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Factors other than fibrosis that increase measured shear wave velocity

Naganuma H *et al.* Factors that increase SWV

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Abstract

Shear wave elastography is now becoming an indispensable diagnostic tool in the routine examination of liver diseases. In particular, accuracy is required for shear wave propagation velocity measurement, which is directly related to diagnostic accuracy. It is generally accepted that the liver shear wave propagation velocity reflects the degree of fibrosis, but there are still few reports on other factors that increase the shear wave propagation velocity. In this study, we reviewed such factors in the literature and examined their mechanisms. Current shear wave elastography measures propagation velocity based on the assumption that the medium has a homogeneous structure, uniform density, and is purely elastic. Otherwise, the measurement is subject to error. The other (confounding) factors that we routinely experience are primarily: (1) Conditions that appear to increase the viscous component; and (2) Conditions that appear to increase tissue density. Clinically, the former includes acute hepatitis, congested liver, biliary obstruction, *etc*, and the latter includes diffuse infiltration of malignant cells, various storage diseases, tissue necrosis, *etc*. In any case, it is important to evaluate shear wave elastography in the context of the entire clinical picture.

Key Words: Liver; Shear wave elastography; Propagation velocity; Artifact; Viscoelasticity; Ultrasound

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Core Tip: Shear wave elastography has become an indispensable diagnostic tool for diagnosing liver disease patients. The shear wave propagation velocity usually reflects the degree of fibrosis, but we must keep in mind other (confounding) factors. The confounding factors due to viscosity include acute hepatitis, congestive liver, and biliary stasis. The other confounding factors due to an increase of tissue density include diffuse infiltration of malignant cells, various stage diseases, and tissue necrosis. It is important to judge shear wave elastography results in the context of the entire clinical picture.

INTRODUCTION

Percussion examination has been historically performed as part of physical examinations and is clinically important^[1]. It is a method of investigating the mechanical characteristics of internal organs through the changes in reflected sound during percussion to recognize how internal organs respond to vibrations. This phenomenon indicates that the sound of reflection is related to tissue stiffness, and it provides useful diagnostic information of tissues. Elastography (stiffness measurement technique) scientifically confirmed this subjective experience-based phenomenon. In recent years, various ultrasound (US) and magnetic resonance elastography techniques for evaluating tissue elasticity have been developed and applied in the clinical setting^[2,3]. The basic principle of these techniques is to use external vibration (or focused US) to create shear waves (SWs) in the tissue and to measure the SW propagation velocity as a function of time and distance^[4,5]. Many algorithms then calculate the SW propagation velocity, based on the assumption that the tissue is unstressed, homogeneous, isotropic, and purely elastic. Under these conditions, the SW velocity is directly related to the elastic modulus of the tissue^[6,7].

Presently, magnetic resonance elastography^[2,3] and US elastography^[8,9] are primarily used. The former is used for detailed examination due to its excellent stability and reproducibility^[2,3]. However, it is bulky and costly. US elastography has attained preferential use in the clinical setting because of its lower cost and easier manipulability of the instrument^[10,11].

Currently, there are three kinds of US-based SW elastography (SWE), namely transient elastography^[12], point SWE^[13], and two-dimensional SWE (2DSWE)^[14,15]. Among these methods, 2DSWE has emerged as the most frequently used diagnostic technique due to its ability to sample a large area in the liver, change the sampling area quickly under B-mode observation, and display color mapping of SW values over the B-mode image, which gives the operator a sense of security. Recently, various 2DSWE devices have been developed by a number of US companies^[16,17], and there have been many studies on the relationship between 2DSWE and liver histology that have shown a high degree of agreement, with the area under the receiver operating characteristic curve of 2DSWE performance of more than 0.9 in the prediction of fibrosis staging^[18,19]. This indicates that 2DSWE can be a useful and accurate tool for evaluating liver stiffness. The precise definition of “increased SW propagation velocity” is not strictly determined, but the reported optimal cutoff values to differentiate liver cirrhosis are approximately 9 kPa (1.7 m/s) in most cases^[20]. Thus, measurements above this threshold are considered increased values.

There are two ways to quantify relative tissue stiffness as SW propagation velocity expressed as m/s and as kPa. The SW propagation velocity is converted automatically to kPa, using the equation $1 \text{ kPa} = 3 \cdot P \cdot (\text{SW propagation velocity})^2$, with the assumption that the examined tissue is always homogeneous, and P (tissue density) is defined as 1.00 kg/m^3 .

THEORETICAL BASIS OF 2DSWE

Existing studies regarding 2DSWE of the liver included various manufacturers and models^[21]. A detailed explanation of the complex working principles of recent SWE

devices in each company is beyond the scope of this review. Despite variations in employed algorithm, the fundamental operating principles of these devices are similar^[21].

The push-pulse produces small tissue movements in the push-pulse plane. These tissue movements produce SWs that propagate and produce minimal tissue movements in the horizontal plane of the push-pulse. The tissue movements in the horizontal plane are called "SWs" and further propagate through the tissue in a sideways direction, away from the push-pulse. The SW movements are tracked by the regular-interval tracking conventional US pulses, which are used to measure the arrival time of SWs (Figure 1). The simple formula to determine the SW velocity is arrival time of SW/distance from the push-pulse. This measurement is possible because the SW propagation velocity is very low (1-10 m/s) compared to the velocity of US pulses (1540 m/s)^[22].

MEASUREMENT OF SW PROPAGATION VELOCITY IN LIVER TISSUE

For SW propagation velocity measurements, assumptions are made that the tissue is homogeneous, perfectly elastic (no viscous component), and the SW propagates in a straight direction^[23,24]. The normal liver is the closest to this condition of all organs, and it is not surprising that a large number of papers have been focused on liver disease^[9]. Generally speaking, the factors that increase the SW propagation velocity include an increase in cell density and heterogeneous tissue structure^[23,24].

Reports on fiber components and SW propagation in muscles have observed that the SW propagation velocity increases when SWs propagate along the fiber running in the muscle^[25,26]. This is an important factor in the increase in SW propagation velocity due to SW propagation of fibrosis in the liver tissue.

OTHER FACTORS LEADING TO INCREASED HEPATIC SW PROPAGATION VELOCITY

In SWE, tissue stiffness is estimated by measuring the SW propagation velocity^[23,27]. Fibrotic tissues are typically stiffer than normal tissues. Therefore, the SW propagation

velocity in fibrotic tissue is naturally faster than in normal tissue. Presently, there are many successful demonstrations of SWE in assessing the severity of liver fibrosis showing a significantly high correlation between the progress of fibrosis and increase in SW propagation velocity in patients with chronic viral hepatitis^[9]. Although there are a relatively small number of publications, increased hepatic SW propagation velocity has been reported due to factors other than fibrosis, including acute, hepatitis^[28], cholestasis^[29,30], hepatic congestion^[31], storage disease^[32], hepatic necrosis^[33], and diffuse infiltration of malignant tumors^[34].

As mentioned in the previous section, the current SW propagation velocity measurement is performed on the assumption that the tissue to be measured is a perfect elastic body. However, the liver is indeed “viscoelastic,” and current SWE measures elastic components and viscous components without distinction. This is thought to be the main cause of increased SW propagation velocity seen in acute hepatitis, hepatic congestion, and biliary congestion^[28,30,31]. On the other hand, increased SW propagation velocity in storage disease, necrosis (Figure 2), or diffuse infiltration of malignant tumors are related to increased tissue density^[34].

INCREASED HEPATIC SW PROPAGATION VELOCITY IN CHOLANGITIS AND SIMILAR PATHOLOGIC CONDITIONS

The main target of current hepatic SWE is various chronic hepatic diseases, particularly viral hepatitis^[9]. Presence of parenchymal fibrosis is considered to be the main cause of increased SW propagation velocity. However, it indicates that similar phenomena can be observed in other pathologies with increased fibrosis within the liver parenchyma.

In patients with chronic cholangitis, it has been reported that the SW propagation velocity in the peripheral liver tissue, in which the tubular structure is invisible on B-mode imaging, is increased^[35,36]. It is presumed that fibrotic peripheral bile ducts are distributed throughout the liver and form an environment similar to fibrosis of chronic hepatitis for SW propagation. Increased SW propagation velocity can be observed in patients with von Meyenburg complex (Figure 3). von Meyenburg complex is a benign

developmental ductal plate malformation affecting the small peripheral bile ducts^[37]. In addition, cases of thickened-wall peripheral small vessels can increase SW propagation velocity in patients with hereditary hemorrhagic telangiectasia (also known as Rendu-Osler-Weber disease)^[38] (Figure 4). Hepatic involvement in hereditary hemorrhagic telangiectasia is characterized by diffuse development of small vascular shunts in the hepatic periphery, which likely increases SW propagation velocity^[38].

ARTIFACTUAL INCREASE IN SW PROPAGATION VELOCITY DUE TO EXAMINATION TECHNIQUES

Measurement of SW propagation velocity can be easily performed using 2DSWE, but it is well known that the results change according to the level of expertise of the ultrasound operator^[39]. The literature includes reports of artifactual factors that give rise to pseudo-increased SW propagation velocity, including a reverberation artifact (Figure 5A), motion artifact due to cardiac motion (seen in the left lobe of the liver) (Figure 5B), and excessive probe compression during subcostal scanning (Figure 5C). However, the possibility of misinterpretation of these artifacts by an experienced SWE practitioner is extremely rare because the patterns produced by the artifacts are characteristic and recognizable.

For example, there are some studies in the literature comparing SWE results of the left lobe and the right lobe of the liver^[40]. However, current guidelines, including the World Federation for Ultrasound in Medicine and Biology and the European Federation for Ultrasound in Medicine and Biology, recommend SW measurement through the right intercostal space only because SW measurements obtained in the left lobe are usually affected by cardiac movement^[8,41].

Recent clinical studies have used SWE to evaluate fatty liver (FL) stiffness. Unfortunately, there is a lack of understanding of the biomechanics of SWE to assess patients with FL due to the complexity of the structure of FL. Unlike the normal liver whose structure may be modeled as isotropic, FL has a heterogeneous structure. The complex structure and mechanical properties present a challenge in obtaining accurate

results of SW propagation velocity^[42]. It is not so rare to encounter artifactually (pseudo) increased SW propagation velocity when observing FL (Figure 5D). The various factors that affect propagation of SW waves in FL need to be properly understood before SWE can be used for accurately assess the severity of FL.

OTHER REPORTED PHYSIOLOGICAL FACTORS THAT INCREASE SW PROPAGATION VELOCITY

Although the precise mechanisms are undetermined, studies have shown that a reduction in blood flow typically results in a decrease in SW propagation velocity in the liver^[43]. In contrast, SW propagation velocity tends to increase with increasing organ perfusion. Other reported factors that change SW propagation velocity include water intake^[44], breathing phases^[45], eccentric exercise, patient positioning^[46], and high calorie meal intake^[47]. These factors can potentially contribute to minimal fluctuations in SW measurements, and care should be taken to account for these fluctuations to reduce the degree of uncertainty.

DISCUSSION

Presently, SWE is routinely used for providing a quantitative evaluation of liver elasticity^[7]. The SW propagation velocity measured is reflective of the biomechanical properties of liver tissue where a higher value usually reflects stiffer (*i.e.* fibrotic) parenchyma^[8,9]. SWE algorithms assume that the liver is purely elastic and homogeneously structured. In most cases these assumptions are true. However, other factors may increase SW propagation velocity. They include acute hepatitis, cholestasis, hepatic congestion, storage disease, hepatic necrosis, and diffuse infiltration of malignant cells and others (Figure 6). Among them, the problem of viscosity (related to acute hepatitis, cholestasis, and hepatic congestion) is the most important because most commercial SWE systems assume soft tissues to be purely elastic and neglect the effects of viscosity when evaluating liver tissue stiffness.

However, the liver tissue is a viscoelastic environment that results in a counterbalance of liver tissue stiffening^[48,49]. When the liver tissue is modeled as a viscoelastic material, the SWs experience frequency dispersion. The SW propagation velocity and SW attenuation increases with increasing frequency rather than remaining constant, and the rate of change (slope) is positively correlated with viscosity^[50-52]. As a result, modeling a viscoelastic material as linear elastic tends to overestimate the SW propagation velocity. When the effects of viscosity are considered, the scope of the diagnostic technique can be further broadened, and SW dispersion provides an estimation of liver viscosity, which may provide additional information of the underlying liver parenchyma.

Recent studies have reported that viscosity alone can serve as a parameter to diagnose several medical conditions such as inflammation and congestion^[48,49]. Although only one company has developed this type of SW dispersion device, it is expected to be an area of great potential for further development. An increase in tissue density is another confounding factor that often poses a challenge in obtaining reliable and accurate SWE readings. However, many problems remain that must be clarified in future studies.

Currently, automated diagnostics incorporating artificial intelligence are spreading rapidly worldwide^[54,56]. SWE is a likely area in which artificial intelligence could be easily utilized. The adoption of artificial intelligence for SWE measurements is expected to correct slight variances in reference values (normal range) among manufacturers and enable prediction of liver fibrosis with higher probability. Artificial intelligence may also be able to detect when the probability of contamination by a confounding factor is high.

CONCLUSION

Although many confounding factors are recognized, our review emphasized that the interpretation of 2DSWE results must incorporate knowledge of these factors. As the

use of 2DSWE becomes widespread, the problems related to confounding factors need clarification and solutions.

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