

Minimizing liver uptake of cationic ^{99m}Tc radiotracers with ether and crown ether functional groups

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Supported in part by Purdue University and research grants: R01 CA115883 A2 (S.L.) from National Cancer Institute, R21 EB003419-02 (S.L.) from National Institute of Biomedical Imaging and Bioengineering and R21 HL083961-01 from National Heart, Lung, and Blood Institute

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Received: September 1, 2009 Revised: January 11, 2010

Accepted: January 18, 2010

Published online: January 27, 2010

Abstract

Ischemia-related diseases, particularly coronary artery disease (CAD), account for the majority of deaths worldwide. Myocardial ischemia is a serious condition and the delay in reperfusion of ischemic tissues can be life-threatening. This is particular true in the aged population. Rapid and accurate early detection of myocardial ischemia is highly desirable so that various therapeutic regimens can be given before irreversible myocardial damage occurs. Myocardial perfusion imaging with radiotracers is an integral component in evaluations of patients with known or suspected CAD. ^{99m}Tc -Sestamibi and ^{99m}Tc -Tetrofosmin are commercial radiopharmaceuticals currently available for myocardial perfusion imaging. Despite their widespread clinical applications, both ^{99m}Tc -Sestamibi and ^{99m}Tc -Tetrofosmin do not meet the requirements of an ideal perfusion imaging agent, largely due to their high liver uptake. The intense liver uptake makes it difficult

to interpret the heart activity in the inferior and left ventricular wall. Photon scattering from the high liver radioactivity accumulation remains a significant challenge for diagnosis of heart diseases. This review will summarize the most recent research efforts to minimize the liver uptake of cationic ^{99m}Tc radiotracers by using ether and crown ether-containing chelators. Fast liver clearance will shorten the duration of imaging protocols (< 30 min post-injection), and allow for early acquisition of heart images with high quality. Improvement of heart/liver ratio may permit better detection of the presence and extent of coronary artery disease. Identification of such a new radiotracer that allows for the improved noninvasive assessment of myocardial perfusion would be of considerable benefit in treatment of patients with suspected CAD.

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Key words: Myocardial perfusion imaging; Cationic ^{99m}Tc radiotracers; Single photon emission computed tomography

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Kim YS, Wang F, Liu S. Minimizing liver uptake of cationic ^{99m}Tc radiotracers with ether and crown ether functional groups. *World J Hepatol* 2010; 2(1): 21-31 Available from: URL: <http://www.wjgnet.com/1948-5182/full/v2/i1/21.htm> DOI: <http://dx.doi.org/10.4254/wjh.v2.i1.21>

INTRODUCTION

Coronary artery disease (CAD) is a leading cause of premature and permanent disability. CAD arises from gradual narrowing of coronary artery due to atherosclerotic deposits. The progressive narrowing of coronary artery

eventually predisposes the patient to myocardial ischemia, a condition in which coronary blood flow decreases to a level below what is needed to meet the demand for oxygen and nutrients. When coronary arterial lumen diameter is reduced by 50%, perfusion abnormalities can be detected but patients are usually asymptomatic. When the diameter is reduced by 70%, clinical symptoms occur during myocardial stress because tissue oxygenation is temporarily below what is needed for adequate heart function. In the advanced ischemic CAD, blood flow and tissue oxygenation are too low to sustain cardiac function at rest. As a result, myocardial infarction occurs. Therefore, rapid and accurate early detection of myocardial ischemia and infarction is highly desirable so that appropriate therapeutic regimens can be given before irreversible myocardial damage occurs.

Diagnostic radiotracers are small molecules labeled with a γ -emitter for single photon emission computed tomography (SPECT) or positron-emitter for positron emission tomography (PET). Nuclear cardiology plays a key role in CAD patient management^[1-12]. Precise measurement of regional blood flow has significant clinical importance in identifying myocardial ischemia and infarction, defining the extent and severity of disease, assessing myocardial viability, establishing the need for medical and surgical intervention, and monitoring the effects of treatment. Thus, the radiotracer must be taken up by the myocardium proportionally to the blood flow in order to evaluate areas with reduced blood flow. If the patient has CAD, there will be an area of reduced radiotracer uptake in the myocardium, corresponding to the area of reduced blood flow. If the reduced uptake is worse under stress conditions than that at rest, the perfusion defect is most likely due to ischemia. Information gained during perfusion imaging studies can be used not only to identify CAD but also to give insight into the patient's prognosis, such as the probability of a hard cardiac event (myocardial infarction or cardiac-related death).

Despite recent development of new non-invasive imaging technologies, such as stress echocardiography and coronary CT (computed tomography) angiography, and wider availability of PET, myocardial perfusion imaging with SPECT radiotracers remains the mainstay of non-invasive evaluations in patients with known or suspected coronary artery disease (CAD)^[1-9]. It is the only available imaging technology that assesses the physiological consequence of coronary stenosis and can be combined with exercise and pharmacological stress^[10].

The introduction of ^{201}Tl in 1970's was the turning point of widespread clinical use of myocardial perfusion imaging, and had a profound impact on therapeutic decision-making in patients with CAD over the last three decades. However, the combination of long half-life ($t_{1/2} = 73$ h), attenuation artifacts due to low abundance of γ -photons and the low count rate from dose constraints may result in suboptimal images in a significant proportion of perfusion imaging studies using ^{201}Tl . In addition, ^{201}Tl images should be taken as soon as it is injected into the patient due to its distribution and

redistribution dynamics, which may not be suitable for situations where immediate imaging is not possible (for example, patients with acute myocardial infarction).

Compared to ^{201}Tl , ^{99m}Tc yields relatively high-energy photons (~ 140 keV) and can be used at high doses due to its short-half life ($t_{1/2} = 6.01$ h). The use of ^{99m}Tc allows simultaneous assessment of myocardial perfusion and cardiac function in a single study^[11]. The combination of half-life, optimal γ -energy and diverse coordination chemistry makes ^{99m}Tc the isotope of choice for development of myocardial perfusion radiotracers. In early 1980s, intensive efforts were focused on the development of ^{99m}Tc complex radiopharmaceuticals^[1,2,5,13]. As a result, ^{99m}Tc -Sestamibi, ^{99m}Tc -Tetrofosmin, and ^{99m}Tc -Teboroxime (Figure 1) have been approved as commercial radiopharmaceuticals for myocardial perfusion imaging in nuclear cardiology. These cationic ^{99m}Tc radiotracers are highly lipophilic with cationic or neutral charge, contain at least two ether-like linkages (N-O-R or C-O-R), and are excreted through the hepatobiliary system due to their high lipophilicity.

An ideal perfusion radiotracer should have a high heart uptake with stable myocardial retention, which linearly tracks myocardial blood flow over a wide range. The uptake in the liver and lungs should be minimal so that diagnostically useful images can be obtained within 30 min post-injection. Despite their widespread applications, both ^{99m}Tc -Sestamibi and ^{99m}Tc -Tetrofosmin do not meet the requirements of an ideal perfusion imaging agent due to their high liver uptake and inability to track the increase in the myocardial blood flow well with roll-off at higher blood flow levels^[14]. The intense liver uptake makes it difficult to interpret the heart activity in the inferior and left ventricular wall^[1,2,5,12,13]. Because of their enterohepatic clearance, the gut uptake is often aggravated by pharmacological stress^[14]. Despite intensive efforts to reduce this interference, photon scattering from the liver activity remains a significant challenge for diagnosis of heart diseases. Thus, it would be of great benefit to develop a new ^{99m}Tc perfusion radiotracer that has high heart uptake with the heart/liver ratio substantially better than that of ^{99m}Tc -Sestamibi and ^{99m}Tc -Tetrofosmin. This review article will summarize recent research efforts to minimize the liver uptake of cationic ^{99m}Tc radiotracers, and will focus on the use of ether and crown ether groups to improve their liver clearance kinetics. The main objective is to illustrate that minimizing liver radioactivity accumulation is critically important for new ^{99m}Tc radiotracers. The ultimate goal is to develop a new ^{99m}Tc perfusion radiotracer that will satisfy the unmet medical need and serve a large population of patients with known or suspected CAD.

IMPROVING LIVER CLEARANCE BY ETHER GROUPS

The usefulness of ether groups to reduce radiotracer liver uptake was first observed in development of ^{99m}Tc -

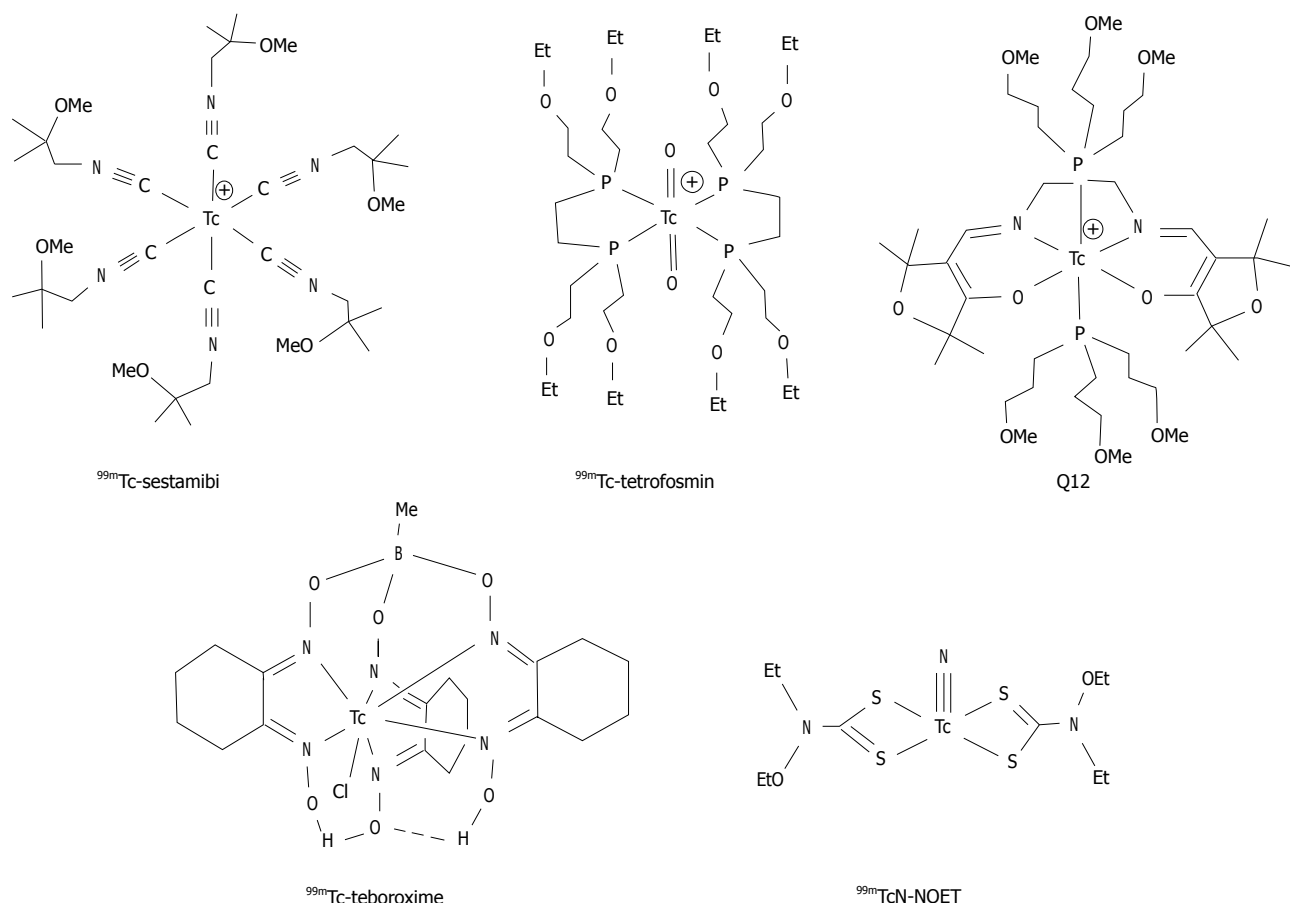


Figure 1 ^{99m}Tc radiotracers useful for heart imaging. ^{99m}Tc -Sestamibi, ^{99m}Tc -Tetrofosmin and ^{99m}Tc -Teboroxime have been approved as commercial radiopharmaceuticals for myocardial perfusion imaging.

Sestamibi^[15-18]. Since then, many ether-containing ligands or chelators have been used to improve T/B ratios of cationic ^{99m}Tc complexes^[19-22]. For example, studies on Q-series of ^{99m}Tc complexes showed that ethers on phosphine ligands could improve the heart uptake and imaging properties^[19]. ^{99m}Tc -Sestamibi, ^{99m}Tc -Tetrofosmin and Q12 all contain six or more ether groups and show much less liver uptake as compared to ^{99m}Tc -Noet and ^{99m}Tc -Teboroxime (Figure 1).

Ether-containing cationic ^{99m}Tc -nitrido complexes.

Duatti's group reported a series of cationic ^{99m}Tc -nitrido complexes (Figure 2), which contain a $[\text{^{99m}Tc}\equiv\text{N}]^{2+}$ core, a bidentate dithiocarbamate (DTC), a tridentate PNP-type bisphosphine^[24,25]. It was found that the amine-N donor atom in the PNP bisphosphine chelator invariably is trans to the $\text{Tc}\equiv\text{N}$ triple bond^[24,25]. The nitrogen heteroatom is important to provide stabilization for the $[\text{^{99m}Tc}\equiv\text{N}]^{2+}$ core. It is remarkable that the combination of DTCs and bisphosphines results in formation of cationic ^{99m}Tc -nitrido complexes of high yield and high radiochemical purity^[24,25]. Results from animal studies show that DTCs and bisphosphines have significant impact on biodistribution properties of cationic ^{99m}Tc -nitrido complexes^[26-29]. Among the cationic ^{99m}Tc -nitrido

complexes evaluated in Sprague-Dawley (SD) rats, ^{99m}Tc -DBODC5 (Figure 2) had a high heart uptake and was able to retain in the rat myocardium for more than 2 h^[26,27]. The liver radioactivity accumulation was almost completely eliminated at 2 h p.i. with the heart/liver ratios being $10 \times$ better than that of ^{99m}Tc -Sestamibi^[26,27]. Imaging studies also showed that ^{99m}Tc -DBODC5 had a fast liver clearance, and was able to give clear images of the heart as early as 15 min post-injection in SD rats^[28]. The first-pass extraction fraction of ^{99m}Tc -DBODC5 was between that of ^{99m}Tc -Sestamibi and ^{99m}Tc -Tetrofosmin^[29]. ^{99m}Tc -DBODC5 is currently under clinical investigation as a new myocardial perfusion radiotracer.

Other bidentate chelators have been used to replace DTC ligands in ^{99m}Tc -DBODC^[30-33]. The use of these bidentate chelators offers a great structural diversity, and allows easy modification of the lipophilicity and biological properties of cationic ^{99m}Tc radiotracers. For example, 2-mercaptopyridine oxide was used to prepare ^{99m}Tc -MPO (Figure 2). ^{99m}Tc -MPO and ^{99m}Tc -DBODC5 shared the same basic structure, but differ in the bidentate π -donor chelating ligand. They also have very similar in vivo stabilities. Biodistribution studies in SD rats showed that ^{99m}Tc -MPO had a high initial heart uptake (2.45 ± 0.58 %ID/g at 5 min post-injection), with a long myocardial retention (2.44 ± 0.46 %ID/g at

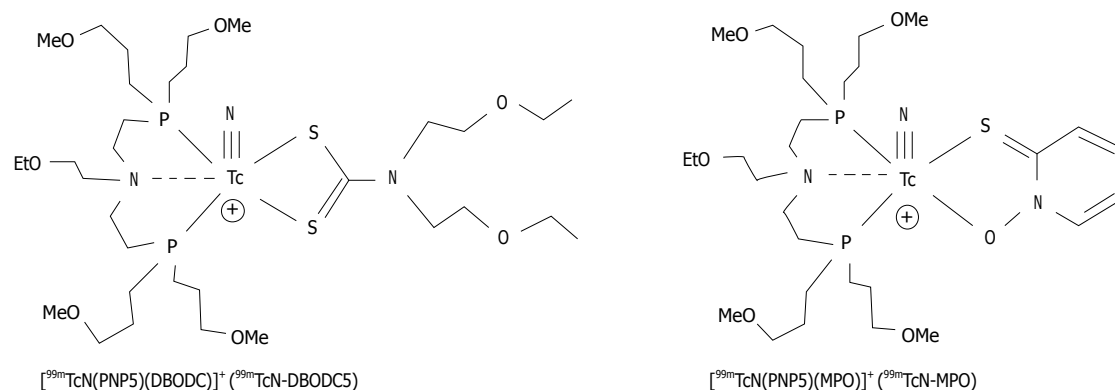


Figure 2 Cationic ^{99m}Tc -nitrido complexes with fast liver clearance and excellent heart/liver ratios. Both $^{99m}\text{TcN-DBODC5}$ and $^{99m}\text{TcN-MPO}$ are under clinical investigation as new myocardial perfusion imaging agents.

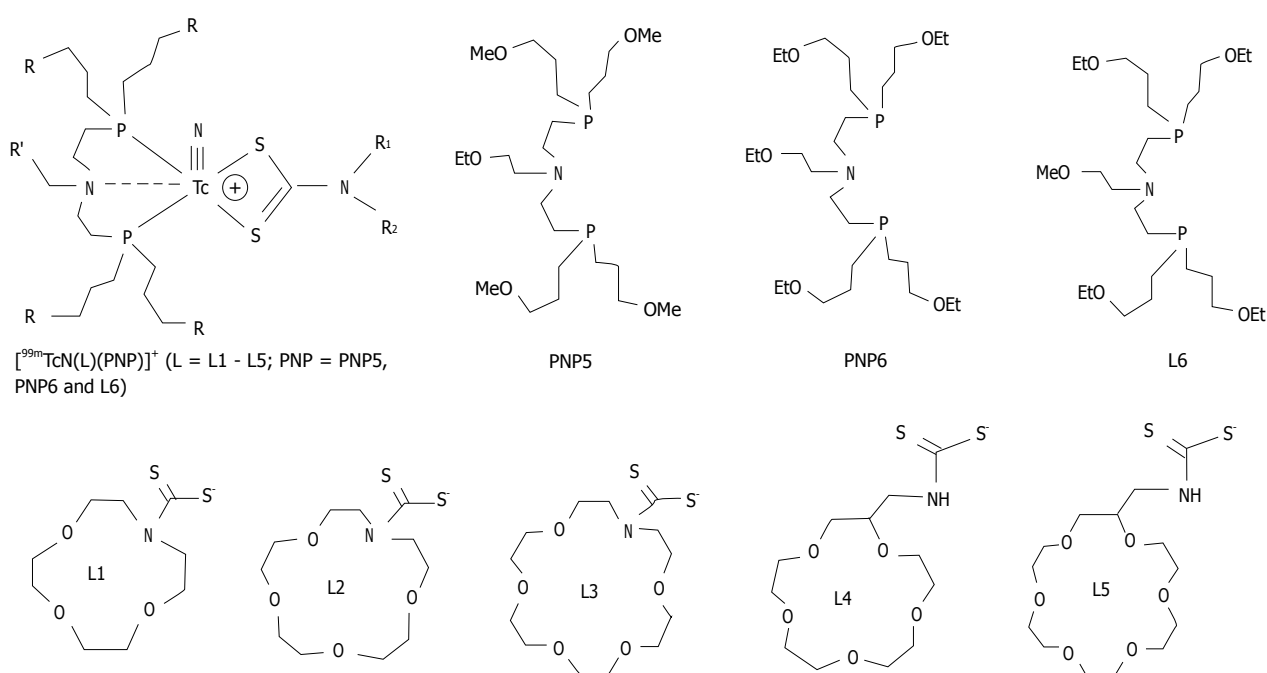


Figure 3 Crown ether-containing DTCs, bisphosphines and their cationic ^{99m}Tc -nitrido complexes.

120 min post-injection)^[46]. The heart uptake of $^{99m}\text{TcN-MPO}$ was between that of ^{99m}Tc -sestamibi and that of $^{99m}\text{TcN-DBODC}$. The liver clearance was fast, resulting in excellent heart/liver ratios. The heart/liver ratio of $^{99m}\text{TcN-MPO}$ at 30 min post-injection was 12.75 ± 3.34 , which is $\sim 4 \times$ higher than that of ^{99m}Tc -sestamibi (2.90 ± 0.62) and $2 \times$ higher than that of $^{99m}\text{TcN-DBODC}$ (6.01 ± 1.45). By 120 min post-injection, the heart/liver ratio of $^{99m}\text{TcN-MPO}$ increased to 27.60 ± 8.44 , which is $8 \times$ that of ^{99m}Tc -sestamibi (3.52 ± 0.34) and is slightly better than that of $^{99m}\text{TcN-DBODC}$ (21.20 ± 3.39) at the same time point, although this difference is not significant within the experimental error.

Crown ether-containing cationic ^{99m}Tc -nitrido complexes

The crown ether-containing DTCs (Figure 3) are of particular interest because they are able to form stable

cationic ^{99m}Tc -nitrido complexes in combination with bisphosphines, and the crown ether groups are able to balance the lipophilicity of cationic ^{99m}Tc -nitrido complexes without changing their overall molecular charge^[31,32]. Both crown ether-containing DTCs and bisphosphines have a significant impact on the lipophilicity of their corresponding cationic ^{99m}Tc -nitrido complexes. For example, $[\text{}^{99m}\text{TcN}(\text{L})(\text{PNP6})]^+$ is much more lipophilic than $[\text{}^{99m}\text{TcN}(\text{L})(\text{PNP5})]^+$ because of the high lipophilicity of the four ethoxy groups in PNP6^[31]. Results from biodistribution studies showed that most of the crown ether-containing cationic ^{99m}Tc -nitrido complexes had a relatively high initial heart uptake with a long myocardial retention^[31]. It was also demonstrated that $[\text{}^{99m}\text{TcN}(\text{L4})(\text{L6})]^+$ ($^{99m}\text{TcN-15C5}$) had the heart/liver ratios that were 4-5 times better than that of ^{99m}Tc -Sestamibi due to its faster liver clearance. The

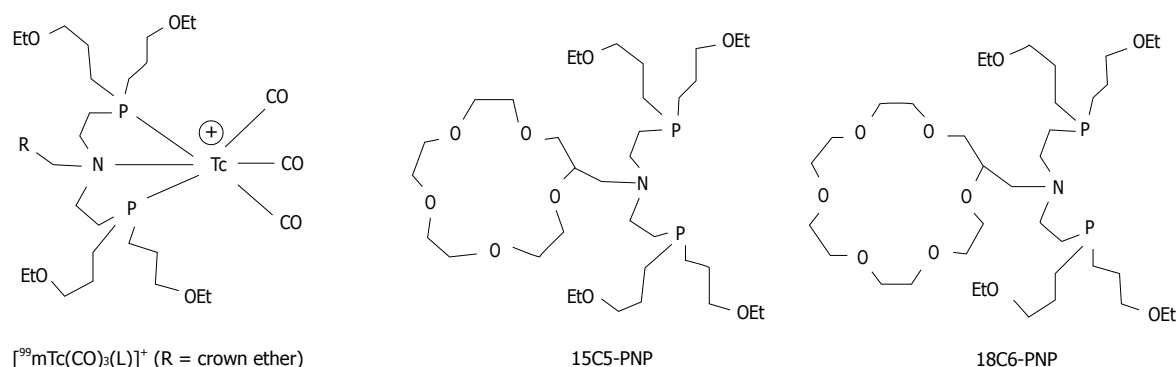


Figure 4 Cationic $^{99m}\text{Tc}(\text{I})$ -tricarbonyl complexes with crown ether-containing PNP bisphosphines.

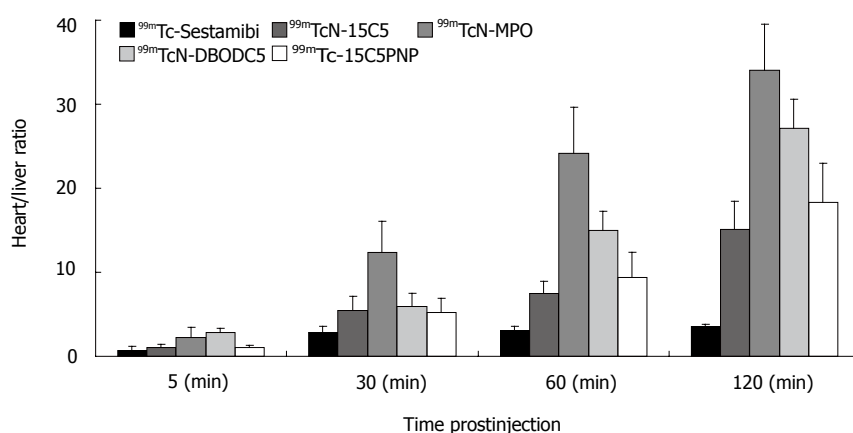


Figure 5 Comparison of heart/liver ratios between $[\text{}^{99m}\text{TcN}(\text{L4})(\text{L6})]^+$ (^{99m}TcN -15C5), $[\text{}^{99m}\text{TcN}(\text{mpo})(\text{PNP5})]^+$ (^{99m}TcN -MPO), $[\text{}^{99m}\text{Tc}(\text{CO})_3(15\text{CPNP})]^+$ (^{99m}Tc -15C5PNP), ^{99m}Tc -Sestamibi and ^{99m}TcN -DBODC5 in SD rats.

heart uptake and heart/liver ratios of ^{99m}TcN -15C5 are comparable to that of ^{99m}TcN -DBODC5^[32]. The results from planar imaging and SPECT studies in dogs further confirm its faster liver clearance kinetics as compared to that of ^{99m}Tc -Sestamibi^[33]. In dogs with acute myocardial infarction, ^{99m}TcN -15C5 was able to detect the perfusion defect as early as 15–30 min.

Crown ether-containing cationic $^{99m}\text{Tc}(\text{I})$ -tricarbonyl complexes

The rich and diverse coordination chemistry of $[\text{}^{99m}\text{Tc}(\text{CO})_3]^+$ offers a tremendous opportunity to develop new $^{99m}\text{Tc}(\text{I})$ -tricarbonyl radiotracers^[34–43]. The $[\text{}^{99m}\text{Tc}(\text{CO})_3]^+$ core has also been widely used to prepare the target-specific ^{99m}Tc radiotracers^[37–40]. In $[\text{}^{99m}\text{Tc}(\text{H}_2\text{O})_3(\text{CO})_3]^+$, all three water molecules are labile with respect to substitution^[40,42]. Monodentate ligands, 2-methoxy-isobutylisonitriles (MIBI) and dimethyl-3-methoxypropylphosphine (DMMP), have been used to prepare complexes $[\text{}^{99m}\text{Tc}(\text{L})_3(\text{CO})_3]^+$ (L = DMMP and MIBI)^[22]. In Sprague-Dawley rats, $[\text{}^{99m}\text{Tc}(\text{DMMP})_3(\text{CO})_3]^+$ and $[\text{}^{99m}\text{Tc}(\text{MIBI})_3(\text{CO})_3]^+$ showed high heart uptake. However, their heart/liver and heart/lung ratios are not as good as that of ^{99m}Tc -Sestamibi due to slow hepatobiliary excretion^[22]. The major challenge is to maintain the “true” cationic nature of $[\text{}^{99m}\text{Tc}(\text{L})_3(\text{CO})_3]^+$ (L = DMMP and MIBI) in the blood circulation.

It has been reported that bidentate ligands form $^{99m}\text{Tc}(\text{I})$ -tricarbonyl complexes with low solution

stability, which may result in high protein binding and high background activity in blood^[37,40]. The chloride in blood may react with $[\text{}^{99m}\text{Tc}(\text{L-L})(\text{CO})_3]^+$ to form neutral complexes $[\text{}^{99m}\text{Tc}(\text{L-L})(\text{CO})_3\text{Cl}]$ that has low heart uptake and slow hepatobiliary excretion. In contrast, the PNP bisphosphines are able to form highly stable cationic complexes $[\text{}^{99m}\text{Tc}(\text{CO})_3(\text{L})]^+$ (Figure 4: L = 15C5-PNP and 18C6-PNP)^[44,45]. The tridentate bisphosphines are critical to maintain the cationic nature of $^{99m}\text{Tc}(\text{I})$ -tricarbonyl complexes. Among the radiotracers evaluated in SD rats, $[\text{}^{99m}\text{Tc}(\text{CO})_3(15\text{C5-PNP})]^+$ (^{99m}Tc -15C5-PNP) had a high initial heart uptake with a long myocardial retention. It also showed a rapid clearance from liver and lungs. The heart/liver ratio of ^{99m}Tc -15C5-PNP is $\sim 2.5\times$ better than that of ^{99m}Tc -Sestamibi at 30 min post-injection. ^{99m}Tc -15C5-PNP is almost identical to ^{99m}TcN -DBODC5 with respect to their heart uptake and heart/liver ratios^[43]. Planar imaging studies also demonstrated that ^{99m}Tc -15C5-PNP had a much better liver clearance profile than ^{99m}Tc -sestamibi.

COMPARISON OF BIODISTRIBUTION CHARACTERISTICS

Figure 5 compares their heart/liver ratios in SD rats at 5, 30, 60 and 120 min post-injection. In general, the heart uptake of ^{99m}TcN -15C5, ^{99m}TcN -MPO, ^{99m}Tc -15C5PNP and ^{99m}TcN -DBODC5 are comparable within

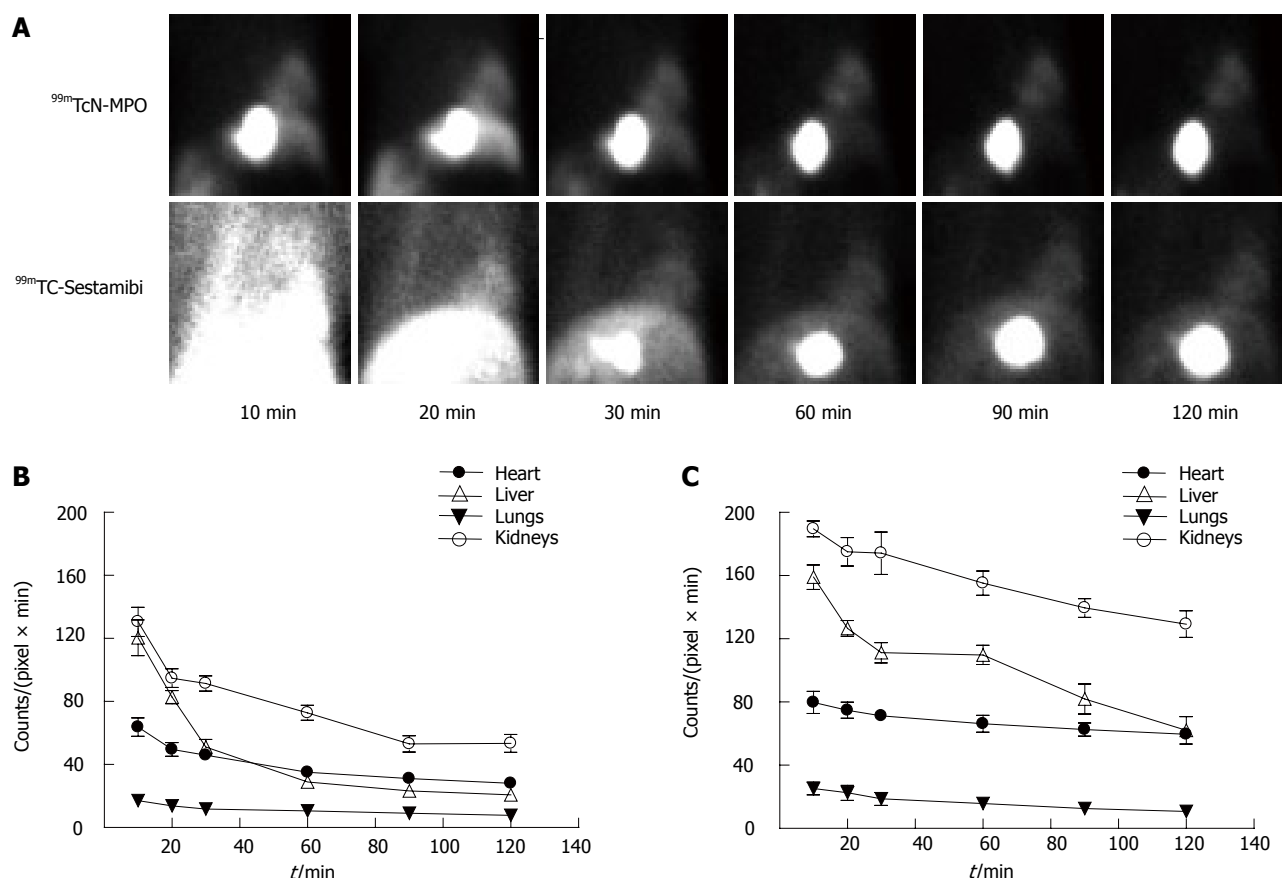


Figure 6 Planar images and organ clearance kinetics of normal dogs. **A:** Planar images of normal dogs administered with $^{99m}\text{TcN-MPO}$ and $^{99m}\text{Tc-Sestamibi}$. Both radiotracers had similar initial myocardial uptake; **B:** Imaging quantification in normal dogs administered with $^{99m}\text{TcN-MPO}$; **C:** Imaging quantification in normal dogs administered with $^{99m}\text{Tc-Sestamibi}$. The liver radioactivity of $^{99m}\text{TcN-MPO}$ was markedly decreased within first 60 min whereas $^{99m}\text{Tc-Sestamibi}$ had a slower reduction in liver radioactivity over time. A mild myocardial washout was observed in the dogs administered with $^{99m}\text{TcN-MPO}$. No significant myocardial washout was seen in dogs administered with $^{99m}\text{Tc-Sestamibi}$.

the experimental error, and is slightly lower than that of $^{99m}\text{Tc-Sestamibi}$, particularly at > 60 min post-injection. However, their heart/liver ratios are much better than that of $^{99m}\text{Tc-Sestamibi}$ at 30-120 min post-injection^[46]. For example, the heart/liver ratio of $^{99m}\text{TcN-MPO}$ (12.75 ± 3.34) at 30 min post-injection is almost twice of that of $^{99m}\text{TcN-DBODC5}$ (6.01 ± 1.45), and is ~ 4 times better than that of $^{99m}\text{Tc-sestamibi}$ (2.90 ± 0.22).

$^{99m}\text{TcN-MPO}$ was further evaluated in normal dogs in comparison with $^{99m}\text{Tc-sestamibi}$. It was found that $^{99m}\text{TcN-MPO}$ and $^{99m}\text{Tc-sestamibi}$ shared very similar blood clearance with $< 50\%$ of initial radioactivity remaining at 1 min, $< 5\%$ of initial radioactivity remaining at 30 min post-injection. The liver uptake in the dogs administered with $^{99m}\text{TcN-MPO}$ decreased rapidly whereas a prolonged liver uptake was seen in all images of the dogs administered with $^{99m}\text{Tc-Sestamibi}$ (Figure 6). The heart/liver ratio of $^{99m}\text{TcN-MPO}$ increased with time (0.53 ± 0.06 at 10 min and 1.22 ± 0.06 at 60 min post-injection), whereas the heart/liver ratio of $^{99m}\text{Tc-Sestamibi}$ remained relatively unchanged over the 2 h study period (0.50 ± 0.03 at 10 min and 0.60 ± 0.02 at 60 min post-injection). SPECT studies (Figure 7) in canines with acute myocardial infarction indicated that the perfusion

defect could be visualized as early as 30 min after administration of $^{99m}\text{TcN-MPO}$ but not $^{99m}\text{Tc-Sestamibi}$. The combination of fast blood clearance, relatively high heart uptake with prolonged myocardial retention makes $^{99m}\text{TcN-MPO}$ a better perfusion imaging radiotracer than $^{99m}\text{Tc-Sestamibi}$. On the basis of preliminary results from the rats and dogs, $^{99m}\text{TcN-MPO}$ was selected as a clinical candidate for human studies.

Safety parameters measured up to 24 h after injection of $^{99m}\text{TcN-MPO}$ revealed no adverse reactions and clinically significant drug-related changes in healthy volunteers (unpublished data). The radiation dosimetry of $^{99m}\text{TcN-MPO}$ is comparable to that of $^{99m}\text{Tc-Sestamibi}$ ^[16] and $^{99m}\text{Tc-Tetrofosmin}$ ^[17]. Figure 8 shows the whole-body images of a healthy volunteer administered with $^{99m}\text{TcN-MPO}$ (~ 25 mCi) at 10, 30, 60 and 240 min post-injection. The radioactivity clearance was so fast that the heart was well separated from the left liver lobe at 10 min post-injection. Although its first-pass extraction fraction was between that of $^{99m}\text{Tc-Sestamibi}$ and $^{99m}\text{Tc-Tetrofosmin}$ ^[5,6], its fast liver clearance of $^{99m}\text{TcN-MPO}$ will allow early visualization of the heart in patients with CAD. The rapid liver clearance may shorten imaging protocols and permit a more precise determination of perfusion defects in the

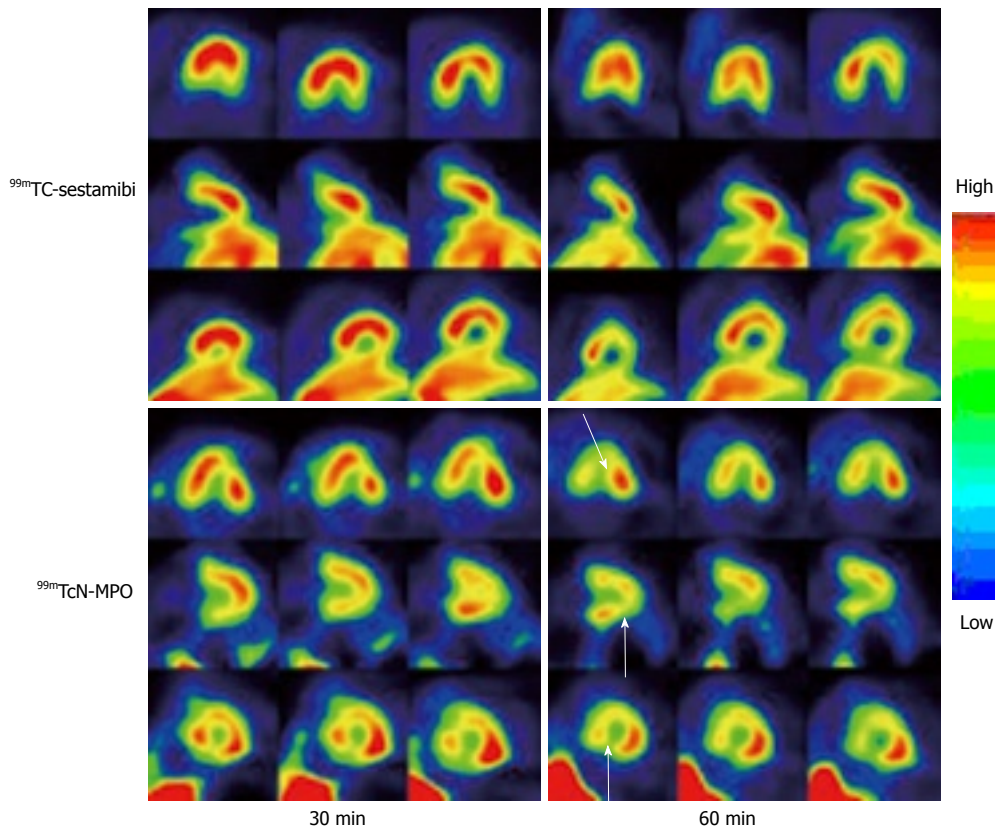


Figure 7 SPECT images of the same dog (with acute myocardial infarction) administered with ~ 10 mCi of ^{99m}Tc -Sestamibi and ^{99m}TcN -MPO at 30 and 60 min p.i. Arrows indicate the presence of perfusion defects due to myocardial infarction. For ^{99m}TcN -MPO, the perfusion defects were clearly seen as early as 30 min post-injection due to its fast liver clearance. For ^{99m}Tc -Sestamibi, there was a significant difference between the perfusion defects and the liver radioactivity.

inferoapical wall on myocardial images. ^{99m}TcN -MPO is an excellent alternative to ^{99m}Tc -Sestamibi for myocardial perfusion imaging when the liver uptake makes it difficult to interpret the heart activity in the inferior and left ventricular wall in patients with known or suspected CAD.

LOCALIZATION MECHANISM

Optimal log P values

Myocardium has the highest mitochondrial population that occupies up to 40% of the total volume of myocytes. Other mitochondria-rich organs include salivary glands, liver and kidneys. This may explain why most lipophilic ^{99m}Tc complex cations tend to have high uptake in mitochondria-rich organs, such as heart, liver and kidneys. For a ^{99m}Tc radiotracer to localize in mitochondria, it must be able to cross plasma and mitochondrial membrane. Regardless of their charge, most small molecules are able to cross the plasma membrane without significant difficulty. However, the mitochondrial membrane is only permeable to those molecules with appropriate molecular charge and molecular shape. While the contribution from mitochondrial potentials provides a driving force for mitochondrial localization of cationic ^{99m}Tc radiotracers, the lipophilicity might modulate their penetration capability across the lipophilic plasma and mitochondrial membranes. There is little information available with regard to the optimal lipophilicity for the heart-selectivity. Cationic ^{99m}Tc radiotracers with the log P values > 1.5 often shows a high protein binding and a slow clearance

from non-cardiac organs while hydrophilic cationic radiotracers with log $P < 0.5$ usually show a low heart uptake with a fast washout from myocardium^[30-32,45]. In both cases, the heart/liver ratio is low because of either high liver uptake or fast myocardial washout. On the basis of studies on cationic ^{99m}Tc -nitrido and $^{99m}\text{Tc(I)}$ -tricarbonyl complexes, it seems that cationic ^{99m}Tc radiotracers must have a log P value in the range of 0.9-1.2 in order to achieve a high heart uptake^[30-32,45,46].

Subcellular distribution characteristics and mitochondrial localization

To understand the myocardial localization mechanism, the subcellular distribution characteristics of ^{99m}TcN -MPO^[47] and ^{99m}TcN -DBODC5^[48] in SD rat hearts were analyzed in comparison with ^{99m}Tc -Sestamibi according to the literature^[49,50]. It was clearly demonstrated that more than 85% of myocardial radioactivity localized in the mitochondria of myocytes for both ^{99m}TcN -MPO and ^{99m}TcN -DBODC5. There was no significant difference between ^{99m}TcN -MPO, ^{99m}TcN -DBODC5 and ^{99m}Tc -Sestamibi with respect to their mitochondrial radioactivity accumulation, and subcellular distribution characteristics.

MULTIDRUG RESISTANCE GENE EXPRESSION AND LIVER CLEARANCE KINETICS

For the last two decades, many cationic ^{99m}Tc radiotracers have been evaluated for their potential as radiotracers

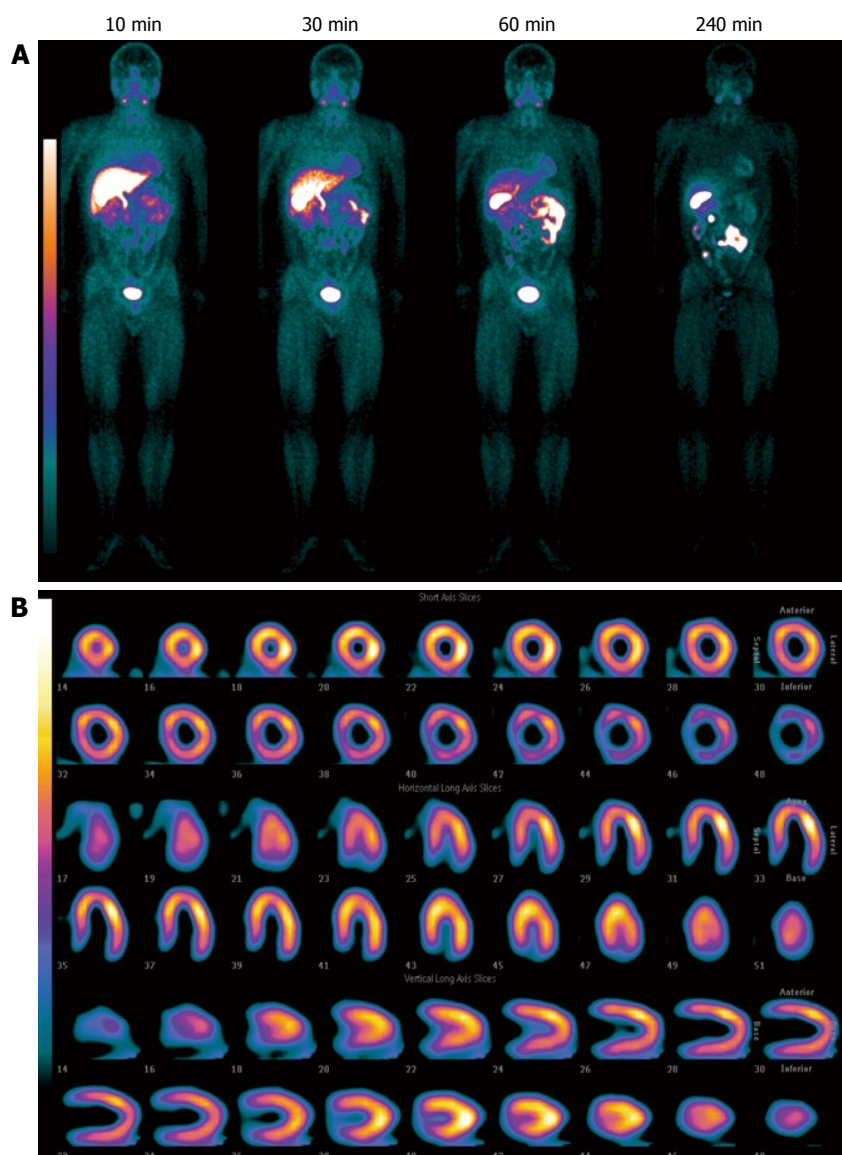


Figure 8 The whole-body images of representative a healthy volunteer administered with $^{99m}\text{TcN-MPO}$. A: Administered with $^{99m}\text{TcN-MPO}$ (~25 mCi) at 10, 30, 60 and 240 min post-injection; B: Representative SPECT images of the heart after administration of $^{99m}\text{TcN-MPO}$ (~25 mCi) at 60 min post-injection.

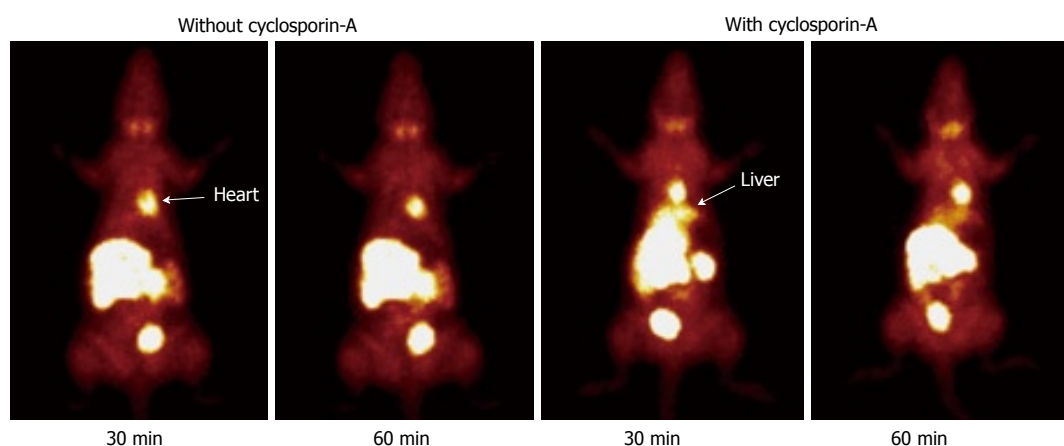


Figure 9 Planar images of the SD rats administered with ~1.0 mCi of $^{99m}\text{TcN-MPO}$ in the absence and presence of cyclosporin-A at 30 and 60 min post-injection. Pre-treatment with cyclosporin-A (14 mg/kg) results in more liver radioactivity accumulation and slower liver clearance.

for heart imaging. However, it is not clear why certain cationic ^{99m}Tc radiotracers show better liver clearance and heart/liver ratios than others, even though they may have a similar lipophilicity. It is well-documented that cationic ^{99m}Tc radiotracers, such as ^{99m}Tc -Sestamibi and ^{99m}Tc -Tetrofosmin, are also clinically useful for noninvasive

imaging of multidrug resistance (*MDR*) in tumors of different origin^[51-53,57,58]. It is well-documented that *MDR1* P-glycoprotein (*MDR1* Pgp) and multidrug resistance associated proteins (*MRPs*) are overexpressed in normal organs that are involved in excretory functions, including kidneys and liver^[54-56]. For example, an increased ^{99m}Tc -

Sestamibi uptake in normal liver of cancer patients has been reported after administration of P-glycoprotein inhibitors^[59,60]. To demonstrate the correlation between the MDR and MRP transport function of hepatocytes and liver excretion kinetics of $^{99m}\text{TcN-MPO}$, both biodistribution and imaging studies were performed using the SD rats in the absence/presence of Cyclosporin A. It was found that the uptake of $^{99m}\text{TcN-MPO}$ in the kidneys and liver was significantly increased, and the radioactivity excretion was delayed, in the presence of Cyclosporin A. Similar results were also obtained in planar images (Figure 9) of SD rats administered with $^{99m}\text{TcN-MPO}$ with/without excess Cyclosporin A. Thus, the MDR/MRP transport function is most likely responsible of the fast efflux of $^{99m}\text{TcN-MPO}$ from kidneys and liver.

CONCLUSION

SPECT remains the modality of choice for myocardial perfusion imaging in current clinical practice. The success of SPECT in nuclear cardiology is largely due to the development of new ^{99m}Tc perfusion radiotracers. Studies on ether- and crown ether-containing cationic ^{99m}Tc complexes clearly show that it is possible to design cationic ^{99m}Tc radiotracers with heart/liver ratios substantially better than that of ^{99m}Tc -Sestamibi. Fast liver radioactivity clearance will shorten the duration of imaging protocols (< 30 min post-injection), and allow for early acquisition of images of high quality. Improvement of the heart/liver ratio will permit better detection of perfusion defects with improved noninvasive assessment of the myocardial perfusion. Preliminary studies on $^{99m}\text{TcN-MPO}$ show that it may have a lower first-pass extraction fraction than ^{99m}Tc -Sestamibi. Thus, future research should focus on cationic ^{99m}Tc perfusion radiotracers with both fast liver clearance and better first-pass extraction fraction. Identification of such a new radiotracer would be of considerable benefit in treatment of patients with suspected CAD.

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