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**Liver metastases: the role of magnetic resonance imaging**

Maino C *et al.* Liver metastases: the role of MRI

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**Abstract**

The liver is one of the organs most commonly involved in metastatic disease, especially due to its unique vascularization. It's well known that liver metastases represent the most common hepatic malignant tumors. From a practical point of view, it's of utmost importance to evaluate the presence of liver metastases when staging oncologic patients, to select the best treatment possible, and finally to predict the overall prognosis. In the past few years, imaging techniques have gained a central role in identifying liver metastases, thanks to ultrasonography (US), contrast-enhanced computed tomography (CT), and magnetic resonance imaging (MRI). All these techniques, especially CT and MRI, can be considered the non-invasive reference standard techniques for the assessment of liver involvement by metastases. On the other hand, the liver can be affected by different focal lesions, sometimes benign, and sometimes malignant. On these bases, radiologists should face the differential diagnosis between benign and secondary lesions to correctly allocate patients to the best management. Considering the above-mentioned principles, it's extremely important to underline and refresh the broad spectrum of liver metastases features that can occur in everyday clinical practice. This review aims to summarize the most common imaging

features of liver metastases, with a special focus on typical and atypical appearance, by using MRI.

**Key Words:** Liver metastases; Magnetic resonance imaging; Gadolinium; Gd-EOB-DTPA; gadoxetate disodium; Liver specific contrast agents; Hepatobiliary contrast agents

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**Core Tip:** To better detect liver metastases, MRI protocol should be correctly performed, using extra-cellular (ECA) or hepatobiliary (HBA) contrast agents. Even if conventional non-enhanced techniques can help depict focal liver lesions, contrast-enhanced sequences are mandatory, to evaluate their behavior in comparison to the healthy liver parenchyma. These aspects allow to determine liver and hepatic lesions' vascularization over time and increase radiologists' diagnostic values. The typical appearance of liver metastases can be easily recognized as hypovascular lesions. However, some primary tumors can produce liver metastases with atypical appearances, such as hypervascular ones, or within calcification, mucin, or other proteins. The multiparametric nature of MRI, combined with the administration of contrast agents, can strongly increase radiologists' confidence in the final diagnosis.

## **INTRODUCTION**

The liver is one of the most common sites of metastatic disease, accounting for up to 25% of all secondary lesions to solid organs due to its unique architectural and vascular composition that provides fertile soil for different primary neoplasms to spread. Consequently, metastases represent the most frequent malignant liver tumors, being about 18-40 times more frequent than primary hepatic neoplasms<sup>[1]</sup>. Cancers from the

gastrointestinal tract, breast, lung, pancreas, neuroendocrine tumors, and melanomas commonly spread to the liver<sup>[2,3]</sup>. Specifically, colorectal cancers (CRCs) are widespread, as 50% of such patients presenting with metastatic liver disease at diagnosis or during the follow-up after surgery<sup>[4]</sup>.

Metastatic spread to the liver represents one of the major prognostic factors, determining the clinical outcome<sup>[5,6]</sup>. Surgical resection is considered the treatment option with the best curative potential for liver metastases. In the case of unresectable disease, besides systemic chemotherapy, many liver-directed approaches have been developed, including local therapies, such as stereotactic body radiation therapy (SBRT) or radiofrequency ablation (RFA), and regional therapies, like peptide receptor radionuclide therapy (PRRT), hepatic artery directed infusional chemotherapy (HAI), trans-arterial chemoembolization (TACE) and trans-arterial radioembolization (TARE)<sup>[7]</sup>. Hence, accurate detection and assessment of secondary liver lesions are pivotal to select the most tailored management approach for each patient and to determine in whom an improved overall survival rate may be expected.

Magnetic Resonance Imaging (MRI) represents the reference standard radiological technique for the detection of liver metastases, with its higher sensitivity and specificity compared to computed tomography (CT) and fluoro-2-deoxyglucose positron emission tomography (FDG-PET)<sup>[8,9]</sup>. The evaluation of secondary liver lesions is one of the most common clinical indications for liver MRI in radiologists' daily practice.

On these bases,<sup>6</sup> the aim of this review is to summarize the role of MRI in the detection and assessment of liver metastases, describing their main imaging features and focusing on the added value of the most recent imaging tools.

## **MR PROTOCOLS**

A comprehensive MRI protocol for liver metastases detection and follow-up after systemic, surgical or locoregional treatments should include the acquisition of T1- and T2-weighted sequences, diffusion weighted imaging (DWI) sequences, dynamic multiphase and/or delayed sequence after intravenous administration of gadolinium-

based contrast agents (GBCA). GBCAs, with intravascular-interstitial distribution, are generally used with T1-weighted sequences, with or without fat suppression techniques. Dynamic contrast enhanced acquisitions improve the identification and characterization of liver metastases depending on their enhancement behavior<sup>[10]</sup>.

The introduction of hepatocyte-specific GBCAs, notably Gd-BOPTA (gadobenate dimeglumine - MultiHance®, Bracco) and Gd-EOB-DTPA (Gadoxetic acid, disodium - Primovis®/Eovist®, Bayer), has increased more and more MRI sensibility and specificity for liver metastases imaging. These GBCAs are taken up by hepatocytes and excreted in the biliary system and they are extremely valuable in follow-up after locoregional or systemic treatments. These molecules present a biphasic enhancement pattern; the first phase, immediately after intravenous injection, is similar to CT dynamic enhancement after iodine contrast injection while a delayed phase occurs after 10 to 120 min after injection<sup>[10,11]</sup>. Lesions not containing hepatocytes cannot take up such molecules; therefore, metastasis appear hypointense compared with surrounding healthy liver parenchyma<sup>[12]</sup>.

Super paramagnetic iron oxide (SPIO) iron-based nanoparticles contrast media were withdrawn from the market in western countries even if they are still used in clinical practice in some oriental countries such as Japan; the target of this class of contrast agents are reticuloendothelial cells (RES)<sup>[10]</sup>.

In clinical practice, MRI liver protocols must be adapted to the patient's specific clinical questions and characteristics<sup>[13]</sup>.

It is recommended to acquire slices as thin as possible (i.e. 3-5 mm), with rectangular field of view (FOV) appropriated to the habitus of the patient. Acquisition plans must include at least axial and coronal. Matrices may vary depending on the sequences used; they should be as high as possible bearing in mind contrast-to-noise ratio. A higher spatial and contrast resolution may be obtained employing 2D and 3D T1w sequences. Temporal resolution is related to the length of acquisition time of a single MRI scan, according to patient's compliance<sup>[10]</sup>.

With modern MRI scanners, the possibility to acquire multiple arterial phases allows either to improve spatial resolution or to reduce scanning time, which is important in case of patients with limited breath-hold capacity or in pediatric ones<sup>[10,11]</sup>.

## NON-CONTRAST ACQUISITION

### Gradient-echo T1 in-phase and out-of-phase

GRE sequences are prone to susceptibility and chemical shift artifacts and such property may be used to detect and quantify iron and fat deposition within liver parenchyma or in focal lesions<sup>[14]</sup>. Chemical shift artifacts are due to the lower precession frequency of fat protons compared to water ones<sup>[15]</sup>. Such differences result in periodic phase coherence (*in-phase*), where every voxel signal is the sum of water and fat signal or opposition (*out-of-phase*) of water and fat signals, whereas the two signals have a phase difference of 180°, and thus nulling each other out<sup>[16]</sup>. Such sequences permit the detection of intracellular fat, either in hepatic lesions or in the hepatic parenchyma<sup>[14,16]</sup>.

### Fast spin-echo (FSE) or turbo spin-echo (TSE) T2 sequences, with or without fat-suppression

They are very rapid sequences; at present also acquired by breath-hold technique. They are characterized by a 90° excitation pulse followed by a train of several 180° refocusing pulses to fill several K-space lines (echo train) during a repetition time. Fluid content is the predominant information obtained from this kind of sequences, thus allowing to discriminate between solid and cystic-like focal lesions. Fat-suppression should be regularly used to increase contrast resolution<sup>[16]</sup>.

### Diffusion-weighted imaging (DWI)

They are basically T2-weighted images, acquired with single shot, echo planar (EPI) technique and fat-suppression. They are crucial to rapidly acquire the diffusion signal

before it nulls<sup>[10,17]</sup>. Different series of diffusion-weighted images are obtained by modifying the gradient strength and magnitude (b-value). One series must be acquired with a b-value of 0, so that no gradient is applied and consequently no diffusion information is present, providing similar information as T2 fat-sat sequences. Other series must be acquired with increasing b-values (b50, b400, b800)<sup>[18]</sup>. These are fundamental for secondary lesion detection, as there is a “black-blood” effect, which increases conspicuity of lesions located next to the vessels. Series acquired with a high b-value (b800) are essential for liver lesion characterization: highly cellular tissues, such as metastases, present restriction to diffusion thus appearing hyperintense in DWI images<sup>[17,18]</sup>. EPI sequences are prone to motion artifacts: breath-hold scans have the advantage of reduced blurring and ghosting artifacts, however their short acquisition times limit spatial resolution, the number of excitations, and number of possible b-values<sup>[17,18]</sup>. On the other hand, navigator or respiratory-triggered techniques improve image signal-to-noise ratio at higher b-values, reducing motion artifacts and blurring<sup>[14]</sup>.

## POST-CONTRAST ACQUISITION

### Dynamic evaluation

Gradient-echo 2D or 3D T1 sequences with or without fat-suppression, acquired before and after gadolinium-based contrast agent administration<sup>[19]</sup>. T1-weighted sequences are very sensitive to susceptibility artifacts thus enabling to detect iron, calcium, air or metal<sup>[16]</sup>. 3D sequences are being used more and more frequently, they are acquired with a modified Dixon technique, that explores the chemical shift effect of fat and water, allowing to separate fat and water peaks allowing to improve the homogeneity of the images, fat-suppression, and providing thinner slice thickness and slice overlap<sup>[16]</sup>. GRE 3D T1-weighted fat-sat sequences (LAVA, VIBE, THRIVE, etc.) are the classical sequences used for dynamic contrast-enhanced studies to evaluate the vascularization pattern of the lesion, usually acquiring one dynamic phase for each breath-hold, about every 25-30 s<sup>[19]</sup>.



At present time, some techniques (CAIPIRINHA, TWIST-VIBE, DISCO or THRIVE 4D sequences, *etc.*), based on parallel imaging and compressed sensing, allow to obtain multi-arterial acquisition in one breath-hold<sup>[20]</sup>. Non-Cartesian acquisition schemes, for example radial sampling, may be performed for dynamic studies jointly with compressed sensing and parallel imaging, further increasing temporal resolution permitting free-breathing dynamic evaluation (Siemens GRASP VIBE sequences), with reduced motion artifacts, in a sort of continuous acquisition<sup>[19,20]</sup>.

Hepatobiliary-reticuloendothelial phases are T1-weighted sequences, with or without fat-sat, if Gd-BOPTA or Gd-EOB-DTPA, both increasing T1 relaxivity, have been administered<sup>[12,19]</sup>. Proton density or T2w sequences are used with SPIOs contrast agents<sup>[12,19]</sup>. For Gd-BOPTA, hepatobiliary phase imaging is recommended after 90-120 min, thus requiring the patient to return to the scanner for final T1-weighted imaging of the liver and bile ducts<sup>[11,12]</sup>. For Gd-EOB-DTPA, hepatobiliary phase acquisition may be performed after 20 min, while the patient is still on the scanner <sup>[5,12]</sup>. On hepatobiliary phase there is an increase in signal intensity of the hepatic normal parenchyma compared to a non-hepatocytic lesion, thus improving MR sensibility in detection and characterization of different types of liver lesion<sup>[5,10,12]</sup>. Furthermore, increasing the flip angle of a T1-weighted 3D sequence from 10° to 30° (Siemens scanner 1.5 T) in the hepatobiliary phase, visually and quantitatively improves the visualization of the biliary ducts, obtaining high quality hepatobiliary images<sup>[21]</sup>.

### **Additional sequences**

**6** HASTE (Half-Fourier Acquisition Single-shot Turbo spin Echo), heavily T2-weighted, with a rapid acquisition time, and acquired *via* breath-hold technique. They are used mainly to evaluate lesions or structures with prominent fluid content: they are the basic sequences for the evaluation of biliary tree and pancreatic ducts (MR colangiopancreatography)<sup>[22]</sup>.

Balanced steady-state GRE (true FISP, FIESTA, balanced fast field echo). They tend to highlight fluid content providing a highly accurate morphologic imaging as well as a



good delineation of vessels and ductal structures. Furthermore, due to their extremely rapid acquisition time (200 ms), these sequences can tolerate optimally motion artifacts. Other additional sequences might be added on a case-by-case basis (sequences for fat and iron overload quantification)<sup>[8,9,11]</sup>.

## **CONCLUSION**

Liver metastases are the most common malignant hepatic tumors occurring in everyday clinical practice, particularly during MR examinations. MRI, thanks to its multiparametric approach, can help radiologists to correctly evaluate and characterize liver metastases, reaching a fitted approach for each patient. The wide spectrum of liver metastases should be well-known, especially in the case of atypical appearance. The usefulness of HBAs, especially Gd-EOB-DTPA, has been widely demonstrated in the international literature and should be adopted whenever a liver MRI in patients with known primary tumors is required. Finally, MRI diagnostic accuracy can reach high values, representing nowadays the non-invasive reference standard technique to stage, re-stage and evaluate the prognosis of cancer patients with secondary liver involvement.

Future directions should be focused firstly on the usefulness of MR as a prognostic tool in patients with liver metastases. Moreover, the integration of AI techniques, especially machine and deep learning models, should be considered to identify liver metastases and to enhance radiologists' confidence in the final diagnosis.

## **ADVANCED TOOLS: RADIOMICS AND ARTIFICIAL INTELLIGENCE**

Radiomics, which uses artificial intelligence (AI) techniques to extract and analyze quantitative features from medical images, has been proven as an effective tool in medical imaging to improve detection and characterization of diseases in terms of diagnosis and prognosis. These algorithms can analyze image patterns, extract meaningful features, and make predictions based on the data, providing valuable insights to clinicians. Among different clinical applications, radiomics has been

proposed by researchers to face different challenges regarding liver metastases, mostly using CT images. Different algorithms have been proposed for diagnosis, prediction of development of liver metastases, response to therapy, recurrence, and survival<sup>[94]</sup>.

AI applied to CT images has shown excellent results in detecting liver metastases with a sensitivity of 93%<sup>[95]</sup> and in making differential diagnosis between liver metastases from other liver lesions, reaching an accuracy of 92%<sup>[96]</sup>. Moreover, some studies assessed the feasibility of using radiomics for response prediction to therapy at lesion level also demonstrating the superiority of radiomic features compared to the standard biomarkers, such as size and RECIST<sup>[97]</sup>.

Despite CT being the diagnostic tool most often used during staging and follow-up, and consequently, the one for which it is easier to develop radiomics tools, MRI is the only technique that allows providing quantitative data to assess morphological and functional information useful for tumor characterization and prediction of response to treatment. Therefore, efforts have been made to correlate MRI-based radiomics data to clinical outcomes. Zhang *et al*<sup>[98]</sup> demonstrated that radiomics features derived from pre-treatment T2 weighted images can correlate with response to chemotherapy, *e.g.*, responding lesions showed a lower angular second moment and higher variance (two homogeneity measures) compared to non-responding ones. Similarly, but using post-treatment MRI features, Reimer *et al*<sup>[99]</sup> demonstrated that higher kurtosis on arterial and portal-venous images and higher skewness in portal-venous phase could identify patients undergoing TARE with a progressive disease earlier compared to standard RECIST criteria. However, when radiomics features are combined into statistical classifiers, *e.g.*, in a multivariate analysis, predictive performances are boosted. For example, Granata *et al*<sup>[100]</sup> proven that combining some radiomics features obtained from T2 weighted images into a statistical classifier, such as the KNN, allows predicting the tumor growth with an AUC of 0.9 in the validation set. Han *et al*<sup>[101]</sup> developed a model to preoperatively identify Histopathological Growth Patterns (HGP) of CRC liver metastases, analyzing the tumor-liver interface zone on MR, reaching an AUC of 0.91 in the cohort of internal validation.

Radiomics has also shown promising results on MRI<sup>4</sup> in the diagnostic field of research, distinguishing different types of liver lesions, and differentiating secondary lesions from benign lesions and primary liver cancer<sup>[102]</sup>. Finally, an important objective that has been pursued with radiomics is the correlation between radiomics and genomics through an approach called radiogenomics. Using MR-based radiomics features, Granata *et al*<sup>[103]</sup> assessed the RAS mutation status, a robust prognostic and predictive biomarker among subjects undergoing liver CRC metastases resection. They performed a multivariate analysis using features extracted from MRI, obtaining an accuracy of 87.5% with 91.7% of sensitivity and 83.3% of specificity on an external validation cohort in predicting RAS mutational status. Despite these promising results, further studies should be conducted to face important challenges such as<sup>4</sup> the instability of radiomic features among different devices and acquisition protocols, especially for MRI images, lack of fully automatic segmentation tools and user-friendly interfaces<sup>[104]</sup>, and shortage of well-annotated multicenter datasets. The latter can be overcome by designing clinical trials enhancing the cooperation between institutions and collaborations between clinicians and medical imaging experts.

### **THE ADDED VALUE OF GD-EOB-DTPA**

Since its introduction, Gd-EOB-DTPA acquired a key role in characterization of malignant liver lesions, especially metastasis, and in evaluating response to therapy. One of the most important published randomized multicenter trials (VALUE)<sup>2</sup> demonstrated the superior diagnostic accuracy of Gd-EOB-DTPA, compared to ECAs-MRI and CT, in patients with suspected CRC liver metastases. The Authors demonstrated that no additional imaging was required for all patients who underwent EOB-MRI, while for patients who underwent ECA-MRI and CT further confirms were needed (in 17% and 39% of cases, respectively,  $p < 0.0001$ )<sup>[86]</sup>.

An important systematic review and meta-analysis showed<sup>2</sup> the higher per-lesion sensitivity of Gd-EOB-DTPA MRI in comparison to CT (median 94.9% vs. 74.2%, respectively,  $p < 0.001$ ). Higher diagnostic values of EOB-MRI were also demonstrated

for small lesions (with an axial diameter <1 cm), with a per-lesion sensitivity of 85.7% (vs 50%,  $p<0.001$ )<sup>[87]</sup>.

Vilgrain *et al*<sup>[33]</sup> published a meta-analysis regarding 1989 patients with 3854 Liver metastases to analyze diagnostic values of DWI and HPB acquired with Gd-EOB-DTPA alone and a combination of both. When considered singularly, HBP was more sensitive than DWI to detect liver metastases (90.6% vs 87.1%). However, the combination of both sequences showed the highest per-lesion sensitivity (95%,  $p<0.0001$ ).

Interestingly, Zech *et al*<sup>[88]</sup> evaluated the cost of the diagnostic workup of CRC liver metastases patients, three different imaging approaches were compared: EOB-MRI, ECA-MRI, and CT. Overall costs were lower when using Gd-EOB-DTPA as the first line imaging technique compared to different strategies. Indeed, no patient in the EOB-MRI group required supplementary imaging to decide on treatment as compared to 18.1% and 39.7% for patients who underwent ECAs-MRI and CT, respectively. To endorse these aspects, Renzulli *et al*<sup>[89]</sup> suggested that EOB-MRI should be the initial imaging modality of choice for patients pre-operatively evaluation.

Kim *et al*<sup>[90]</sup> studied the importance of EOB-MRI compared to CT in CRC patients with synchronous liver secondary lesions. They found out that EOB-MRI increased the detection of liver secondary lesions, helping a more fitted treatment, with an overall increase in survival rate (estimated 5-year survival of 70.8% for EOB-MRI vs 48.1% for CT).

EOB-MRI has also proved useful for predicting therapeutic responses. Recently, Gu *et al*<sup>[91]</sup> evaluated whether some HBP parameters, such as the relative tumor enhancement (RTE) and the standard deviation value of signal intensity ratio (SDR), can predict the pathological response to systemic therapy in CRC liver metastases. RTE and SDR values were significantly higher in the responder group in comparison with the non-responder one ( $p<0.001$ ).

Similarly, Murata *et al*<sup>[92]</sup> demonstrated that the mean pre-treatment RTE was significantly higher in responders in comparison with the non-responder group (37.2% ± 10.9% vs 17.9% ± 10.5%,  $P = 0.0006$ ). Larger and prospective studies should aim to

better evaluate the usefulness of EOB-MRI as a prognostic factor in patients with liver metastases.

Finally, EOB-MRI is even worthwhile in the assessment of chemotherapy-induced liver disease, as in the case of sinusoidal obstruction syndrome (SOS), especially during the early stages. The under-expression of OATP by centrilobular hepatocytes reflects the reticular hypointensity appearance on HBP which can be more easily detected than with conventional MRI sequences<sup>[89,93]</sup>.

### **USEFULNESS OF DWI**

The most sensitive MRI sequences to detect liver metastases are DWI and HBP images. Diffusion restriction and HBP hypointensity are typical features of liver secondary lesions<sup>[67]</sup> (**Figure 7**).

DWI technical principles are based on the evaluation of water molecules' motion and is currently used in clinical practice to assess lesions and tissue properties<sup>[67,68]</sup>. Specifically, b-values are DWI-related parameters able to assess the degree of diffusion of a specific lesion or tissue<sup>[69]</sup>.

Considering that water diffusion in highly cellular tumors is more restricted compared to healthy tissues, a higher b-value might null signals from healthy tissues, resulting in marked cancer-to-healthy tissue contrast, thus leading to lesion hyperintense signals<sup>[68,69]</sup>. The diagnostic values of high b-values have been investigated and reported in several tumors, including liver metastases<sup>[70]</sup>. An important meta-analysis reported 87.1% (95 % CI, 83.2- 90.1 %) sensitivity for DWI in liver metastases detection<sup>[33]</sup>. Moreover, different studies showed that DWI was more sensitive than T2-weighted images for CRC liver metastases<sup>[71-73]</sup>. In particular, it has been underlined the essential role of DWI, despite the very low spatial resolution, in the detection of small ( $\leq 1$  cm) lesions<sup>[74]</sup>.

The second most important parameter obtained by DWI is the apparent diffusion coefficient (ADC) map, which correlates with tissue cellularity, relying on the mono-exponential model<sup>[69]</sup>. ADC values can help not only to characterize lesions but also to



predict prognosis. Two meta-analyses established that ADC values might contribute to response to chemotherapy evaluation and prediction in CRC liver metastases<sup>[75,76]</sup>. Specifically, Drewes *et al*<sup>[76]</sup> demonstrated that the pre-treatment mean ADC in responder group was lower compared to the non-responder group ( $1.15 \times 10^{-3} \text{ mm}^2/\text{s}$  vs  $1.37 \times 10^{-3} \text{ mm}^2/\text{s}$ , respectively). Similarly, Sobeh *et al*<sup>[75]</sup> demonstrated that the most robust response predictor to therapy was a lower baseline ADC value with a pooled mean difference of  $-0.12 \times 10^{-3} \text{ mm}^2/\text{s}$  among responders and non-responders. To strengthen these data, a systematic review confirmed that ADC value might be a promising tool for response to chemotherapy prediction in CRC liver metastases<sup>[77]</sup>. Moreover, the assessment of ADC values might be useful for the earlier evaluation of chemotherapy response in comparison with the RECIST criteria<sup>[76,78]</sup>. Indeed, Cui *et al*<sup>[79]</sup> reported an prompt increase in ADC values (on day 3 or day 7 after chemo) in responding lesions, thus representing the change in tissue composition: this aspect may allow clinicians to prevent overtreatment, thus avoiding adverse effects<sup>[78]</sup>. However, the ADC map may not be a sufficient diagnostic imaging method itself but needs to be integrated with other MRI sequences<sup>[80]</sup>.

To move forward, it's important to highlight that the ADC map relies on the mono-exponential model based on the Gaussian movement of water molecules. However, considering that tumor heterogeneity affects the non-Gaussian diffusion behavior, two new diffusion techniques, namely intravoxel incoherent motion (IVIM) and diffusion kurtosis imaging (DKI), were introduced<sup>[78]</sup>.

IVIM evaluates both diffusion and microcapillary perfusion modifications, analyzing the signal decay curve obtained from multiple b-values<sup>[81]</sup>, while DKI is a straightforward extension of DWI providing a sensible measure of tissue structure depending on a probability distribution function<sup>[69,82]</sup>. Both modalities were analyzed by different studies, with a special focus as a predictor tool for response to therapy. In particular, Zhang *et al*<sup>[83]</sup> demonstrated the possible role of IVIM and DKI in predicting response to therapy in CRC liver metastases: at baseline, lower D values on IVIM map



and higher K values on DKI map were independently associated with a good response to chemotherapy.

However, in clinical practice, DWI sequences are sometimes affected by artifacts, especially due to motions (cardiac pulsations and peristaltic movements) or magnetic susceptibility (especially at the boundary surfaces)<sup>[84]</sup>. Different techniques were developed to avoid or at least reduce the amount of artifacts, firstly to increase reader's confidence for the final diagnosis. In fact in 2021, some Authors aimed to compare the clinical utility of single-shot echo-planar imaging (SS-EPI) using different breathing schemes and readout-segmented EPI (RS-EPI). The Authors found out that RS-EPI has the higher signal-to-noise ratio (SNR), suggesting it as an emerging technique to be applied in everyday clinical practice<sup>[85]</sup>. More details regarding the usefulness of advanced DWI techniques are out of the scope of the present review; more details can be found in the review by *Saito et al*<sup>[84]</sup>.

## **CONVENTIONAL MRI FEATURES OF LIVER METASTASES**

### **Typical appearance**

Liver metastases typically occur as multifocal nodular lesions but less frequently they can occur as a solitary lesion, large confluent masses, or have an infiltrative appearance with multiple small lesions spread in the hepatic parenchyma (**Figure 2**). Two other rare patterns of distribution include the miliary diffusion which can be observed in lung, breast carcinomas, uveal melanoma, and neuroendocrine tumors and metastases situated in the gallbladder fossa in gallbladder cancer due to peculiar venous drainage<sup>[32]</sup>. Liver metastases from extrahepatic carcinomas usually have ill-defined margins and can present variable sizes, ranging from small nodules to bulky masses. MRI sequences like DWI and HBP images are particularly useful to identify small lesions, especially those with diameters < 1 cm<sup>[33]</sup>.

The typical appearance of liver metastases is variable depending on the primary cancer, the lesions size, the extent of the disease, and background liver tissue. On non-contrast MRI, liver metastases are classically hypointense compared to the surrounding liver

parenchyma. A slightly hypointense rim can be observed at the periphery of the lesions, reflecting the most viable tissue. Radiologists should be aware that some metastases can demonstrate various degrees of spontaneous hyperintensity on T1-weighted images, suggesting the presence of high protein concentration (mucinous tumors), necrosis (colorectal adenocarcinomas), melanin (melanoma) or methemoglobin (hemorrhage)<sup>[34]</sup>. Fat in mass is not observed in hepatic metastases with few exceptions on fat-containing tumors such as liposarcomas or malignant teratomas<sup>[35,36]</sup>. On T2-weighted images, liver metastases can demonstrate variable mild to moderate T2 hyperintensity, reflecting the variable amount of hypercellularity and internal desmoplastic fibrotic stroma. Elevated signal on T2-weighted images is related to cystic or necrotic changes in larger metastatic lesions, whereas smaller lesions may appear isointense. Marked hyperintensity on T2-weighted sequences may be detected in metastases from neuroendocrine tumors, which can resemble the imaging appearance of small hemangiomas. Up to 25% of liver metastases can demonstrate a targetoid appearance on T2-weighted images, also known as target sign, which is characterized by a mild central T2 hyperintensity surrounded by a peripheral rim of moderate-to-marked T2 hyperintensity<sup>[32]</sup>(**Figure 4**). DWI and the apparent diffusion coefficient (ADC) map are useful to detect liver metastases, showing a restricted diffusion with ADC values lower than those of the parenchyma because of increased cellularity of the lesions. Targetoid appearance can be observed also on DWI, with a peripheral rim of marked diffusion restriction indicating the peripheral proliferative area of the metastases as opposed to the central necrotic region<sup>[37]</sup>.

On post-contrast images, liver metastases can be classified according to the enhancement pattern on the late hepatic arterial phase as hypovascular or hypervascular metastases, as detailed below. On the portal-venous phase, hepatic metastases show washout, either complete or more prominent at the lesion's periphery. The peripheral washout sign, in which a peripheral rim is hypointense compared to the lesion's center and to surrounding parenchyma, can be present in both hypervascular

and hypovascular metastases, but it's observed more frequently in hypervascular ones<sup>[38]</sup>. Histopathologically, peripheral washout might reflect perfusion alterations at the peripheral area of the lesions, which presents good arterial supply and good venous drainage of contrast<sup>[37]</sup>. It is important to note that washout appearance should be assessed on portal-venous and delayed phases when using ECAs, while it can be evaluated exclusively on portal-venous phase when Gd-EOB-DTPA is administered, as its uptake by functional hepatocytes starts at approximately 90 s after the contrast injection<sup>[39]</sup>.

Liver metastases are typically hypointense compared to the background liver tissue on the HBP acquired after the administration of HBAs. However, metastases can also demonstrate a targetoid appearance on the HBP with marked hypointensity at the periphery of the lesion as opposed to the central cloud of enhancement likely due to contrast accumulation in the extracellular space or central fibrotic stroma<sup>[40,41]</sup>. Aberrant expression of OATP transporters has also been occasionally reported in CRC liver metastases<sup>[42]</sup>. Compared to FDG-PET and CT, EOB-MRI demonstrated the highest sensitivity (93.1%) in detecting liver secondary lesions with improved specificity (87.3%) in comparison with CT<sup>[43]</sup>. Moreover, MRI can significantly improve liver metastases detection in patients with hepatic steatosis, which can be easily overlooked on CT especially when small in size<sup>[44]</sup>.

### **Hypovascular metastases**

Hypovascular metastases are lesions in which the arterial phase enhancement is inferior or similar compared to that of the healthy liver and therefore appear hypointense on the late hepatic arterial phase. Arterial phase hypoenhancement is the most frequent pattern in liver metastases and it can be typically observed in gastrointestinal carcinomas, bladder, prostate, and lung cancers. These lesions typically demonstrate persistent hypoenhancement on the post-arterial phases and are hypointense on the HBP.

### **Hypervascular metastases**

Hypervascular metastases manifest as lesions in which the arterial phase enhancement is higher compared to that of the liver parenchyma and therefore appear as hyperintense on the late hepatic arterial phase. The arterial phase hyperenhancement can be heterogenous and it can be observed in the whole or part of the lesions or be more pronounced at the periphery (e.g. rim arterial phase hyperenhancement). Hypervascular liver metastases with whole lesion hyperenhancement typically arise from hypervascular primary cancers such as neuroendocrine ones, renal cancer, melanoma, and thyroid cancer. These lesions can demonstrate early wash-out on the portal-venous phase or, more rarely, fading or persistent enhancement on post-arterial phases (**Figure 5 and 6**).

Metastases with peripheral arterial phase hyperenhancement are characterized by a targetoid appearance on post-contrast phases, showing rim hyperenhancement on arterial phase with washout on portal-venous or delayed phases, reflecting the increased cellularity at the lesion's periphery, in comparison with the central hypoperfused area<sup>[37,45]</sup>.

MRI can improve the detection of arterial phase hyperenhancement by acquiring multiple arterial phases. This technique allows to detect early enhancement that can be missed on late arterial phase with improvement in enhancement detection compared to single-phase acquisition<sup>[46,47]</sup>. However, its usefulness for differential diagnosis between liver metastases and other liver lesions needs to be validated. Finally, subtraction images should always be considered to detect the arterial phase hyperenhancement in lesions showing hyperintensity on pre-contrast T1-weighted images.

### **Atypical appearance**

In current clinical practice, unusual radiologic features of liver metastases may be found thus making it challenging to discriminate metastases from other focal liver lesions. Detailed knowledge of atypical imaging features of liver metastases with a good understanding of the histopathologic background is crucial for accurate differential

diagnosis. Among these, metastases with cystic appearance, calcifications, or fat are herein discussed.

#### *Cystic liver metastases*

Cystic liver metastases usually appear on MRI as strongly hyperintense on T2-weighted sequences, hypointense on non-contrast T1-weighted images, with lack or rim enhancement on contrast-enhanced T1-weighted images. They may occur mainly from CRC, pancreatic cancer, neuroendocrine tumors (NETs), ovarian cancer, gastrointestinal stromal tumors (GISTs), melanoma and sarcomas. The causative mechanisms of cystic appearance of liver metastases may vary<sup>[37,48]</sup>:

1. Rapid growth beyond hepatic arterial blood supply of the lesion, thus causing central necrosis, such as in NETs, GISTs, sarcomas, melanomas, angiosarcomas, testicular carcinomas, or squamous cell carcinomas
2. Mucinous components of the primary tumor, such as in mucinous CRCs or ovarian carcinomas
3. Marked T2-weighted hyperintensity due to the primary histological features
4. Changes after chemotherapy, including necrosis or cystic or mucinous regression.

Mucinous metastases from CRC are particularly challenging in daily practice because, in addition to marked T2-weighted hyperintensity, they show a lack of diffusion restriction in about 81% of cases, thus making the differential diagnosis with benign cysts very challenging<sup>[49]</sup>.

#### *Calcified liver metastases*

Calcified liver metastases usually show small or diffuse calcifications appearing hypointense on both T1- and T2-weighted imaging, and are better demonstrated on CT. Calcified liver metastases may occur mainly from CRC liver metastases, bone-forming tumors (osteosarcoma and chondrosarcoma), lung, breast, prostate, stomach, ovary, thyroid, neuroendocrine tumors, GISTs, neuroblastoma, and melanoma<sup>[50-52]</sup>.

The causative mechanisms of the calcified appearance of liver metastases may vary:

1. Dystrophic calcifications resulting from necrosis and/or hemorrhage within the tumor
2. Mucoid calcifications related to the presence of mucin produced by mucinous adenocarcinomas
3. Proper production due to the intrinsic nature of the primary metastasizing malignancies
4. Changes after chemotherapy, including mineralization of necrotic tissue.

The occurrence of calcifications in CRC is well-known since the first years of the 1960s when Engel S<sup>[53]</sup> described their occurrence in the primary tumor at pathology and Miele AJ<sup>[54]</sup> identified them in liver metastases on abdominal radiographies in four patients, with pathology confirmation in three of the four patients. In patients with CRC, calcifications may be present in up to 11% of cases before chemotherapy<sup>[51]</sup> and in about 5% of cases after chemotherapy usually - though not always - indicating tumor response<sup>[55]</sup>.

#### *Fat-containing liver metastases*

The occurrence of fat in liver metastases may be distinguished based on the fat distribution and type of fat into three different scenarios. First, intralesional macroscopic fat may be encountered in metastases from liposarcoma and will show hyperintensity on T2-weighted non-fat-sat sequences, and heterogenous appearance on T1-weighted images with moderate signal loss on opposed-phase and increased signal on in-phase images, indicating the presence of macroscopic fat. Second, intralesional intracellular fat may be encountered very rarely having been described in liver metastases from renal cancer<sup>[56]</sup>. Third, liver metastases from malignant teratomas can contain extracellular fat, calcifications, and necrotic components <sup>[35,36]</sup>.

#### **The role of MR in TSTC lesions**

Too small to characterize (TSTC) liver lesions are defined as those small liver lesions - typically 1.5 cm in diameter or smaller - that cannot be confidently characterized on CT



by the interpreting radiologist on the available images. In most cases, TSTCs are benign<sup>[57]</sup>, and this is particularly true for solitary hepatic lesions up to 1 cm, that therefore do not require any follow-up if identified in low-risk patients including patients with no known primary cancer, hepatic risk factors or hepatic failure<sup>[58,59]</sup>.

#### *Indications to MRI for TSTC*

TSTC lesions up to 1 cm identified on CT need follow-up with MRI at 3-6 mo whenever identified in high-risk patients, including patients with known primary cancer with a propensity for liver diffusion, cirrhosis, and/or other hepatic risk factors<sup>[58,59]</sup>.

Characterization with MRI of TSTC lesions between 1 and 1.5 cm is indicated whenever suspicious imaging features are present or if "flash-filling" imaging features are identified in high-risk patients<sup>[58,59]</sup>. Suspicion imaging features embrace blurred margins, heterogeneous density, nodularity or mural thickening, thick septa, intermediate-to-high attenuation on portal venous-phase acquisitions, and enhancement of at least 20 HU between precontrast and post-contrast CT<sup>[59]</sup>.

In addition to the previous settings, MRI characterization or follow-up should be considered<sup>[58]</sup>:

- if an incidental TSTC lesion smaller than 1 cm is newly detected on CT follow-up even in low-risk patients,
- if a small cystic lesion is encountered in patients with ovarian cancer or GISTs,
- in case of small TSTC growing over time.

#### *MRI characterization of TSTC*

MRI with and without injection of contrast media is oftentimes regarded as the problem solver for the characterization of hepatic TSTC. To date, contrast-enhanced MRI allows to permit a conclusive diagnosis in 95% of liver lesions, with only 1.5% of patients with MRIs requiring further exams<sup>[60]</sup>. The MRI diagnostic accuracy depends on the sequences acquired and type of contrast agent used, as well as the lesion itself. A step-by-step approach to MRI is mandatory for the characterization of hepatic TSTC. Non-

contrast enhanced MRI sequences allow to identify some key imaging clues for the diagnosis of small benign lesions that should be regarded before looking at contrast-enhanced images. The analysis of T2-weighted images and DWI are oftentimes sufficient to characterize small liver cysts and small hemangiomas which are the most common incidental liver lesions; indeed, both lesions will show a lack of diffusion restriction or the so-called "T2-shine through" phenomenon, and then cysts will be as bright as the cerebrospinal fluid on T2-weighted sequences while hemangiomas will show a slightly lower hyperintensity as compared to the cerebrospinal fluid on T2-weighted images<sup>[61]</sup>. A clear knowledge of these pre-contrast characteristics allows to avoid misdiagnosis if a "pseudo-washout" is identified on the 3-minute phase with Gd-EOB-DTPA<sup>[62]</sup>. Dual-phase sequence, with in- and opposed-phase images, may allow to identify focal fat accumulation or focal fat sparing that may occasionally mimic a true liver lesion<sup>[63]</sup>. MRI without intravenous contrast agent may therefore answer the clinical question between benignity and malignancy in some cases. In addition, as Moosavi B *et al*<sup>[64]</sup> demonstrated in their study on newly discovered indeterminate focal liver lesions in non-cirrhotic subjects, the information obtained from the HBP does not necessarily modify the diagnosis or the diagnostic confidence. Therefore, in selected cases if the radiologist is confident with the lesion characterization on non-contrast sequences (e.g. cyst, hemangioma), the routine use of intravenous contrast agent may not be necessary<sup>[65]</sup>. Some TSTC lesions remain indeterminate after the assessment of non-contrast MRI sequences. In these cases, post-contrast images may prove to be helpful, and the choice of the contrast agent should be tailored on a per-patient and per-lesion bases. Contrast-enhanced MRI with ECAs may be particularly helpful if the slow-filling hemangioma is the most likely diagnosis and the acquisition of pure extracellular phases would allow to capture complete filling of the lesion. On the other hand, Gd-BOPTA MRI allows to obtain both pure delayed extracellular phases and HBP images although requiring acquisition at 2 h from contrast agent injection, and may be helpful if obtaining information from both delayed extracellular and HBP is deemed necessary. Finally, Gd-EOB-DTPA MRI allows to obtain an HBP at 10-20 minutes from contrast

agent injection. For the differentiation between hepatocellular adenoma and focal nodular hyperplasia, the acquisition of the HBP may be very helpful in the majority of cases demonstrating iso-to-hyperintensity or a donut-like appearance on HBP in case of focal nodular hyperplasia and hypointensity on HBP in most cases of hepatocellular adenomas<sup>[66]</sup>. However, hepatocellular adenomas may occasionally demonstrate inhomogeneous iso-to-hyperintensity on HBP, thus leaving the final diagnosis to pathology for confirmation<sup>[41]</sup>.

## **CONCLUSION**

Contrast-enhanced sequences are mandatory to correctly characterize focal liver abnormalities to assess the vascular behavior of liver parenchyma and lesions.

Extra-cellular contrast agents (ECAs) have historically represented the reference standard for liver-enhanced MRI. All ECAs are distributed within the extra-cellular interstitial space, and despite manufacturers or chemical formulations, they shorten T1 relaxation time, producing a signal intensity enhancement during their biodistribution. From a practical point of view, enhancement proprieties are similar to iodinated contrast media for CT, firstly with the opacification of hepatic arteries and hypervascular lesions (arterial phase, 30-40 s after bolus administration), then liver parenchyma and portal vein (portal-venous phase, 60-80 s after bolus administration), and finally by moving into the interstitial space (delayed phase, 180-300 s after bolus administration). After whole-body distribution, the excretion is entirely through the kidneys<sup>[23]</sup>.

More recently, the introduction of hepatobiliary contrast agents (HBAs) added relevant information to the previous clinical practice, showing some degree of biliary excretion. Due to their ability to bind specific receptors regularly expressed in healthy hepatocytes [organic anion transporter (OATP)], HBAs allow the acquisition of the so-called hepatobiliary phase (HBP) and consequently can increase the diagnostic accuracy for different focal liver lesions. In fact, after the administration of contrast medium bolus, the initial biodistribution is similar to those of ECAs, providing multi-phase dynamic

post-contrast imaging. Moreover, after a specific time, healthy hepatocytes start the uptake of HBAs, which will then be excreted into the biliary ducts. Consequently, in the HBP images, both the liver and the biliary tree are significantly enhanced, while liver vessel and non-hepatocellular lesions show a low signal intensity<sup>[24]</sup>.

Only two HBAs are approved for the clinical practice: Gd-BOPTA and Gd-EOB-DTPA <sup>[25]</sup>. When using Gd-BOPTA, about 3-5% of the contrast dose is eliminated by biliary excretion. In contrast, with Gd-EOB-DTPA, about half of the dose is taken up by hepatocytes and excreted with the bile. Thus, these two contrast media need different acquisition times to obtain diagnostic HBP images, which are acquired about 1.5-3 h after Gd-BOPTA injection and about 15-20 minutes after Gd-EOB-DTPA administration in non-cirrhotic livers. Consequently, the HBP can be acquired at the end of the liver MRI protocol in the case of Gd-EOB-DTPA, while in a second step in the case of Gd-BOPTA<sup>[26,27]</sup>. **Figure 1** summarizes MRI protocols by using ECAs and HBAs.

Choosing the best contrast media when acquiring a liver MR protocol cannot be straightforward, considering that both ECAs and HBAs present advantages and disadvantages. It's well-known that arterial phase acquisition during ECAs' administration can be more robust in comparison with Gd-EOB-DTPA because the latter leads to a lower enhancement of healthy parenchyma (reducing the lesion to liver contrast) and the higher frequency of artifacts<sup>[28]</sup>. Moreover, ECAs allow better detection of lesion washout over time, while the rapid uptake of Gd-EOB-DTPA precludes its evaluation during the transitional phase (acquired 180 to 300" after injection).

On the other hand, the evaluation of HBP can increase contrast resolution between liver parenchyma and secondary lesions. Mainly, one of the most relevant advantages of HBAs is the easy detection of non-hepatocellular lesions and lesions with non-functioning hepatocytes, including hepatic adenomas, hepatocellular carcinoma (HCC), and metastases. Indeed, when impaired hepatocytes are present, the whole lesion or part of it can be easily depictable as hypointense during the HBP images. Moreover, HBAs can increase diagnostic accuracy in the case of focal nodular hyperplasia (FNH),

where functioning hepatocytes increase the uptake of contrast agents, resulting in a hyperintense lesion during the HBP<sup>[29]</sup>.

Due to the high specificity and sensitivity in detecting hepatic focal lesions, HBAs should always be preferred in oncologic patients with known extra-hepatic primary cancer, especially in cases of increased risk of the disease's spread to the liver. The number and location of liver secondary lesions can significantly modify the patient's management and is crucial for treatment strategies' success<sup>[30]</sup>.

Considering that patients with known primary tumors should undergo different follow-up examinations, abbreviated MRI (AMRI) protocols - composed of DWI, T2W, and HBP - have been proposed. In a recently published review, the Authors summarize the advantages and disadvantages of these new approaches. Even if not recommended nor approved by either international society, AMRI could increase the availability of MRI examinations and therefore facilitate strict surveillance of liver metastases, preserving an acceptable accuracy in their detection and characterization<sup>[31]</sup>.

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