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Deep learning based radiomics for gastrointestinal cancer diagnosis and treatment: A minireview

Wong PK et al. DPR for gastrointestinal cancer

35 Abstract

Gastrointestinal (GI) cancers are the major cause of cancer-related mortality globally. Medical imaging is an important auxiliary means for the diagnosis, assessment and prognostic prediction of GI cancers. Radiomics is an emerging and effective technology to decipher the encoded information within medical images, and traditional machine learning is the most commonly used tool. Recent advances in deep learning technology have further promoted the development of radiomics. In the field of GI cancer, although there are several surveys on radiomics, there is no specific review on the application of deep-learning-based radiomics (DLR). In this review, a search was conducted on Web of Science, PubMed, and Google Scholar with an emphasis on the application of DLR for GI cancers, including esophageal, gastric, liver, pancreatic, and colorectal cancers. Besides, the challenges and recommendations based on the findings of the review are comprehensively analyzed to advance DLR.

Key Words: Radiomics; Deep learning; Gastrointestinal cancer; Medical imaging

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Core Tip: Radiomics, especially deep-learning-based radiomics (DLR), has revolutionized the diagnosis, assessment and prognosis of gastrointestinal (GI) cancer. This review provides an analysis and status of DLR in GI cancer and identifies future challenges and recommendations.



INTRODUCTION

Gastrointestinal (GI) cancers, mainly include colorectal, gastric, liver, esophageal, and pancreatic cancers, and are the leading cause of cancer-related mortality globally^[1]. According to CANCER TOMORROW^[2], a forecast of the global burden of cancer mortality and incidence, by 2040, new cases of GI cancer and deaths will increase significantly (Figure 1). In recent years, computed tomography (CT), magnetic resonance imaging (MRI), positron emission tomography (PET), ultrasound (US) and other medical imaging techniques have been widely used in GI cancer diagnosis and treatment^[3,4]. It is foreseeable that with the increase in GI cancer, the amount of medical imaging data will continue to grow. However, manual reading cannot cope with this growth, and the disparity in expertise among radiologists causes a high rate of missed diagnosis and misdiagnosis. In addition, traditional CT, MRI, PET, US, and other imaging examinations cannot observe changes in tumor heterogeneity, which can provide a better understanding of the causes and progression of cancer^[5]. The development of radiomics technology provides new opportunities and methods to solve these dilemmas.

Radiomics is an emerging method for quantitative analysis and prediction of tumor phenotypes using machine learning or statistical models, and was proposed by Lambin *et al*^[6] in 2012. In recent years, radiomics has been widely used in GI cancer and showed notable outcomes in tumor characterization, therapy response assessment, and prediction of survival rate after surgery^[7-11]. Compared with the conventional method of using only manual inspection, radiomics can extract high-dimensional features that are difficult to be quantitatively described by the doctors from massive radiological images, and to correlate them with clinical and pathological data of patients in order to improve diagnosis and prognostication^[12]. The fundamental premise of radiomics is that the developed descriptive models may produce useful prognostic, predictive and diagnostic information. Radiomics can be divided into two main categories: conventional radiomics, also referred to handcrafted radiomics (HCR) and deep-

learning-based radiomics (DLR), also referred to as discovery radiomics^[13]. Given the benefits of these two approaches, hybrid solutions that mix HCR and DLR also exist.

The HCR workflow is divided into multiple steps: (1) Image acquisition and reconstruction; (2) image segmentation and delineation of region of interest (automatic, semi-automatic, or manual delineation); (3) feature extraction and quantification. This is the core step of HCRs. The extracted features are mainly handcrafted features (also referred as pre-designed features), including shape, texture and intensity features. Some features may be highly correlated or redundant, so feature dimensionality reduction is an important step in feature analysis; and (4) Clinical target-oriented model building and validation. At this step, classic machine learning algorithms are usually used to develop high-precision and high-efficiency prediction models, and the models are trained and validated with sufficient data. The workflow of HCR is depicted in Figure 2.

Although HCR has been widely adopted in GI cancer and has achieved significant results, it has some deficiencies, such as low degree of automation and standardization, cumbersome and time-consuming feature extraction steps, and insufficient robustness and accuracy. Recently, deep learning, a promising technique in characterization of medical images, has gained much attention^[14-17]. Many researchers have adopted DLR to overcome the limitations of conventional radiomics^[18-22]. DL refers to a broad class of algorithms rather than a specific model. As long as a deep neural network structure is used to represent features at a deeper level, it can be called DL model. One of the most popular DL models used in medical imaging is convolutional neural networks (CNNs), which can automatically learn representative features from medical images. The use of CNNs in radiomics makes it easy to build an end-to-end feature extraction process, thereby avoiding the tedious and handcrafted feature extraction process. CNNs can also be used in image reconstruction and segmentation to improve the automation level of HCR, and the accuracy and reliability of diagnosis and prediction (Figure 2).

DL techniques are revolutionizing radiomics. In the field of GI cancer diagnosis and treatment, while there are several surveys on HCR^[9-11], there is no specific review on the

application of DLR. To provide a comprehensive overview of DLR in GI cancer, the performance of DLR in gastroenterology is summarized in this review, with an emphasis on the diagnosis and treatment of GI cancers, including esophageal, gastric, liver, pancreatic, and colorectal cancers. The original contributions to knowledge of this review are: (1) A unique interdisciplinary viewpoint on radiomics by discussing state-of-the-art DLR solutions; and (2) the challenges and recommendations based on the findings of the review are thoroughly analyzed to advance the field.

DLR FOR ESOPHAGEAL CANCER

Esophageal cancer is the seventh most prevalent form of cancer and the sixth most lethal cancer globally^[1], and it is classified into esophageal squamous cell carcinoma (ESCC) or esophageal adenocarcinoma according to the type of cells. In consideration of the low overall 5-year survival rate of patients and the variation in responsiveness of patients to the current treatments such as neoadjuvant chemotherapy (NAC) and neoadjuvant chemoradiotherapy (NCRT) due to tumor heterogeneity, it is vital to have accurate diagnosis, pretreatment evaluation and survival rate prediction. The number of DLR studies regarding esophageal cancer has been growing, with most of the studies exploring treatment response, and the others investigating disease classification and survival rate prediction.

An important preoperative topic of esophageal cancer is diagnosis, yet the number of relevant DLR studies for diagnosis is minimal. Takeuchi *et al*^[23] fine-tuned VGG16 to develop a DLR model for the diagnosis of esophageal cancer from CT scans, and its performance was comparable to that of the radiologists during testing, with a higher accuracy of 84.2% and specificity of 90.0%.

Response to treatment, especially NAC and NCRT, is one of the most popular research interests in the field of esophageal cancer. Hu *et al*^[24] designed a CT-based model to predict the pathological complete response to NCRT of patients with ESCC using DL features, in which the support vector machine (SVM) classifier executed the classification action. The DL features were extracted using pretrained models, and the

optimal one used ResNet50 that achieved an area under the receiver operating characteristic curve (AUC) of 0.805 and accuracy of 77.1% for the testing cohort, which achieved better results than using handcrafted features. Ypsilantis et al^[25] designed a 3S-CNN model that extracted DL features from PET scans and predicted whether the patient with esophageal cancer was non-responsive to NAC. This model was also compared with other competitive machine learning algorithms and results showed that it surpassed the other models with an average specificity, sensitivity and accuracy of 80.7%, 81.6%, and 73.4% respectively. Amyar et al^[26] presented a novel 3D CNN model named 3D RPET-NET that predicted the response to CRT using esophageal cancer images of FDG-PET scans, and a comparative analysis with other approaches in the literature was also carried out. Three-dimensional RPET-NET obtained the best results with an accuracy of around 72% and even reached 75% when using tumor volume with an isotropic margin of 2 cm. Li et al^[27] proposed a CT-based 3D DLR model (3D-DLRM), which was modified from ResNet34. Its aim was to predict whether patients with locally advanced thoracic ESCC had an objective or nonobjective response to concurrent CRT, achieving a validation AUC and positive predictive value of 0.833 and 100%, respectively. They also evaluated a model integrating the 3D-DLRM with clinical selected factors that even outperformed the individual 3D-DLRM, reaching a validation AUC of 0.861.

Other research interests of esophageal cancer include patient survival rate prediction and lymph node (LN) metastasis. The latter is a significant prognostic factor for ESCC. Wang *et al*^[28] compared the use of an HCR model, DLR model and DLR nomogram for the prediction of the survival rate of esophageal cancer patients after 3 years of CRT, in which DL features were extracted and selected by DenseNet-169 to build the DLR model. This DLR nomogram attained the highest validation AUC of 0.942 and Harrell's concordance index (C-index) of 0.784, surpassing the results produced by the sole use of HCR and DLR models. Yang *et al*^[29] proposed a 3D-CNN model based on ResNet18 to predict esophageal cancer patient survival rate using PET scans. The model was initially pretrained to classify abnormal and healthy esophagus, and then trained to classify

whether patients survived or expired within a year after diagnosis in the second stage, and the model obtained an AUC of 0.738. Gong et al[30] developed a hybrid radiomics nomogram to predict local recurrence-free survival (LRFS) of locally advanced ESCC patients who received definitive CRT from contrast-enhanced CT (CECT) scans, and it was combined with radiomic features, features extracted by 3D-DenseNet and prognostic clinical risk factors. The final model achieved a C-index of 0.76 for its external validation set, indicating the effectiveness of the addition of DL features for better prediction performances.

Some studies also discuss the application of DLR to prediction of LN metastasis, which is an effective prognosis factor of ESCC. Wu *et al*^[31] built a model involving HCR, computer vision and DLR to predict the LN status of ESCC patients, and they also constructed two simpler models for efficacy comparison, and they exploited Convolution Neural Network-Fast (CNN-F) to extract DL features from CT images. The model with all signatures involved performed the best with C-statistic of 0.875, 0.874, and 0.840 for training, internal validation, and external validation cohorts, and those demonstrate its satisfactory discriminative ability.

The studies about the application of DLR for esophageal cancer are summarized in Table 1.

DLR FOR GASTRIC CANCER

Gastric cancer (GC) is the fifth most prevalent form of cancer and the fourth most lethal cancer globally^[1]. To ameliorate the low survival rate of patients, early diagnosis of disease and systematic treatment methods are necessary. The application of DLR in GC has been a promising area for research with a rising number of relevant studies published every year, that aim to tackle or refine the existing concerns regarding GC.

Many studies focused on prediction of treatment response of patients. Cui *et al*^[32] constructed a pretreatment venous-phase CT-based DLR nomogram that combined handcrafted features, DL features and remarkable clinicopathological factors to identify locally advanced GC patients with good response to NAC. The nomogram achieved

better than the clinical model and the separate use of two features that were built for comparison, attaining C-index values of 0.829, 0.804, and 0.827 in its internal validation cohort and two external validation cohorts, respectively. Li et al^[33] developed a combined artificial intelligence (AI) model that incorporated feature outputs from HCR and DLR models, which aimed to determine whether the patients had signet ring cell carcinoma (SRCC) of GC and predict survival and treatment response to postoperative chemotherapy from CECT images. They also compared its efficacy with the clinical, HCR and DLR models, and the AI model obtained the best results with an AUC of 0.786 and accuracy of 71.6% for diagnosing SRCC for the test cohort. The AI model also evaluated that SRCC patients with higher risks had shorter median overall survival (OS) and insignificant improvements in median OS after receiving adjuvant chemotherapy than those of lower risk, indicating its good capability to predict survival and response to treatment. Tan et $al^{[34]}$ built a dual-energy CT delta radiomics model to predict the treatment response to chemotherapy of patients with far-advanced GC. They developed a V-Net segmentation model, and the application of this semiautomatic segmentation model to the delta radiomics model shortened the diagnostic time and achieved better results in terms of mean AUC (0.728 vs 0.687 in the testing cohort, 0.828 vs 0.749 in the independent validation cohort) than using manual segmentation.

Survival rate prediction is also a popular topic for DLR of GC. Hao *et al*[35] combined clinical variables, radiomic features and DL features to build a CT-based prediction Cox proportional-hazard model, which served to predict the OS and progression-free survival (PFS) of patients with GC. The model acquired the highest C-index of 0.783 and 0.770 for OS and PFS when using postoperative clinical variables, and the most dominant variables for survival prediction were identified as important prognostic factors in the subsequent survival analysis. Some studies only made use of DL techniques to build predictive models for similar purposes. Zhang *et al*[36] proposed a multi-focus and multi-level fusion feature pyramid network (MMF-FPN) to predict OS risks of GC patients from CT images, and other models using existing methods in the

literature were used for comparison. The experimental results showed that MMF-FPN was the finest model that attained the highest C-indexes (validation: 0.74, testing: 0.76) and hazard ratios (validation: 3.50, testing: 9.46).

To do a preoperative prediction of early recurrence of patients with advanced GC from CT images, Zhang *et al*^[37] designed a radiomics nomogram that utilized clinical characteristics and radiomics signature containing handcrafted and DL features as input. The radiomics nomogram reached an AUC and accuracy of 0.806 and 0.723, respectively, while having considerable k values of 0.932 for both intra- and inter-reader agreement, exceeding the results obtained by the radiomics signature and clinical modal built for comparison.

Accurate prediction of LN status of GC, which is a remarkable prognostic factor, is of importance to determine the appropriate treatment. Guan et al[38] explored the efficacy of using different DL models to extract features and machine learning classifiers (i.e., SVM and random forest) to build a CT-based predictive model for the evaluation of LN status. Other models using radiomic features and integrated features were built for comparison, and the best model was ResNet50-RF with an AUC and accuracy of 0.9803 and 98.10%, respectively. A nomogram based on DL feature scores and clinical risk factors was also developed and a higher AUC of 0.9914 was achieved in the testing cohort. Dong et al[39] proposed a similar DLR nomogram to evaluate the number of LN metastases of locally advanced GC patients before surgery, in which radiomics signatures that contained handcrafted and DL features and clinical characteristics were used. The performance of the model was evaluated with four validations sets; three of which were collected from China and one from Italy. The model showed its good discriminative capability to identify N-staging of GC with higher C-indexes of 0.797 in the validation sets from China and 0.822 in the set from Italy, and it outperformed other predictors such as clinical models and single signatures. To predict the LN status and prognosis of patients, the dual-energy CT-based DLR nomogram created by Li et al[40] incorporated CT-reported LN and two radiomics signatures for arterial-phase and venous-phase CT images, in which DL features were extracted via CNN. The

nomogram performed better and gained a higher AUC of 0.82 than the clinical model built alongside for comparative analysis, and the associated prognosis prediction was satisfactory in terms of PFS (C-index: 0.64) and OS (C-index: 0.67). Jin *et al*^[41] developed a DLR model that adopted ResNet-18 to evaluate the LN status in nodal stations using CECT, and the high value of the median AUC of the 11 stations (0.876) proved the excellent prediction ability of the model. The authors attempted to build a nomogram combining the DL features with clinical features, but no significant improvements in the results were observed.

Other prognostic factors of GC have also been investigated in previous studies. Sun et $al^{[42]}$ exploited DL techniques to build a CT-based radiomics nomogram for evaluating the status of serosal invasion of advanced GC patients. Three radiomics signatures were generated based on the three phases of CT images with their DL features extracted using CNNs, and they were integrated with clinical characteristics to form the nomogram. The final model outperformed other models, such as clinical and phenotypic models, and its AUC for test sets I and II was 0.87 and 0.90, respectively. Li et al^[43] compared the use of DL features and radiomic features to create a CECT-based GC risk (GRISK) model using similar procedures for the prediction of the status of lymphovascular invasion in patients with localized GC. The team explored the use of deep transfer learning models to build a gastric imaging marker, in which five pretrained models and an auto-encoder were utilized for feature extraction and reduction, respectively. Then, it was integrated with patient clinical and radiological characteristics to construct its own GRISK model. The GRISK model with deep transfer learning gastric imaging marker obtained comparable AUC (0.722 vs 0.725) and accuracy (0.671 vs 0.710) with the other model with the radiomics gastric imaging marker but did not surpass the latter model.

The studies investigating the usage of DLR for GC are summarized in Table 2.

DLRs FOR LIVER CANCER

Primary liver cancer is the sixth most prevalent form of cancer and the third most lethal cancer globally, and some of its common phenotypes are hepatocellular carcinoma (HCC) and intrahepatic cholangiocarcinoma^[1]. Taking the high mortality caused by this disease into account, the clinical application of early diagnosis, individualized evaluation and prognosis prediction are valued. The exploitation of DLR technology in liver cancer has been rapidly developing, and various solutions for the issues in different phases of diagnosis and treatment are emerging.

Computer-aided diagnosis does not only aid radiologists such as shortening the diagnosis time, but also allow them to evaluate appropriate treatments at earlier stages of liver cancer. Ding $et\ al^{[44]}$ constructed a CT-based DLR model that fused a radiomics signature and a DL model, to differentiate HCC into low or high grade. The DL model was an alteration of VGG19 and it performed better than the radiomics signature, with better AUC (0.7513 $vs\ 0.7475$) and accuracy (66.31% $vs\ 65.78\%$). The fused DLR model was the optimal model with observable improvements in the results, achieving an AUC of 0.8042 and accuracy of 72.73%.

Accurate prediction of patient response to different therapies is critical to realize personalized treatment at different stages of HCC. Peng *et al*^[45] developed a multi-class DL model from ResNet50 to predict four treatment responses to transarterial chemoembolization (TACE) therapy of HCC patients using CECT scans. Its performance was assessed using confusion matrices and receiver operating characteristic curves, and the model attained an AUC over 0.90 for all four classes in both validation sets, and accuracies of 85.1% and 82.8% for validation sets 1 and 2, respectively. In the next year, they combined conventional radiomics and DL to build a new CECT-based DLR model that served to predict the initial treatment response to TACE of HCC patients preoperatively^[46]. Different from their prior work, they designed their own CNN for feature extraction and prediction, and the DL model was integrated with five radiomics models built with different classic machine learning algorithms or tumor size feature to build integrated models for efficacy comparison. The DL model outperformed all individual radiomics models with an AUC of 0.972, while all

integrated models yielded higher values of AUC than merely using DL model. The combination of DL with random forest classifier obtained the highest AUC of 0.994.

Survival prediction is also an important research area to facilitate individualized HCC treatment. To predict the OS of HCC patients who were treated with stereotactic body radiation therapy, Wei et al[47] established a CECT-based DL network model that comprised two variational-autoencoder-based survival models and one CNN-based model for extracting radiomic features, clinical features and CT features. The performance of the separate models and the integrated radiomics model using either DL network or Cox hazard model was compared by C-index, in which the integrated model produced the highest C-index of 0.650 in repeated cross-validation among all models. Liu et al^[48] developed two separate DLR models to differentiate HCC patients who received radiofrequency ablation (RFA) or surgical resection into high or low risks using CEUS images, and the corresponding radiomics signatures were built. Afterwards, two radiomics nomograms were constructed by combining the signatures with clinical variables to predict the 2-year PFS of patients and both models. Both DLR models achieved satisfactory values of C-index (0.726 for RFA, 0.741 for surgical resection). The good agreement of the survival predictions of the nomograms was demonstrated from the calibration curves.

Postoperative recurrence of cancer is one of the primary causes of death, which extends to the increase in recurrence risk assessment using DLR. To predict the early recurrence of HCC patients using multi-phase CECT scans, Wang *et al*^[49] explored the predictive ability of various kinds of models, and they included a DLR model based on ResNet, a clinical model extracting features from clinical data and three combined CNN-based models of different structures. Experimental results demonstrated that the integration of DL features and clinical features improved the prediction accuracy, and one combined model obtained the highest AUC of 0.825. The team improved their study by comparing the DL model with a conventional radiomics model, and one more combined model of another structure was added to the comparative analysis of their previous work^[50]. The DL model performed better than the radiomics model with an

average AUC of 0.7233 and accuracy of 69.52%, while one of the combined models surpassed the rest in the comparative analysis and reached 0.8248 and 78.66% in its average AUC and accuracy, respectively. They also investigated the effect of attaching a joint loss function to the best model on the average AUC and accuracy, and the two metrics were improved to 0.8331 and 80.49%. He *et al*^[51] presented an intelligent-augmented DL model for Risk Assessment of Post LIver Transplantation (i-RAPIT) model in their study, which was a multi-network model that estimated the recurrence risk of HCC patients after liver transplantation. The i-RAPIT model was composed of two deep CapsNet networks for feature extraction from MR and pathological images, and a natural-language-processing-based radial basis function (NLP-based RBF) for extracting clinical features. Before the MR images were entered into the model, U-Net was also exploited for tumor and liver detection in the images. The model achieved a total accuracy of 82%, and AUC of 0.87 and F-1 score of 84% when comparing with other network combinations.

Early detection of microvascular and macrovascular invasion is another practical approach to select the proper therapy for HCC patients and reduce mortality. Jiang *et al*^[52] adopted 3D-CNN to build a CT-based DL model for predicting the status of microvascular invasion of HCC patients, and three models based on radiomics features, radiologic features, and integration of the two kinds of features and clinical characteristics was also used for comparison. The results produced by the four models were excellent, with the DL model achieving better results for a few metrics such as AUC (0.906), and sensitivity (93.2%) in the validation set. Wang *et al*^[53] devised a new DL model named MVI-Mind that consisted of a light-weight transformer for segmentation and a CNN for prediction of microvascular invasion, and several DL techniques were used to compare the proposed methods. The MVI-Mind attained highest mean intersection over union of 0.9006 and accuracy of 99.47% as compared with other DL segmentation algorithms, and it maintained its superiority in prediction and obtained AUC values of 0.9223, 0.8962, and 0.9100 for arterial phase, portal venous phase and delayed period CT images, respectively. For estimating the status of

macrovascular invasion using CT scans, Fu *et al*^[54] utilized the concept of multi-task DL neural network (MTnet) to build predictive models. Radiomic features from CT images, clinical and radiological factors were fused to construct the proposed model, and it was modified from U-Net that contained modules engaged in tumor segmentation, feature extraction and prediction. It exhibited the most outstanding performance with an AUC of 0.836 among all models built for comparison.

The studies investigating the implementation of DLR for liver cancer are summarized in Table 3.

DLR FOR PANCREATIC CANCER

Pancreatic cancer is the seventh most deadly cancer worldwide, in which pancreatic adenocarcinoma or pancreatic ductal adenocarcinoma (PDAC) are the most prevalent, accounting for the high mortality rate^[1]. The number of deaths caused by this disease is almost equivalent to the number of cases due to the overall poor prognosis, so the introduction of advanced AI technologies is essential and urgent to rectify the situation. In these few years, the field of DLR in pancreatic cancer has flourished and more critical issues such as disease differentiation and survival prediction have been discussed.

Achieving an accurate diagnosis of PDAC gives a great contribution to avoiding false predictions and improving the survival outcomes of patients. For distinguishing between PDAC and autoimmune pancreatitis using CT scans, Ziegelmayer *et al*^[55] developed a DLR model that utilized VGG19 to extract DL features, and its efficacy was compared with a model trained on handcrafted radiomic features. The former model performed better with higher mean values in AUC, sensitivity, and specificity (0.90, 89% and 83%) over the cross-validation procedure. Liao *et al*^[56] used a DL model based on the coarse-to-fine network architecture search (C2FNAS) to perform segmentation of CECT images for radiomic feature extraction, and they were used for training the machine learning model for prediction. The DL segmentation model obtained a mean Dice score of 0.773 for segmentation while the prediction model yielded an AUC of 0.960 when distinguishing between PDAC and the control group (non-cancerous

diseases and normal pancreas). Tong *et al*^[57] constructed a ResNet-50-based DLRs model to classify PDAC and chronic pancreatitis patients from CEUS images, and the outputs were the probability of being PDAC or chronic pancreatitis, and heatmaps with highlighted regions that displayed the detected lesions. A two-round reader study was conducted to test the effectiveness of the model. The model achieved an AUC of 0.967 and 0.953 in two validation sets and outperformed the radiologists in the first round, while radiologists could obtain higher accuracies in determining the disease with the aid of the model in the second round.

Prediction of treatment response is also a critical aspect in the field of DLR in pancreatic cancer. Watson $et~al^{[58]}$ built a CNN model based on LeNet to classify, using CT scans, whether PDAC patients had a pathological response or no response to NAC. It was compared with two models: a hybrid DL model that had the same architecture as the pure DL model but captured both CT image features and one clinical feature [\geq to 10% decrease in carbohydrate antigen (CA)-19], and a CA-19 model only taking in the feature regarding CA-19 decrease. Both DL models could produce superior results than the CA-19 model, and the hybrid DL model obtained a slightly higher AUC than the pure DL model (0.784 vs 0.738).

Survival prediction is another vital feature of PDAC that occupies a substantial portion of the existing DLR studies. Muhammad *et al*^[59] designed a CNN architecture modified from AlexNet to evaluate the survival risk of PDAC patients that received radiomic features extracted from CECT images, and the model reached a C-index of 0.85, indicating itself as a good survival model. Zhang *et al*^[60] also made use of a CNN that was pretrained with non-small cell lung cancer images to construct their CT-based survival model for patients with resectable PDAC, in which a modified loss function was used. The proposed model accomplished finer prognostic predictions than the conventional radiomic model with an index of prediction accuracy of 11.81% and C-index of 0.651. They released another paper in the same year and compared the efficacy of DL and radiomic features from CECT images by feeding them separately to a random forest classifier to build a DLR model for predicting OS^[61]. Similar to their prior

work, the DL features were extracted by a pretrained CNN model but with a different structure. The model that used DL features attained an AUC of 0.81, which was higher than the other model based on radiomic features and gained a hazard ratio of 1.38 when the respective risk scores (predicted probabilities of deaths) were tested in survival analyses. Later, they further modified their previous DLR model to a risk score-based feature fusion model to predict 2-year OS^[62]. Two small models based on DL and radiomic features separately were embodied in the framework to generate their corresponding risk scores, and these risk scores were used to train the main prediction model. The performance of the proposed model was later assessed with other models using different feature reduction techniques, and the risk score model achieved the highest AUC of 0.84. Yao et al^[63] devised a new multi-task network model to perform both survival and tumor surgical margin prediction of resectable PDAC patients simultaneously using multi-phase CECT scans. Inside the model, a 3D-CNN model incorporated with a nnUNet for pancreas segmentation was exploited for the margin prediction part, while the combination of 3D-ResNet18 and Contrast-Enhanced 3D Convolutional Long Short-Term Memory (CE-ConvLSTM) network was responsible for survival prediction. The model achieved the results exceeding all other deep models in the comparative analysis, which yielded a C-index of 0.705 in predicting survival outcome and a balanced accuracy of 73.6% in determining the resection margin. They revised their preliminary work by incorporating pancreatic anatomical features into the model and switching to implement an automatically self-learning segmentation method that used 3D UNet as the network architecture and nnUNet as the backbone model for training^[63]. The new model attained the highest survival C-index of 0.667 and balanced accuracy of 67.1% for resection margin prediction among all the models including their previous model and other DL and radiomics models.

LN metastasis also possesses a high prognostic value in pancreatic cancer and it is noteworthy to have an early and accurate prediction of its status. An *et al*^[64] developed a DLR model with different radiomics signatures extracted from dual-energy CT scans for the prediction of LN metastasis by a pretrained ResNet-18 model. Experiments of

adding key clinical features were conducted to compare the effectiveness of using different approaches. The combined model integrated DL features and key clinical features yielded the highest AUC of 0.92 and accuracy of 86%.

The expression of various genes is an influential factor for patient prognosis and preoperative prediction of these prognostic factors can assist the diagnosis and treatment evaluation process. To predict the status of *HMGA2* and *C-MYC* gene expression of PDAC patients, Li *et al*^[65] compared the use of radiomic features, DL features (extracted by pretrained CNN) and integration of both features in a CT-based model using an SVM classifier. Region of interest segmentation was conducted by two experienced radiologists individually, and the model was tested with different segmented images for improving the validity of the study. A model using DL features and all features achieved similar values in all evaluation metrics for both *C-MYC* and *HMGA2* tests, while DL features selected by Doctor B obtained outstanding average AUC scores (*C-MYC*: 0.90, *HMGA2*: 0.91) and accuracies (*C-MYC*: 95%, *HMGA2*: 88%) in the two gene tests.

The studies investigating the application of DLR for pancreatic cancer are summarized in Table 4.

DLR FOR COLORECTAL CANCER

Colorectal cancer (CRC) is the third most common kind of cancer and the second leading cause of cancer-related fatalities worldwide^[1]. It is crucial to carry out research on the diagnosis, treatment response prediction, and survival prediction of CRC, which can improve the prognosis of patients and significantly reduce the social and medical burden. In recent years, promising research results have emerged in the preoperative, intraoperative and postoperative stages of CRC using DLRs technology, covering the entire process of CRC diagnosis and treatment.

DLR is revolutionizing the treatment options for CRC. When making treatment decisions for CRC patients, identifying *KRAS* mutations, which may contribute to the continued proliferation of tumors, can help personalize treatment and care for CRC

patients^[66]. For preoperative prediction of KRAS mutations in patients with CRC, HCR and DLR were merged into a noninvasive model created by Wu et al^[67]. The model, which mixed the handcrafted and DLR radiomics features, produced a C-index for the original cohort of 0.815 and the validation cohort of 0.832, which was higher than using HCR or DLR alone. For the individualized treatment decision-making in colorectal liver metastases (CRLM) management, the prediction of chemotherapeutic response is crucial. To predict the response to chemotherapy in CRLM, Wei et al[68] developed a ResNet10-based DLR model that used contrast-enhanced multidetector CT images as inputs. They also developed an HCR model for comparison. The DLR model achieved a higher AUC than the HCR model when predicting the response to chemotherapy in CRLM (training: 0.903 vs 0.745; validation: 0.820 vs 0.598). Microsatellite instability (MSI) function is a predictive biomarker for clinical outcomes and predicts responses to adjuvant 5-fluorouracil and immunotherapy in CRC. A DL model that was created using the MobileNetV2 architecture by Zhang et al[69] was adopted to predict the MSI status of CRC based on MR images. With AUC values of 0.868, the best model successfully identified 85.4% of the MSI status, indicating that the suggested model may aid in locating individuals who might benefit from chemotherapy or immunotherapy.

DLR in CRC also emphasizes the need to predict treatment response. For improving NCRT response prediction in locally advanced rectal cancer, Fu et al^[70] compared the handcrafted and DL features extracted from pre-treatment diffusion-weighted MR images. The DLR approach produced a mean AUC of 0.73, while the HCR method yielded a mean AUC of 0.64, which demonstrated that DLR may achieve higher classification performance compared with HCRs. To predict the distant metastasis in locally advanced rectal cancer patients receiving NCRT, Liu et al^[71] exploited the use of a DLR model based on MR images. DLR achieved a C-index of 0.747 and AUC of 0.894 at 3 years. In order to define tumor morphological change for response evaluation in patients with metastatic CRC, Lu et al^[72] offered a DLR study using CNN and recurrent neural network. They discovered that the DL network performed better than the size-based equivalent with C-index (0.649 vs 0.627), and was capable of predicting the early

on-treatment response in metastatic CRC. The predictive performance could be improved by the integration of DL network with size-based methodology.

LN metastasis, which is a key prognostic factor for CRC is among the other study topics of CRC. Ding *et al*^[73] adopted a DLR nomogram based on faster region-based CNN (Faster R-CNN) to predict LN metastasis in patients with CRC. Patient age, Faster R-CNN-detected LN metastasis, and tumor differentiation were predictors in the Faster R-CNN nomogram for predicting LN metastasis, with AUCs in the training and validation sets of 0.862 and 0.920, respectively. Zhao *et al*^[74] applied a DLR model related with genomics phenotypes for predicting LN metastasis in CRC and showed good performance with AUCs of 0.81, 0.77, and 0.73 in the training, testing and validation sets, respectively. Li *et al*^[75] examined the performance of the three most popular classification techniques-DL, conventional machine learning, and deep transfer learning-to determine the most efficient way for automatic classification of CRC LN metastases. Deep transfer learning was the most successful, with an accuracy of 0.7583 and AUC of 0.7941. All of these studies have shown that DLR technology has good performance in the prediction and classification of LN metastasis.

The studies exploring the creation of DLR for CRC are summarized in Table 5.

CHALLENGES AND RECOMMENDATIONS

In the past several years, with the development of DL technology, the research and application of DLR in tumor diagnosis, treatment and prognosis have been increasing. To perform a systematic evaluation of the status of DLRs for GI cancer, we conducted an extensive review on all original publications between January 1, 2015, and August 30, 2022. Even though several published articles have confirmed the exceptional performance of DLR, there are still many issues that algorithm designers and doctors must address. Below is a list of the challenges and recommendations for DLR in future research summarized by our team.

Prospective and multi-center studies

According to the most recent research, most studies on DLR were retrospective and single center. Retrospective studies may have sample selection bias and cannot truly reflect the distribution of clinical cases, which could jeopardize the precision of DLR models. As different centers have different machine parameters, scanning settings, and diagnostic rules, single-center studies limit the generalization of the DLR models. Prospective and multi-center studies can evaluate the reliability and accuracy of the DLR models, enhance their generalization, and bridge the gap between academic studies and clinical applications. Thus, carrying out prospective and multi-center studies is the key to accelerating the clinical application of DLRs models.

Development of user-friendly DL models

We found that many physicians do not really want to use DLR methods for related research because the models usually have complex structures, large parameters, poor interpretability, non-existence of gradients, overfitting, and other problems, which limit the promotion and use of DLR technology. Therefore, it is necessary to develop simple and user-friendly models and training schemes for non-professional users. Publication of more source codes and pre-training weights are ways to reduce the development and training difficulty of DL models. For overfitting problems, development of automatic data augmentation schemes and image synthesis schemes can increase the amount of training data. For the black box nature of DL models, attention maps and network dissection schemes can be integrated into the model to improve interpretability.

Establishment of accessible datasets

For DLR, the dataset is the new oil. DLR analysis requires a large amount of data to train and validate models; however, most studies are based on private datasets and do not use uniform construction standards, which will hinder the reproducibility of the studies and deployment of DLR models. Thus, a professional data development organization that combines multi-center data should be established. The organization should also standardize the development process of multiple kinds of datasets and

make the datasets publicly accessible. Additionally, to reward data contributors, researchers who use these datasets could charge appropriate fees.

Efficient fusion of multiple features

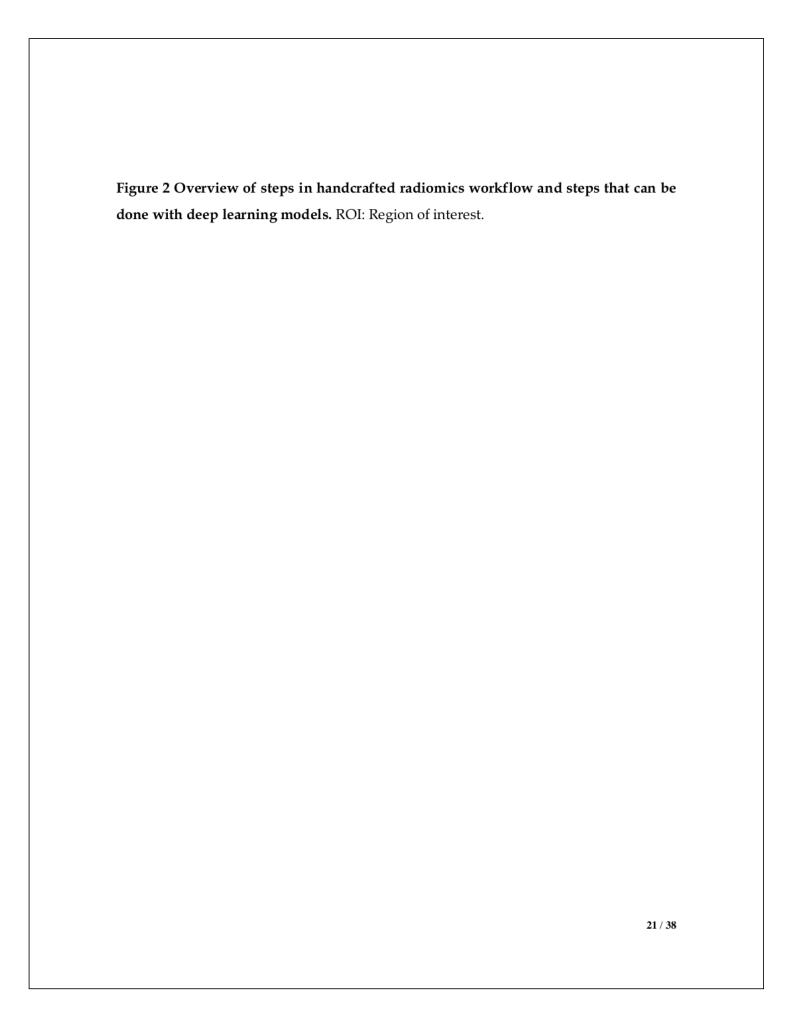
DLR is a new technology in the field of AI for medical image analysis. Although its performance is satisfactory, it is not a panacea, especially in the case of extreme shortage of data. Numerous studies have demonstrated that combining HCR and DLR, can result in better performance. Thus, we suggest integrating other clinical features, genomics, handcrafted features, and DL features to build an optimal solution. Moreover, a suitable feature dimensionality reduction scheme should also be adopted to reduce the redundancy of the integrated features. In addition to imaging features, features extracted from clinical data sources, such as gene expression, clinical characteristics, and blood biomarkers, can also be combined to enhance radiomic features.

CONCLUSION

Globally, GI cancers account for a large portion of cancer-related fatalities. For the diagnosis and treatment of GI cancer, DLR can offer a simpler, quicker and more reliable approach. This article is the first comprehensive review on DLR in the GI tract. The status, difficulties, and suggestions discussed in this review can help engineers create optimal radiomics products to support clinical decision-making and offer guidance for diagnosis and treatment of other tumors. Despite the success of DLR in GI cancer, prospective and multi-center studies are still needed. Development of user-friendly DL models, the creation of large public databases, and the fusion of multiple features are also necessary to encourage the clinical application of radiomics.

Figure Legends

Figure 1 Estimated global new cases and deaths of major gastrointestinal cancers from 2020 to 2040^[2].



1 Table 1 Summary of studies using deep-learning-based radiomics for esophageal cancer

	,	1 0	0	,		
Ref.	Imaging	Study design	Study aim	DL model	Dataset	Outcomes
Takeuchi et	CT	Retrospective	Detection of	VGG16	1646 CT images	images Accuracy: 84.2%; F
$al^{[23]}$, 2021			esophageal cancer		(1500 images for	value: 74.2%;
					training and	Sensitivity: 71.1%;
					validation, 146 for	Specificity: 90%)
					testing)	in test set
Hu <i>et al</i> ^[24] , CT	CT	Retrospective	Evaluation of	of ResNet50	231 patients (161 in	AUC: 0.805; C-
2021			response to NCRT to		training cohort, 70 index:	index: 0.805;
			ESCC		in testing cohort)	Accuracy: 77.1%;
						Sensitivity: 83.9%;
						Specificity: 71.8%)
						for the testing
						cohort
Ypsilantis	PET	Retrospective	Prediction of	of 3S-CNN	107 patients	Sensitivity: 80.7%;
et al ^[25] ,			response to NAC in			Specificity: 81.6%;
2015			patients with			Accuracy: 73.4%
			esophageal cancer			

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75.0%;	76.0%;	74.0%;			PPV:					Ċ							
			7.74		0.833;					0.942;	0.784					.738	
Accuracy:	Sensitivity:	Specificity:	AUC: 0.74		AUC:	100%				AUC:	index: (AUC: 0.738	
of 3D RPET- 97 patients					306 patients (203 in AUC: 0.833; PPV:	training cohort, 103 100%	in validation	cohort)		154 patients (116 in AUC: 0.942;	training cohort, 38 index: 0.784	in validation	cohort)			1107 scans	
RPET-	_				of ResNet34					of DenseNet-						3D-CNN	uo pa
3D	NE				Res					Den	169					3D-(base
Jo	radio-	.ii	with	ıcer	of	sponse	among	locally	CC	of	s for	with	cancer	yr with	rapy	of	cancer based
u	to	erapy		eal car	u	ıt re		with	d TES	u	rates		eal		diothe	ation	
Prediction	response to radio- NET	chemotherapy	patients	esophageal cancer	Prediction	treatment response	to CCRT	patients with locally	advanced TESCC	Prediction	survival	patients	esophageal	after 3	chemoradiotherapy	Identification	esophageal
Retrospective	I	0	H	Ð	Retrospective	1	+	ii.	0	Retrospective	S	H	y	to .	0	Retrospective	9
PET					CI					CI						et PET	
Amyar <i>et</i> PET	010				Li et al ^[27] , CT					Wang et	022						al ^[29] , 2019
1	7				et	1				gui	al ^[28] , 2022					હ	٦, 2
Amya	$al^{[26]}$, 2019				Ľ	2021				W	al[2					Yang	a][29

		patients with poor KesNet18	_	
		prognosis		
Gong et CECT	Retrospective	Prediction of LRFS in 3D-	397 patients	C-index: 0.76
al ^[30] , 2022		esophageal cancer Densenet		
		patients after 1 yr of		
		definitive		
		chemoradiotherapy		
Wu et al ^[31] , CT	Retrospective	Prediction of LN CNN-F	411 patients	C- index: 0.840
2019		status of patients		

Neoadjuvant chemoradiotherapy; NAC: Neoadjuvant chemotherapy; ESCC: Esophageal squamous cell carcinoma; CCRT: CT: Computed tomography; PET: Positron emission tomography; CECT: Contrast-enhanced computed tomography; NCRT: Concurrent chemo-radiation therapy; TESCC: Thoracic esophageal squamous cell carcinoma; LRFS: Local recurrence-free survival; LN: Lymph node; CNN-F: Convolutional neural network-fast; AUC: Area under the receiver operating characteristic curve; PPV: Positive predictive value; DLR: Deep-learning-based radiomics.

1 Table 2 Summary of studies using deep-learning-based radiomics for gastric cancer

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Ref.	Imaging	Study design	Study aim	DL model	Dataset	Outcomes
Cui <i>et al</i> ^[32] , CT	CT	Retrospective	Prediction of response DenseNet-121	DenseNet-121	719 patients	C-index: 0.829
2022			to NAC in patients			
			with LAGC			
Li <i>et al</i> ^[33] , CT	CI	Retrospective	Diagnosis and	and Modified U-	U- 855 patients	patients For diagnosis, AUC:
2022			prediction of	Net	(598 in training	(598 in training 0.786; accuracy: 71.6%;
			chemotherapy		cohort; 257 in sensitivity:	sensitivity: 77.3%;
			response to SRCC		testing cohort)	specificity: 69.2% for
			patients			testing cohort
Tan <i>et al</i> [34], CT	CT	Retrospective	Prediction of response	V-Net	116 patients	Mean AUC: 0.728 (testing
2020			to chemotherapy in			cohort); 0.828 (validation
			patients with gastric			cohort) when using semi-
			cancer			segmentation
Hao <i>et al</i> [35], CT	CT	Retrospective	Prediction of OS and Attention-	Attention-	1061 patients	patients C-index of OS: 0.783; C-
2021			PFS after gastrectomy;	guided VAE	(743 for	for index of PFS: 0.770 when
			evaluation of effects of		training; 318	318 only using postoperative
			variables on survival		for testing)	variables

		prediction		
Zhana at CT	Rotrognoctivo	Prediction of OS viete MME HPN	640 rationts Cind	nationts Cindox 076. Hazand
Znang et C1	verrospective	Frediction of OS risks Minif-FFIN		lex: U./6; паzard
a[[36], 2021		of patients with	(337 in training ratio: 9.46 in test set	9.46 in test set
		gastric cancer	set; 181 in	
			validation set;	
			122 in test set)	
Zhang et CT	Retrospective	Prediction of early DCNNs	669 patients AUC:	AUC: 0.806; accuracy:
al ^[37] , 2020		recurrence of patients	0.723;	0.723; sensitivity: 0.827;
		with AGC	specif	specificity: 0.667
Guan et CT	Retrospective	Prediction of ResNet50-RF	347 patients AUC:	patients AUC: 0.9803; accuracy:
al ^[38] , 2022		preoperative status of	(242 for 98.10%;	%; sensitivity:
		LNM of gastric cancer	training; 105 98.39%;	%; specificity:
		patients	for testing) 0.9767	0.9767% for testing of
			ResN	ResNet50-RF
Dong et CT	Retrospective	Prediction of the DenseNet-201 730 patients	730 patients C-index:	lex: 0.822 in
al ^[39] , 2020		number of LNM in	valida	validation set
		LAGC		

				- 1	
Li et al^{40} , CI	Retrospective	Prediction of LNM DCNNs	DCNNs	204 patients	patients AUC: 0.82 in test set; C-
2020		and prognosis in		(136 in training	(136 in training index of OS: 0.67; C-
		gastric cancer patients		set, 68 in test	set, 68 in test index of PFS: 0.64
				set)	
Jin et al ^[41] , CT	Retrospective	Prediction of LNM ResNet-18	ResNet-18	1699 patients	Median AUC: 0.876;
2021		status in LN stations			median Sensitivity: 0.743;
		of gastric cancer			median Specificity: 0.936
		patients			in validation cohort
Sun et al ^[42] , CT	Stage I:	I: Prediction of serosa DCNNs	DCNNs	572 patients	AUC: 0.87; accuracy:
2020	Retrospective;	invasion of AGC		(252 in training	80%; sensitivity: 0.73;
	stage II:	patients		set, 176 in test	specificity: 0.85 in test set
	Validation			set I, 144 in test	set I, 144 in test I. AUC: 0.90; accuracy:
				set II)	85%; sensitivity: 0.75;
					specificity: 0.93 in test set
					П
Li <i>et al</i> [43] , CT	Retrospective	Evaluation of	of SqueezeNet,	1062 patients	patients AUC: 0.725; sensitivity:
2022		lymphovascular	ResNet50,	(728 for	73.2%; specificity: 60.3%;
		invasion of localized Inception V3, training,	Inception V3,	training, 334	accuracy: 71.0% for

ing) radiomics GRISK model	(final model) in testing	tackoo.
VGG19, for testing))eepLoc	
gastric cancer patients VC	Ď	

carcinoma; OS: Overall survival; PFS: Progression-free survival; AGC: Advanced gastric cancer; LNM: Lymph node metastasis; LN: Lymph node; DCNNs: Deep convolutional neural networks; MMN-FPN: Multi-focus and multi-level fusion feature pyramid network; UC: Area under the receiver operating characteristic curve; C-index: Harrell's concordance index; GRISK: Gastric Risk; CT: Computed tomography; NAC: Neoadjuvant chemotherapy; LAGC: Locally advanced gastric cancer; SRCC: Signet ring cell RF: Random forest; VAE: Variational auto-encoder; DLR: Deep-learning-based radiomics.

Table 3 Summary of studies using deep-learning-based radiomics for liver cancer

Ref.	Imaging	Study design Study aim	Study aim	DL model	Dataset		Outcomes		
Ding et	CT	Retrospective	Evaluation of VGG19	of VGG19	1234	patients	1234 patients AUC: 0.8042; accuracy:	12; accu	racy:
a[[44], 2021			HCC		(799 in training 72.73%;	training	72.73%;	sensitivity:	vity:
			differentiation		cohort,	cohort, 248 in 70.75%;	70.75%;	specificity:	icity:
					validation	_	75.31% in testing cohort	esting co	hort
					cohort;	187 in	cohort; 187 in for the fused DLRs	I pəsnı)LRs

					independent	ndent	model		
					testing cohort)	cohort)			
Peng et CT	Retrospective	Prediction	of I	of ResNet50	789 pat	789 patients (562 Accuracy:	Accuracy:	85.1%	.ii
$al^{[45]}$, 2020		different			ii	training	training validation	cohort	1;
		treatment			cohort;	cohort; 89 and accuracy:	accuracy:	82.8%	ii
		responses	to		138 in	validation	138 in validation validation cohort 2	ohort 2	
		TACE in	HCC		cohorts	cohorts 1 and 2)			
		patients							
Peng et CT	Retrospective	Prediction) jo	of CNN	310 pat	ients (139	310 patients (139 AUC: 0.994		
al ^[46] , 2021		initial response to	nse to		ii	training			
		TACE in HCC	HCC		cohort;	cohort; 171 in			
		patients			validation	on			
					cohort)				
Wei et al ^[47] , CT	Retrospective	Prediction of OS CNN) SO J	NNC	167 patients	ients	C-index: 0.650 in cross	.650 in	cross
2021		of HCC patients	atients				validation		
		treated with SBRT	SBRT						
Liu <i>et al</i> ^[48] , US	Retrospective	Prediction of PFS		CNN	214 RF,	A patients	214 RFA patients C-index of RFA: 0.726; C-	RFA: 0.72	:6; C-
2020		of HCC patients	atients		(149 fo	(149 for training; index		of su	surgical

		treated with RFA	65 for	for resection: 0.726
		or surgical	validation),	
		resection	205 SR patients	
			(144 for training;	
			61 for validation)	
Wang et CT	Retrospective	Prediction of early ResNet	167 patients	AUC of best model: 0.825
al ^[49] , 2019		recurrence of		
		HCC patients		
Wang et CT	Retrospective	Prediction of early ResNet	167 patients	For the best model with
al ^[50] , 2020		recurrence of		joint loss function, AUC:
		HCC patients		0.8331; accuracy: 80.49%
He et al ^[51] , MRI and	and Retrospective	Evaluation of U-net,	109 patients (87 Total	Total accuracy: 82%;
2021 pathological		HCC recurrence CapsNet	for training; 22	recall: 80%; precision:
data		risk of liver	for testing)	89%; AUC: 0.87; F-1
		transplantation		score: 84%
		recipients		
Jiang et CT	Retrospective	Prediction of 3D-CNN	405 patients (324	405 patients (324 AUC: 0.906; sensitivity:
al ^[52] , 2021		microvascular	in training set, 81	75.7%; specificity: 93.2%;

		invasion status of	Jo			in validation set)	accuracy:	85.2%;	F-1
		HCC patients					score: 87.2% in validation	in validat	ion
							set		
Wang et CT	Retrospective	Prediction	Jo	of Transformer,		138 patients	For arterial phase images	phase ima	ses
al ^[53] , 2022		microvascular		CNN			in validation set, AUC:	n set, Al	JC:
		invasion status of	Jo				0.9223; Average accuracy:	age accura	ıcy:
		HCC patients					86.78%		
Fu <i>et al</i> ^[54] , CT	Retrospective	Prediction	Jo	of Modified l	5	U- 366 patients (281 AUC: 0.836 in validation	AUC: 0.836	in validat	ion
2021		macrovascular		Net		in training cohort	cohort		
		invasion status in	in			cohort, 85 in			
		HCC patients				validation			
						cohort)			

CT: Computed tomography; MRI: Magnetic resonance imaging; US: Ultrasound; HCC: Hepatocellular carcinoma; TACE:

Transarterial chemoembolization; PFS: Progression-free survival; RFA: Radiofrequency ablation; SBRT: Stereotactic body radiation therapy; CNN: Convolutional neural network; AUC: Area under the receiver operating characteristic curve; C-index: Harrell's concordance index; DLR: Deep-learning-based radiomics.

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Ref.	Imaging	Study design	Study aim	DL model	Dataset	Outcomes
Ziegelmayer et	CT	Retrospective	Identification	VGG19	86 patients (44 AIP	86 patients (44 AIP Sensitivity: 89%; specificity:
<i>al</i> ^[55] , 2020			of PDAC and		patients and 42	83%; AUC: 0.90
			AIP		PDAC patients)	
Liao et al ^[56] , CT	CT	Retrospective	Identification	CNN	3120 images (1872	3120 images (1872 Sensitivity: 89.9%; specificity:
2022			of PDAC, non-		for training, 624 for	for training, 624 for 91.3%; AUC: 0.960 when
			cancerous		validation, 624 for distinguishing	distinguishing between
			pancreatic		testing)	PDAC and control group
			diseases and			
			normal			
			pancreas			
Tong et al ^[57] ,	SN	Retrospective	Identification	ResNet-50	558 patients	AUC: 0.967; sensitivity: 87.2%;
2022			of PDAC and			specificity: 100%
			CP			
Watson et al ^[58]	CT	Retrospective	Prediction of	of LeNet	81 patients (65 for	81 patients (65 for AUC: 0.785; brier score: 0.174;
			pathologic		training and	sensitivity: 81.4%; specificity:
			response of		validation; 16 for	validation; 16 for 60.4% in test set of hybrid

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C-index: 0.76; Hazard ratio: IPA: 11.81%, C-index: 0.651 in 98 patients (68 in AUC: 0.81; Hazard Ratio: 1.86 deep learning model 9.46 in test set testing cohort training cohort; 30 in testing cohort) 520 patients 159 patients testing) Evaluation of AlexNet Evaluation of CNN Prediction of CNN of risk scores to PDAC patients probability of OS of PDAC Evaluation of patients with high or low PDAC patients PDAC patients distinguish patients; survival to NAC survival hazard Retrospective Retrospective Retrospective

Muhammad et CT

 $al^{[59]}$, 2018

Zhang et al^[60], CT

Zhang et all61], CT

	of 2. CNN 98 patients (68 in AUC: 0.84; specificity: 68%;	of training cohort; 30 sensitivity: 91%.	in testing cohort)	nts	of CNN 205 patients C-index: 0.705 for survival	risk prediction; balanced accuracy:	tumor 73.6%, sensitivity: 81.3%,	specificity: 65.9% for resection	of margin prediction		nts	of CNN 1209 patients C-index: 0.667 for survival	risk palanced accuracy:	tumor 67.1%; sensitivity:	specificity: 74.3% for resection	of margin prediction	
risk	Prediction of 2. CNN	yr OS	resectable	PDAC patients	Prediction of	survival risk	and tur	resection	margin	resectable	PDAC patients	Prediction of	survival	and tur	resection	margin	resectable
	ective				ective							ective					
	Retrospective				Retrospective							Retrospective					

		PDAC patients		
An <i>et al</i> ^[64] , CT	Retrospective	Prediction of ResNet-18 148 patients (88 in For combined model,	148 patients (88 in	For combined model,
2022		LNM status	training cohort, 25	training cohort, 25 AUC: 0.92; accuracy: 86%;
		and OS in	in validation cohort,	in validation cohort, sensitivity: 94%; specificity:
		PDAC patients	35 in testing cohort) 78% in testing cohort	78% in testing cohort
Li <i>et al</i> [65], 2019 CT	Retrospective	Prediction of CNN	111 patients	Average AUC score: 0.90;
		HMGA2 and C-		accuracy: 95%; sensitivity:
		MYC gene		92%; specificity: 98% in C-
		expression		MYC test with deep features
		status of PDAC		selected by Doctor B; average
		patients;		AUC score: 0.91; accuracy:
		Prediction of		88%; sensitivity: 89%;
		survival time		specificity: 88% in HMGA2
		of patients		test with deep features
				selected by Doctor B

CT: Computed tomography; US: Ultrasound; PDAC: Pancreatic ductal adenocarcinoma; AIP: Autoimmune pancreatitis; CP: 20 Chronic pancreatitis; NAC: Neoadjuvant chemotherapy; LNM: Lymph node metastasis; OS: Overall survival; AUC: Area under the

receiver operating characteristic curve; C-index: Harrell's concordance index; CNN: Convolutional neural network; IPA: Index of prediction accuracy; DLR: Deep-learning-based radiomics.

Table 5 Summary of studies using deep-learning-based radiomics for colorectal cancer

Table 5 Summary of Studies usin	of studies usi	ng deep-learning-based radiomics for colorectal cancer	d radiomics for co	lorectal cancer		
Ref.	Imaging	Study design	Study aim	DL model	Dataset	Outcomes
Wu <i>et al</i> ^[67] , 2020	CT	Retrospective	Predicting KRAS CNN	CNN	Primary	C-index of 0.815 for
			status in patients		cohort: 279	279 the primary cohort
			with CRC.		patients;	and 0.832 for the
					Validation	validation cohort
					cohort: 119	
					patients	
Wei <i>et al</i> ^[68] , 2021	CT	Retrospective	Predicting the	the ResNet10	192 patients	AUC of DLR: 0.820;
			response to			AUC of HCR: 0.598
			chemotherapy in			
			CRLM			
Zhang et al ^[69] , MRI	MRI	Retrospective	Predicting the	the MobileNetV2	491 patients	Accuracy: 85.4%;
2021			MSI status of			AUC: 0.868

	AUC of DLR: 0.73;	AUC of HCR: 0.64			C-index of 0.747 and	AUC of 0.894 in the	validation cohort			C-index: 0.649					AUC for training:	0.862; AUC for	validation: 0.920
	43 patients				235 patients					1028 patients					545 patients		
	VGG19				the ResNet18					of CNN+RNN					Faster RCNN		
CRC	Predicting	NCRT response	in patients with	LARC	Predicting the	distant	metastasis of	LARC patients	receiving NCRT	Prediction of	early on-	treatment	response in	mCRC	Prediction of	metastatic LN in	CRC
	Retrospective				Retrospective					Retrospective					Retrospective		
	MRI				MRI					CT					MRI		
	Fu <i>et al</i> ^[70] , 2020				Liu <i>et al</i> ^[71] , 2021					Lu <i>et a</i> l ^[72] , 2021					Ding et al ^{[73}], MRI	2020	

Zhao et al ^[74] , CT	Retrospective	Prediction	of of	Prediction of Autoencoder	423 patients	AUC	for	AUC for training:	÷.
2022		metastatic LN in	.ii			0.81;	AU	0.81; AUC for	H
		CRC				valida	tion: 0	validation: 0.73; AUC	()
						for testing: 0.77	ting: 0	.77	
Li <i>et al</i> ^[75] , 2020 MRI	Retrospective	Classification of AlexNet	of of	AlexNet	3364 samples Accuracy:	Accura	acy:	75.83%;	
		CRC LI	N		(1646 positive; AUC: 0.7941	AUC:	0.7941		
		Metastasis			1718 negative)				
		images							

CRC: Colorectal cancer; CT: Computed tomography; MRI: Magnetic resonance imaging; CRLM: Colorectal liver metastases; MSI: Microsatellite instability; NCRT: Neoadjuvant chemoradiotherapy; LARC: Locally advanced rectal cancer; mCRC: Metastatic colorectal cancer; LN: Lymph node; CNN: Convolutional neural network; RNN: Recurrent neural network; AUC: Area under the receiver operating characteristic curve; C-index: Harrell's concordance index; DLR: Deep-learning-based radiomics; HCR: Handcrafted radiomics; Faster R-CNN: Faster region-based convolutional neural network.

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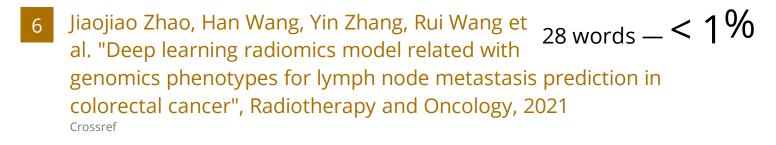
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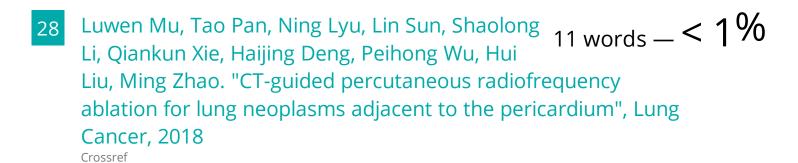
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