine tumors with high differentiation (G1-G2, Ki-67 < 10%) generally showed high expression of SSTR and positive SSTR imaging. Moreover, the degree of malignancy was low, the level of glycolysis was decreased, and the metabolism of FGD was only slightly increased or defective, which led to low sensitivity of ^{18}F -FDG PET [18,19]. In contrast, due to the loss of SSTR and negative SSTR imaging, the increase of malignant degree led to increased glycolysis[20], high metabolism of FGD and increased sensitivity of ^{18}F -FDG PET/CT. In addition to the above three SSTR agonists, SSTR inhibitors have other advantages such as several binding sites, low degradation rate and longer retention in tumors[21] (Table 2)[17].

Fibroblast activation protein imaging

Cancer-associated fibroblasts (CAFs) are a major component of the mesenchyme surrounding epithelial cancer cells. Fibroblast activating protein (FAP) is a marker of CAFs. It is highly expressed in tumor stromal fibroblasts of most common human epithelial carcinomas, and has lower expression in normal tissues[22]. CAFs can form physical and metabolic barriers, which is partly responsible for the resistance of pancreatic carcinoma to chemotherapy and radiotherapy, by reducing the therapeutic effect of combined chemotherapy on pancreatic carcinoma[23]. High expression of CAFs in pancreatic carcinoma is associated with shorter OS and disease-free survival[24,25].

At present, the commonly used FAP-targeted imaging agents are various radionuclide-labeled small molecular FAP inhibitors (FAPIs), mainly FAPI-04, FAPI-21 and FAPI-46. The commonly used imaging agent $^{68}Ga/^{18}F$ -labeled FAPI-04 shows a significantly high uptake in pancreatic carcinoma, which has a good diagnostic efficacy for the primary focus of pancreatic carcinoma. In a comparative study of pancreatic carcinoma and pancreatitis, ^{68}Ga -FAPI-04 PET/MR and ^{18}F -FDG PET/CT positive rates were both 100%, but the former SUV_{max} was significantly higher than the latter SUV_{max} ($P < 0.05$). In addition, ^{68}Ga -FAPI-04 could detect more lymph node metastases, but ^{18}F -FDG was able to detect more liver metastases than ^{68}Ga -FAPI-04[26]. ^{68}Ga -FAPI-04 may be superior to ^{18}F -FDG and CT in the diagnosis of lymph node, bone, liver, lung, peritoneal and pleural metastases of pancreatic carcinoma[27,28]. Deng *et al*[29] reported a 65-year-old male patient with pancreatic head cancer and liver metastasis. ^{18}F -FDG showed slight uptake in the pancreatic lesions and the tenth rib on the right, but not in many low-density or isodensity nodules in the liver, while ^{68}Ga -FAPI PET/CT showed strong FAPI uptake in the pancreatic lesions and the tenth rib on the right, as well as multiple liver lesions.

Our team conducted a comparative study of FAPI and FDG imaging of pancreatic cancer (Figure 1), and redesigned FAPI based on new ideas, which is expected to exceed the existing FAPI-04, FAPI-21 and FAPI-46 in imaging and therapeutic effects. At present, chemical synthesis has been completed and radionuclides such as iodine and technetium have been labeled, and further cellular and animal experiments will be conducted soon.

Table 1 Summary of sensitivity and specificity of different imaging modalities for the diagnosis of pancreatic cancer[16]

Year	Study type	Pancreatic cancer-all (n)	¹⁸ F-FDG PET-CT		CT		MRI		EUS	
			Sens	Spec	Sens	Spec	Sens	Spec	Sens	Spec
2016	Retrospective study	139-139	0.78	-	0.76	-	-	-	-	-
2014	Retrospective study	33-52	1	0.9	0.92	0.5	0.89	0.75	1	0.88
2009	Meta-analysis	3857 ¹	0.9	0.8	-	-	-	-	0.81	0.93
2017	Meta-analysis	3567-5399	0.89	0.7	0.9	0.87	0.93	0.89	0.91	0.86
2014	Retrospective study	80-91	0.68	0.73	-	-	-	-	-	-
2018	Prospective study	278-583	0.93	0.76	0.89	0.71	-	-	-	-
2015	Retrospective study	50-70	0.92	0.65	0.82	0.65	-	-	-	-

¹The study included a total of 3857 patients, but we were unable to obtain the specific number of pancreatic cancer.

This table is adopted from[16]. Sens: Sensitivity, Spec: Specificity. PET: Positron emission tomography; CT: Computed tomography; MRI: Magnetic resonance imaging; EUS: Endoscopic ultrasound.

Table 2 Summary of the main clinical key points of the two EANM/ENETS recommended radiopharmaceuticals[17]

Clinical key points			
Radiopharmaceuticals	Main indication	Diagnostic accuracy	False positive findings
⁶⁸ Ga-TATE, TOC, NOC	Staging and restaging any non-insulinoma panNET case; detection of the unknown primary tumour site or early relapse; evaluation in-vivo SRE; selection for PRRT and/or cold SSA	Sensitivity: 86% to 100%; specificity: from 79% to 100%	Pancreatic uncinata process, accessory spleens (including intra-pancreatic, splenules, infectious/inflammatory findings, non-neuroendocrine tumours)
¹⁸ F-FDG	High grade G2, G3 and NEC; prognosis; rapid tumour progression in earlier diagnosed G1-G2 tumours	Sensitivity: 40% in G1, 60% in G2; 95% in G3 patients	Infectious/inflammatory findings, non-neuroendocrine tumours

This table is adopted from[17]. TATE: Tyr(3)-octreotate; NOC: 1-Nal(3)-octreotide; TOC: D-Phe1-Tyr(3)-octreotide; NEC: Neuroendocrine carcinomas.

Integrin receptor imaging

Tumor neovascularization (angiogenesis) is necessary for maintaining the growth of malignant tumors, which plays a key role in tumor growth, invasion and metastasis, it is an important target for tumor diagnosis and treatment.

Integrin $\alpha\beta_3$ receptor is an important component of the 24 integrins, which is highly expressed on the cell surface of tumor neovascular endothelial cells and many solid tumors. However, it has low or no expression in mature vascular endothelial cells and most normal tissues and organs in healthy people, and plays an important role in angiogenesis, metastasis and tumor invasion[30,31]. The integrin $\alpha\beta_3$ receptor is highly expressed in about 60% of invasive pancreatic carcinomas, and the small polypeptide arginine glycine aspartic acid sequence (RGD) can be targeted to bind to $\alpha\beta_3$ receptor. Using radionuclide-labeled RGD peptides, such as ¹¹¹In, ¹⁸F, ⁶⁸Ga-labeled RGD, can be used to visualize and treat pancreatic carcinoma. Our research team has also studied RII and RIT based on molecular probes constructed by different radionuclide-labeled RGD and RRL peptides[32].

In addition to the integrin $\alpha\beta_3$ receptor, integrin $\alpha V\beta_6$ is also highly expressed in pancreatic carcinoma[33]. Radiation molecular pancreatic probes constructed from the radionuclide ^{99m}Tc and ¹¹¹In-labeled HHK can target $\alpha V\beta_6$ with high specificity to achieve early diagnosis of pancreatic carcinoma and its metastases[34,35]. Based on previous studies, our research team redesigned the HHK peptide (Figure 2). The Gd-DOTA-HHK compound was obtained by chelating Gd³⁺, which can achieve high specific enhancement of tumor $\alpha V\beta_6$ receptor during MRI T1WI scanning. Single photon emission CT imaging with high sensitivity and MRI with high soft tissue resolution combine perfectly to achieve high sensitivity and non-invasive visualization of $\alpha V\beta_6$ targets at high resolution.

In addition, some researchers have explored the application of radionuclide labeling dopa, Exendin-4, CXCR4, and PSMA in pancreatic carcinoma.

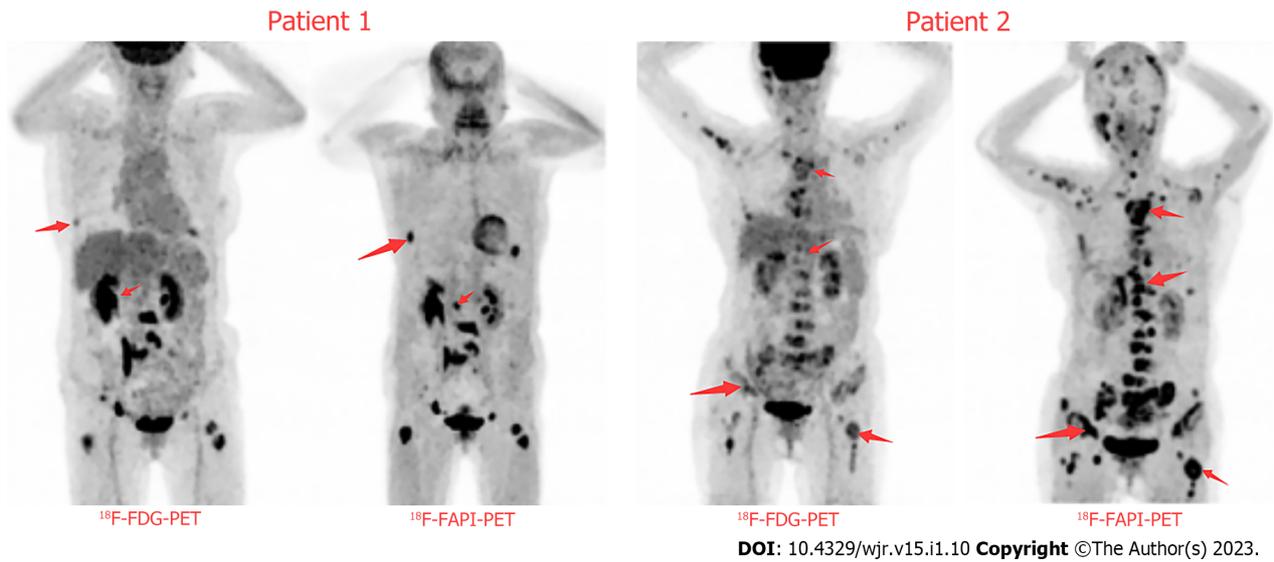


Figure 1 Two patients with pancreatic cancer imaged with ¹⁸F-FDG-positron emission tomography compared with ¹⁸F-FAPI-positron emission tomography. Patient 1 was a 69-year-old female. Patient 2 was a 70-year-old female. ¹⁸F-FAPI-positron emission tomography (PET) detected more lesions than ¹⁸F-FDG-PET, and also had better contrast. PET: Positron emission tomography.

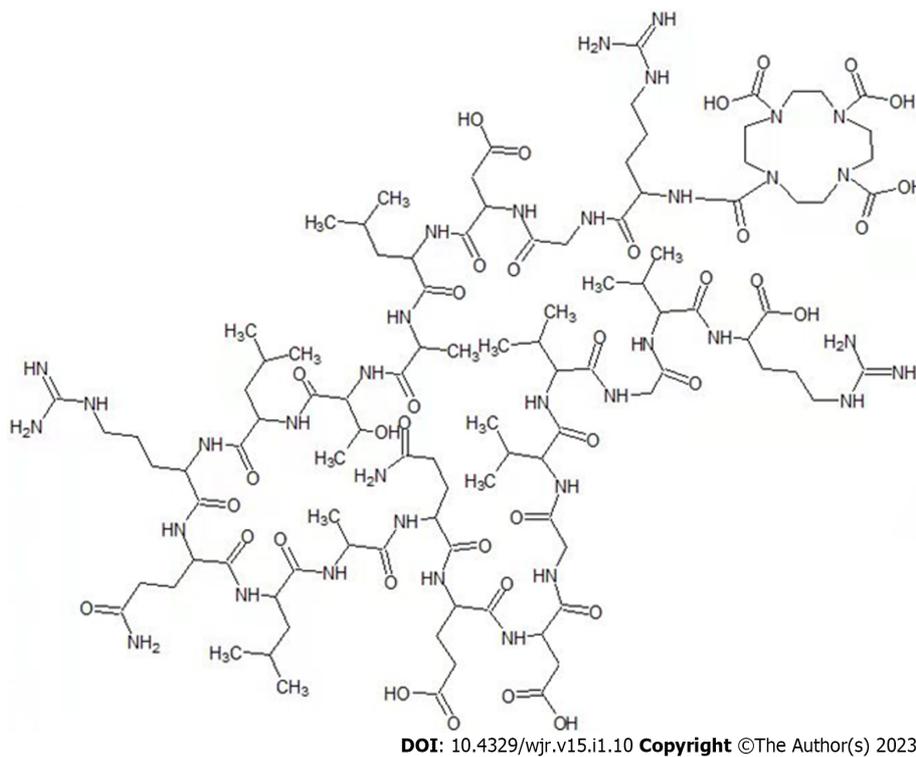


Figure 2 Structure of the redesigned HHK peptide.

MAGNETIC RESONANCE MOLECULAR IMAGING

MRI utilizes magnetic resonance to obtain electromagnetic signals from the human body, which can be reconstructed by computer to show the different chemical components in the same tissue. Because MRI has the advantages of high soft tissue resolution, non-radiation, unrestricted imaging depth and multi-sequence imaging, and with the development of MRI-specific imaging agents, it is possible to evaluate lesions from multiple dimensions of functional and molecular images by MRI.

Diffusion-weighted imaging

Diffusion-weighted imaging (DWI) is the most widely used conventional MRI technique in addition to

T1WI and T2WI. The diffusion movement of water molecules reflects the microstructure of the tumor, such as internal cell density, extracellular space and heterogeneity. When the cell density increases, edema, fibrosis, *etc.*, affect the cell membrane function, which can be detected due to enhanced signal.

Increased b-value (>1000 s/mm²) DWI can increase lesion detection, but high b-value DWI images often exhibit low signal noise ratio, large diffusion-sensitive gradients that tend to distort images and longer scan times. The emergence of computed DWI has partially solved the above problem[36]. Liang *et al*[37] explored the value of computed DWI (cDWI) technique in the diagnosis of pancreatic carcinoma, and the results initially showed that a b-value of c1000-c1500 s/mm² at cDWI technique could effectively display pancreatic carcinoma as well as maintain the image quality. Compared to DWI, intravoxel incoherent motion imaging is based on a biexponential model, which can quantify the diffusion and perfusion motions of water molecules separately. It can reflect the diffusion and perfusion characteristics of tissue cells, respectively, and has the advantages of fast-imaging, low-noise, and multi-parameters[38].

MR dynamic enhancement/Perfusion imaging

MR enhanced or perfusion imaging facilitates T-staging of pancreatic carcinoma by observing the relationship between the lesion, its surrounding tissue and vascular invasion. Both dynamic contrast-enhanced MRI (DCE-MRI) and perfusion MRI can provide quantitative information on blood flow perfusion of lesions (such as tumor tissue)[39]. The most common forms include T2'-weighted dynamic susceptibility contrast (DSC) perfusion and T1-weighted DCE perfusion[40]. However, there are significant differences between the two imaging methods, PWI (DCE and DSC) can reflect the tumor microenvironment such as blood vessel density and blood flow state by quantitative and functional parameters, such as first transit time, mean transit time, time to peak, *etc.* while dynamic enhancement can only obtain time perfusion curves through multi-phase dynamic enhancement, but they are not molecular imaging *per se*.

MR targeted molecular imaging

The basic principle of MR targeted molecular imaging is similar to nuclear medicine molecular imaging. The first step is to construct a specific molecular probe, and then introduce it into the body. After the probe actively and specifically binds to the imaging target, the lesions containing specific molecular targets in the body will be imaged by MRI[41]. Due to the high specificity of the molecular probe, delayed scan time, continuous enhancement within the tumor and relatively high signal on T1WI during the delayed scan, the specificity of the diagnosis is greatly improved[42,43], which helps to improve the detection rate of early microscopic pancreatic carcinoma lesions.

MR molecular probes meet the requirements of high specificity, affinity and signal elements that can be detected by MRI, such as T1 contrast agent represented by gadolinium (Gd), manganese, zinc chelates (Positive) and T2 contrast agent represented by MNP (Negative). Gd is used as a signal component to synthesize paramagnetic molecular imaging probes, mainly to shorten the longitudinal relaxation time of hydrogen protons, increase the T1 relaxation rate and produce positive T1WI contrast [43]. The traditional Gd agent enhanced MRI is diagnosed by the hemodynamic characteristics of lack of blood supply in pancreatic carcinoma, with low relaxation rate and lack of tissue specificity[44]. In recent years, MNP, as represented by SPION, has been applied in MR molecular imaging studies, mainly to shorten the transverse relaxation time, improve the T2 relaxation rate and produce negative T2WI contrast. Compared with Gd and SPION, it has better magnetization and biocompatibility, and no risk of nephrogenic systemic fibrosis[45,46].

In recent years, MR molecular imaging of pancreatic carcinoma is mainly based on basic scientific research. At present, the main targets involved are SSTR[47], urokinase-type plasminogen activator receptor[48], insulin-like growth factor-1 receptor, $\alpha\text{V}\beta_3$, epidermal growth factor receptor, vascular endothelial growth factor receptor-2[49], *etc.*, but their prospect of clinical application requires further study. In addition, targets such as reticulin-1 (plectin-1)[50], mucin-1[51], MUC4, carcinoembryonic antigen-related cell adhesion molecule 6[52], γ -glutamyltransferase 5[53], P32 protein[54], mesothelin [55], thymus fine cell differentiation antigen-1, cathepsin E, neutrophil gelatinase-associated lipid transport protein[56] were also examined, which could lead to a new imaging target for pancreatic carcinoma.

The slow progress of MR targeted molecular imaging compared to nuclear medicine molecular imaging is mainly due to its own limitations. First, the specificity of the above-mentioned types of targets is poor, which affects the specificity of MR molecular imaging[56]. Second, high concentrations of Gd molecular probes are required for imaging, which is difficult to achieve when some molecular targets are expressed at low levels. Finally, factors such as low blood supply, low perfusion in pancreatic carcinoma, denser stromal components in the tumor, and excessive uptake of the molecular probe by the reticuloendothelial system such as liver and spleen *in vivo* decrease the aggregation dose in the tumor, thus affecting the effect of MR molecular imaging[57]. It can be optimized from the following aspects: (1) Improve the biocompatibility of molecular probes and appropriately prolong their blood circulation time to promote more molecular probes to bind to the tumor; (2) The molecular probe simultaneously combines more Gd ions to obtain higher relaxation rate[43]; (3) Multi-target molecular imaging facilitates specific imaging of lesions[42]; and (4) Reduce the volume and molecular weight of

molecular probe to achieve better penetration efficiency, paramagnetic resonance effect, reduce immunity and reticuloendothelial system uptake *in vivo*[42].

Different imaging techniques have their advantages and disadvantages, and their combined application can achieve complementary advantages and improve the value of clinical applications[58]. In addition, the management of radiopharmaceuticals is extremely strict in some countries, and very few radiopharmaceuticals are clinically approved. Therefore, in addition to the research and development of various imaging agents with high specificity and high sensitivity mentioned above, AI technology to improve diagnostic performance or complement existing technologies may be worth exploring.

ARTIFICIAL INTELLIGENCE AND RADIOMICS

AI, artificial intelligence, can be used to mine various medical images for biometric information and imaging features that are not easily perceived by physicians. In recent years, the application of AI-based radiomics has been used for lesion detection, pathological diagnosis, radiotherapy target delineation and curative effect prediction, so as to improve effective treatment decision-making for cancer patients. Based on radiomics, the cross-validated support vector machine classification diagnostic model can automatically extract quantitative features from MDCT[59]. Liu *et al*[60] used the AI system of R-CNN depth neural network to verify the diagnosis of CT images of pancreatic carcinoma in 100 cases, and established an AI diagnosis system of pancreatic carcinoma based on enhanced CT images. The system can assist doctors to identify pancreatic carcinoma, normal pancreatic tissue, chronic pancreatitis or benign pancreatic tumors. Mori *et al*[61] constructed ¹⁸F-FDG-PET/CT radiomic model to predict the recurrence survival value of patients with LAPC after radiotherapy for locally advanced pancreatic cancer, which could significantly improve treatment outcome while avoiding over-treatment of patients with poorer expected outcomes.

Radiomics based on AI has the potential to supplement information for clinical diagnosis and treatment and help solve certain clinical problems, but there are some limitations, such as incorrect tumor screening, insufficient design of database, case number and sensitive feature algorithm.

CONCLUSION

Nuclear medicine molecular imaging is based on the principle of injecting microscopic molecular probes into the body and selectively targeting them to appropriate sites based on different properties, in order to qualify or quantify organs, tissues or lesions for assessing diseases at the molecular level. Molecular imaging in nuclear medicine has made significant advances in the assessment of pancreatic carcinoma in recent years.

FOOTNOTES

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